



# Accelerators for particle therapy

Marco Schippers



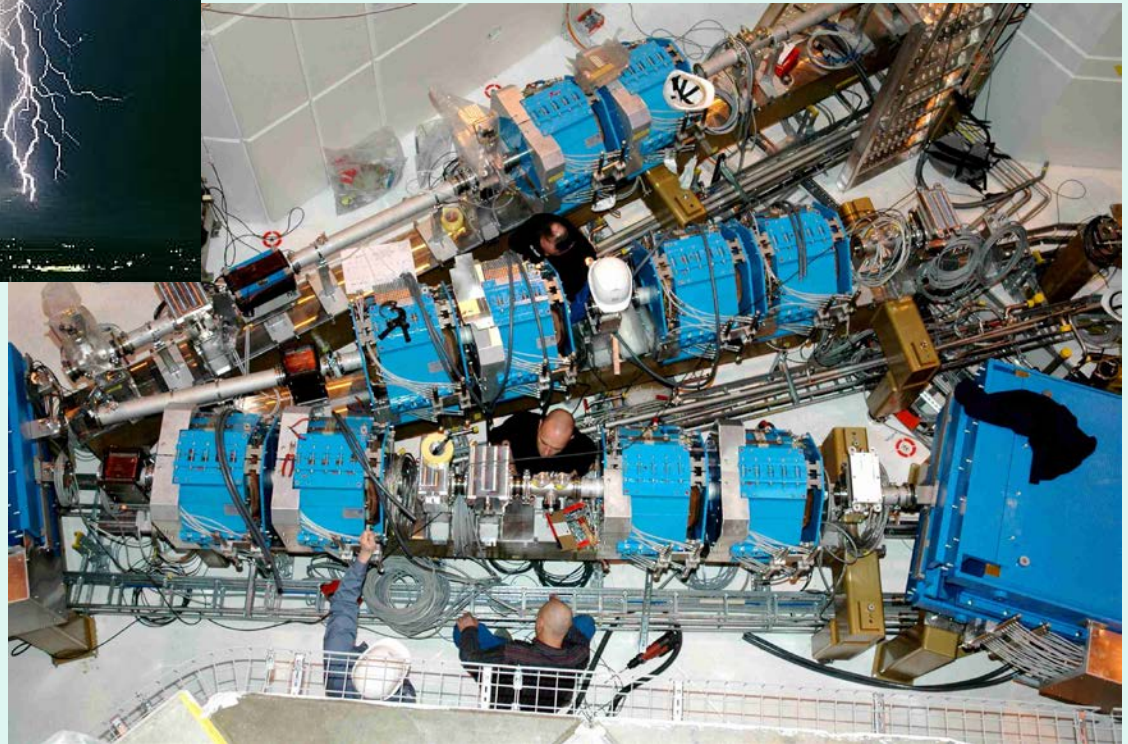
PAUL SCHERRER INSTITUT

Goal of this lecture: give you an idea on possibilities  
of current accelerators

- **electric and magnetic fields**
- **synchrotron**
- **cyclotron**
- **synchro-cyclotron**
- **New developments**

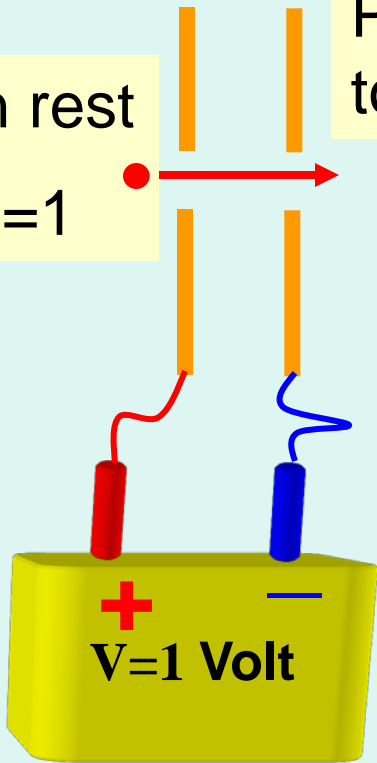
Vendors are acknowledged  
for sharing information and images !!

More details in: J.M. Schippers, Rev. Acc. Science and Techn. 2 (2009) 179-200  
H. Paganetti (ed.), Proton Therapy Physics, Chapter 3.



Proton in rest

$q=1$




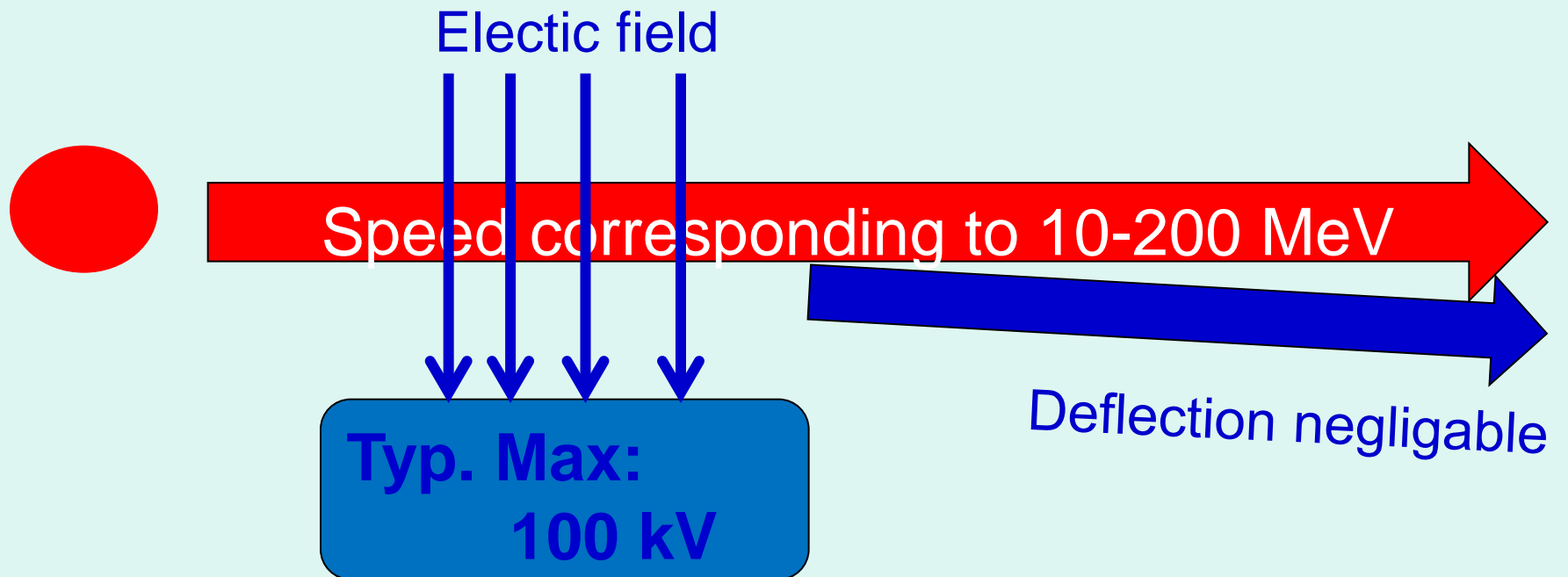
Proton has been accelerated to an energy of  $q \times V = 1 \text{ eV}$

Electric fields are limited in strength

But:

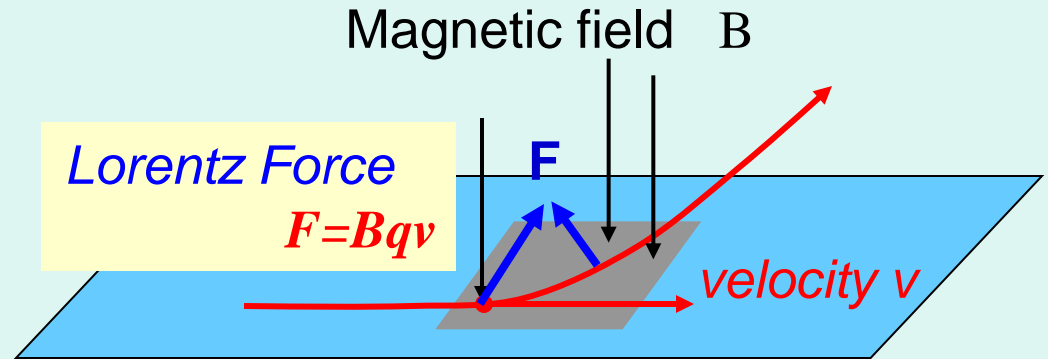
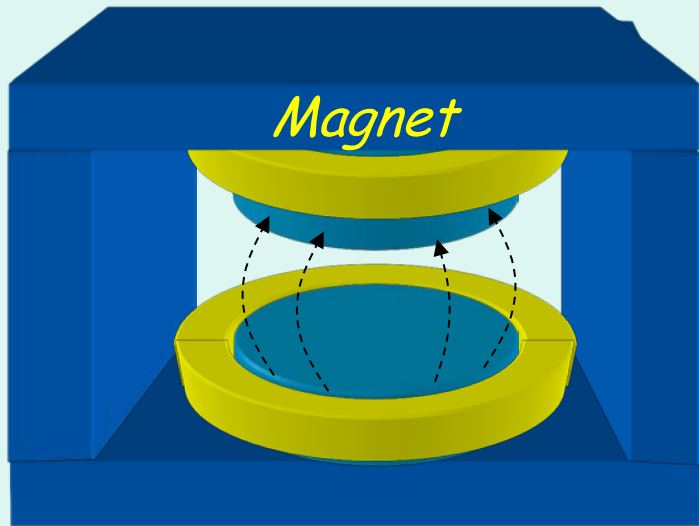
Repeated acceleration  $\rightarrow$  high energy

$$E = qV + qV + qV + qV$$




→ used for **focusing/deflecting** **only at low energy**  
(e.g. in injection line of synchrotron)

# Magnetic fields



Lorentz force = “centripetal force”  $mv^2/\rho$   
 $\Rightarrow$  track = circular orbit with radius  $\rho$

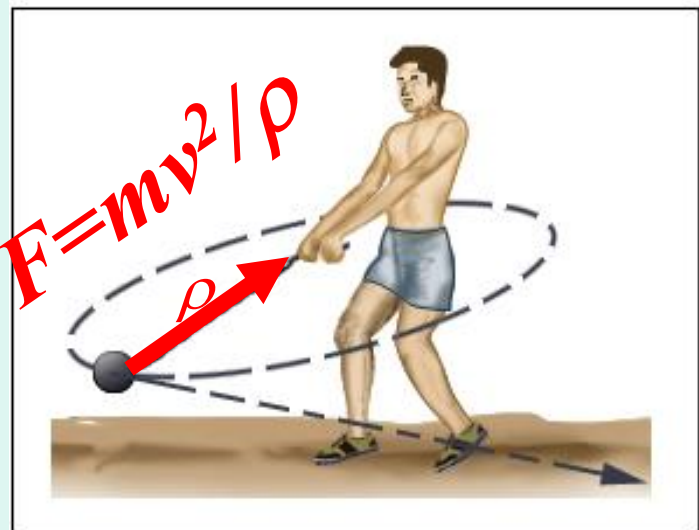
energy  $E$  and charge  $q$

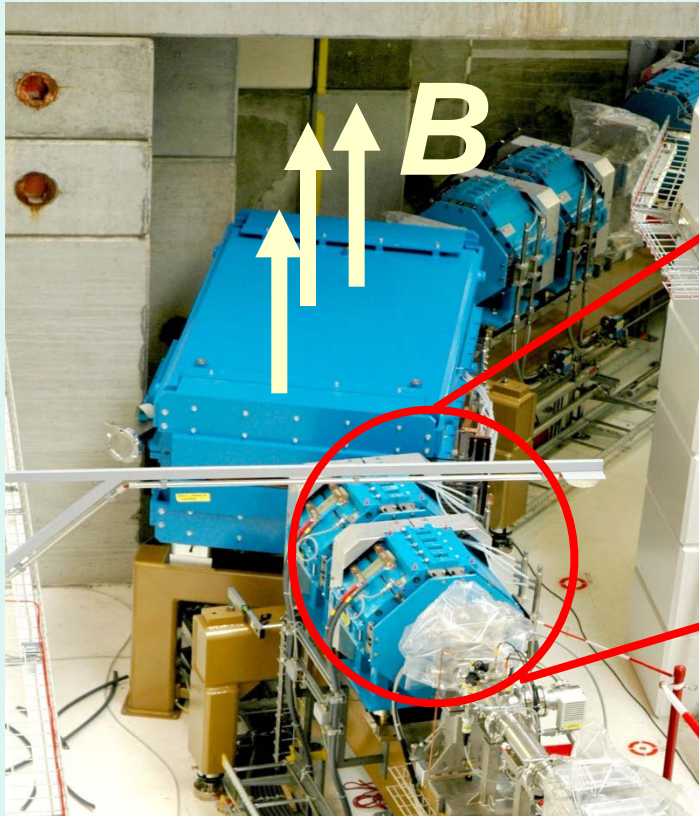
$\Leftrightarrow$  magnetic rigidity:  $B\rho (= p/q)$ :  
**magnet strength  $B$  to bend with radius  $\rho$**

70 MeV  $p$ :  $B\rho = 1.2 \text{ Tm}$

250 MeV  $p$ :  $B\rho = 2.4 \text{ Tm}$

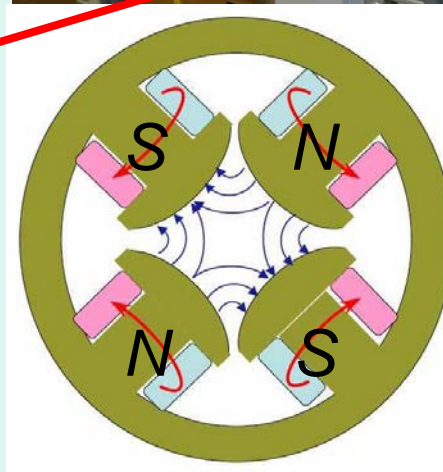
450 MeV/nucl  $C^{6+}$ :  $B\rho = 6.8 \text{ Tm}$





*Dipole magnet:*

*bends the beam direction*



*Quadrupole magnet:  
(de)focuses the beam*

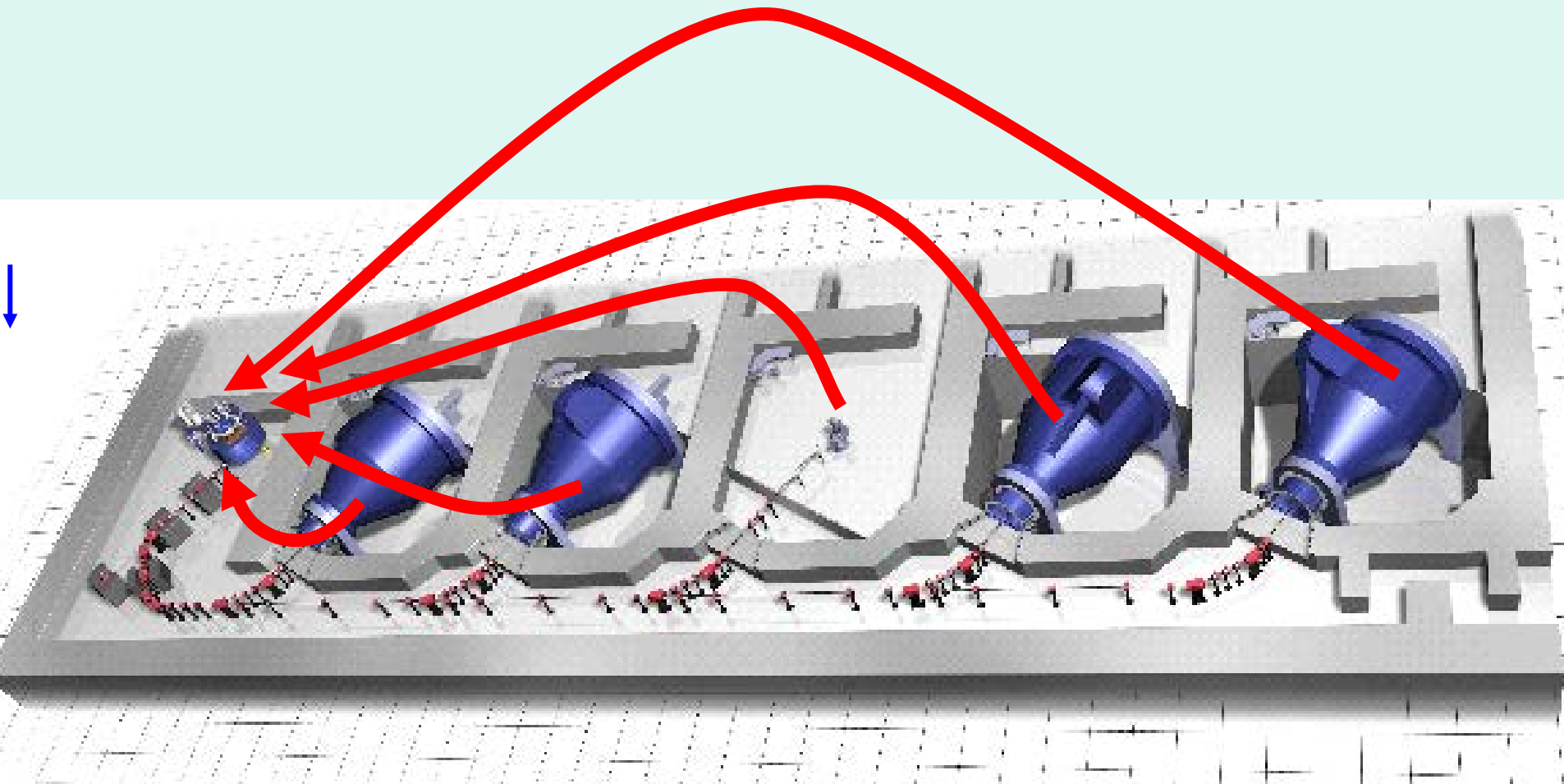
Traversing electromagnetic fields:

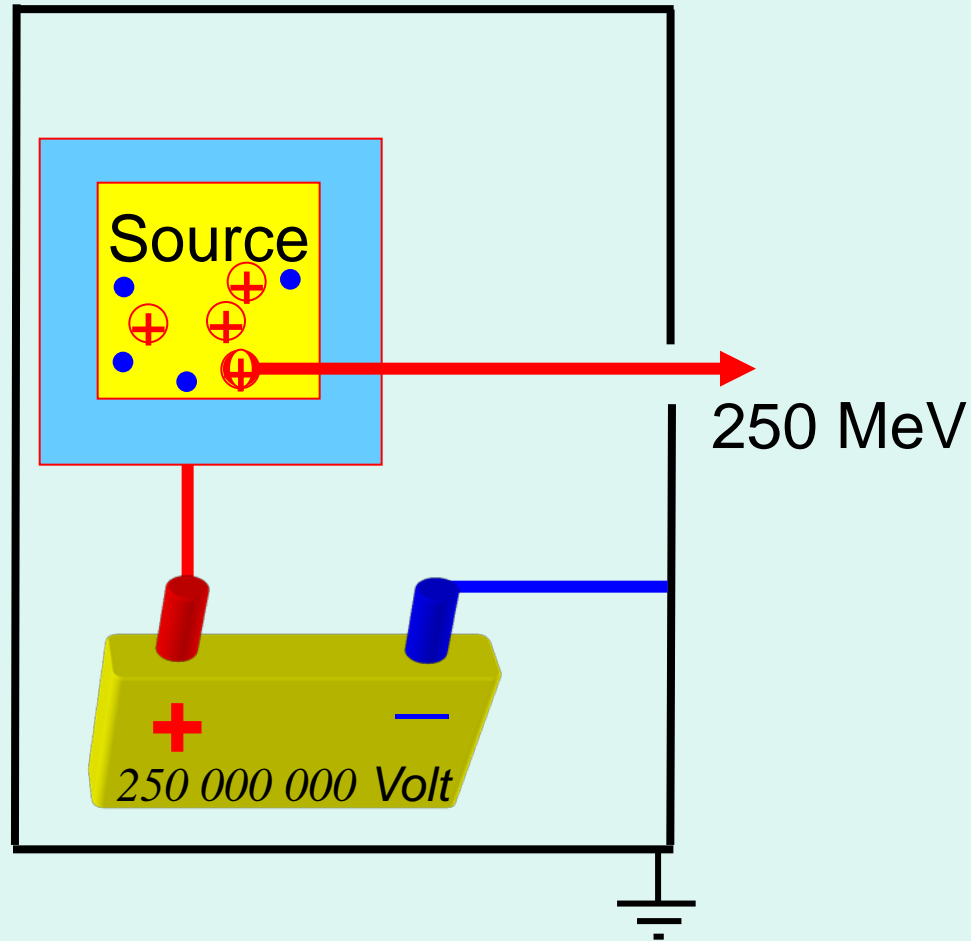
**E:** acceleration

**B:** directing and focusing



However, **NOT** independent....





# Present accelerator choice



**cyclotron**

**synchrotron**

**Protons**

in use,  $\varnothing$ 3.5-5 m

in use,  $\varnothing$ 8-10 m

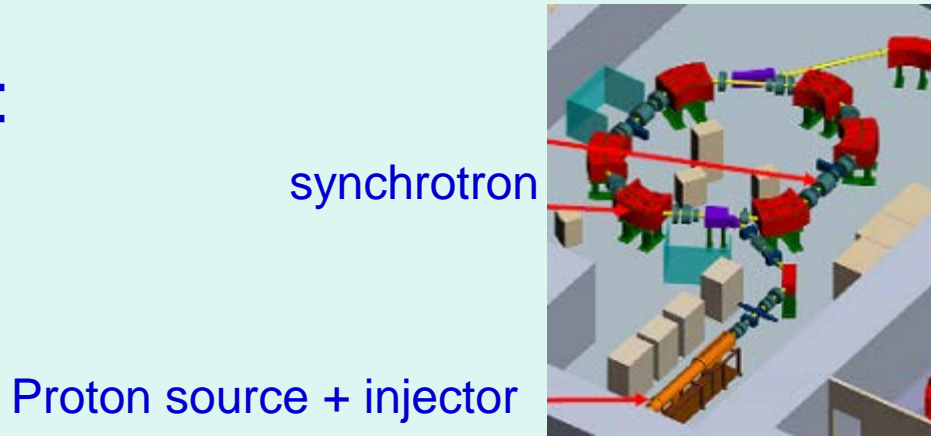
**Carbon ions**

test phase

in use,  $\varnothing$ 25 m

# Synchrotron (1945)

Protons only:  
( $\varnothing$  ~8 m)

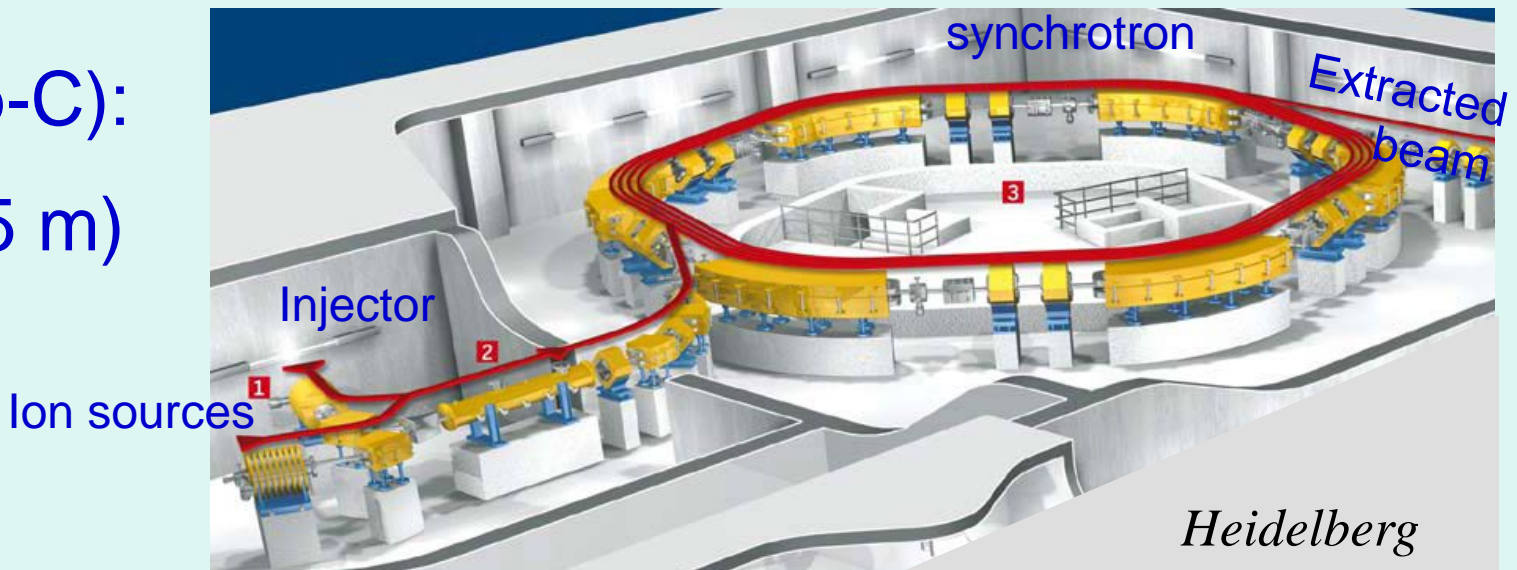


Extracted beam

synchrotron

Proton source + injector

Ions (p-C):  
( $\varnothing$  ~25 m)



synchrotron

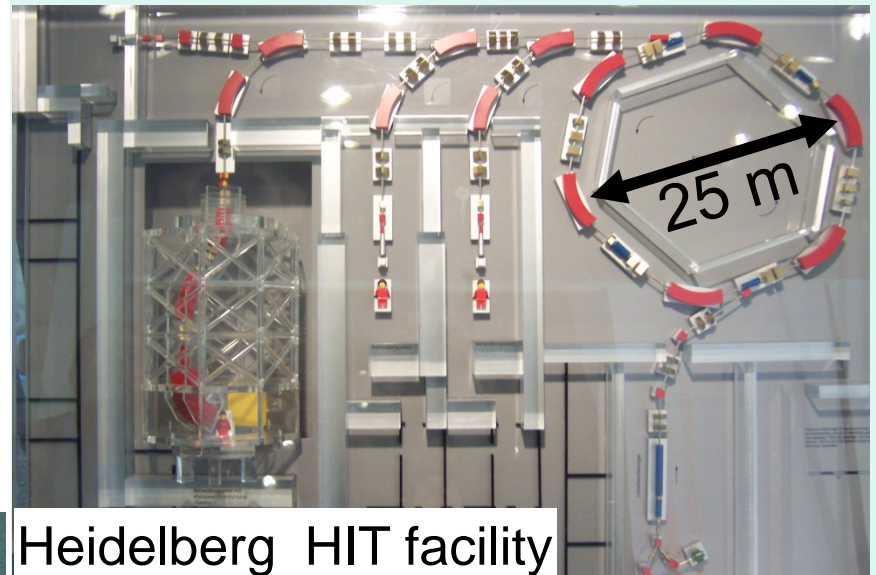
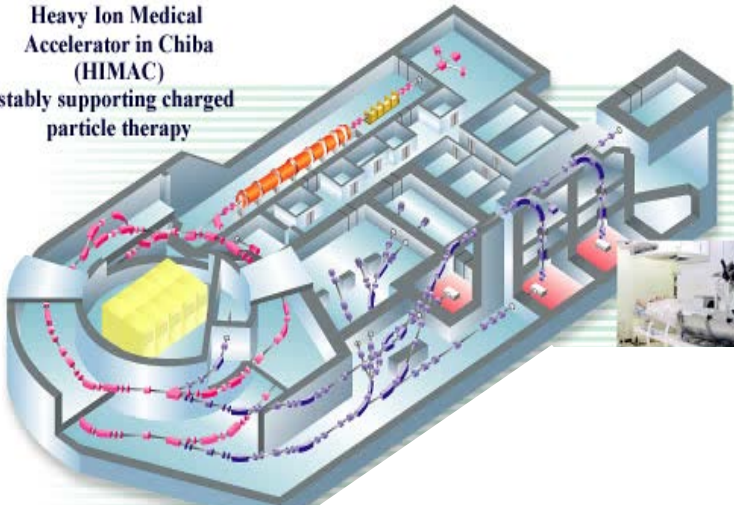
Extracted beam

Injector

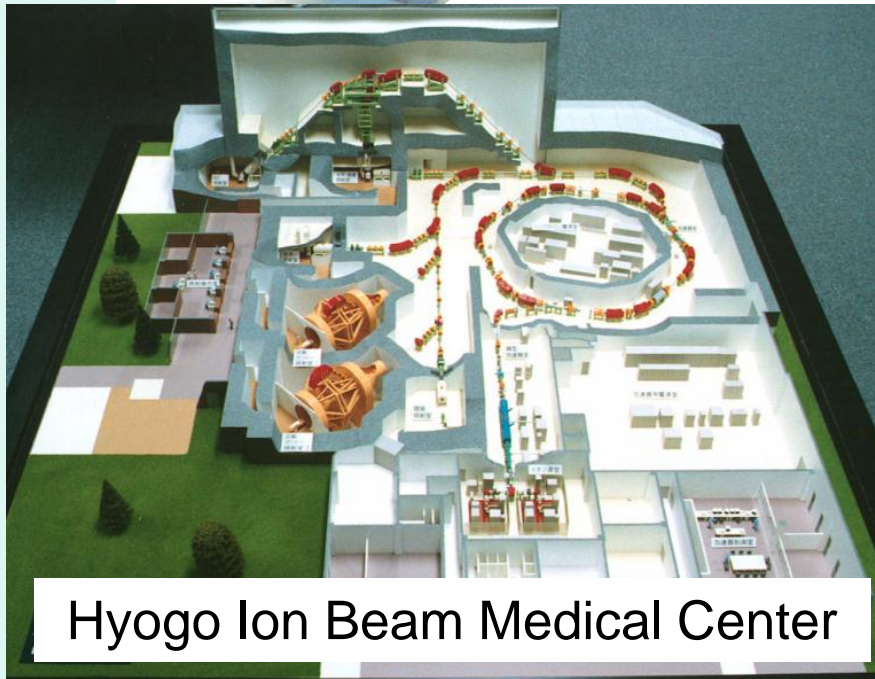
Ion sources

Heidelberg

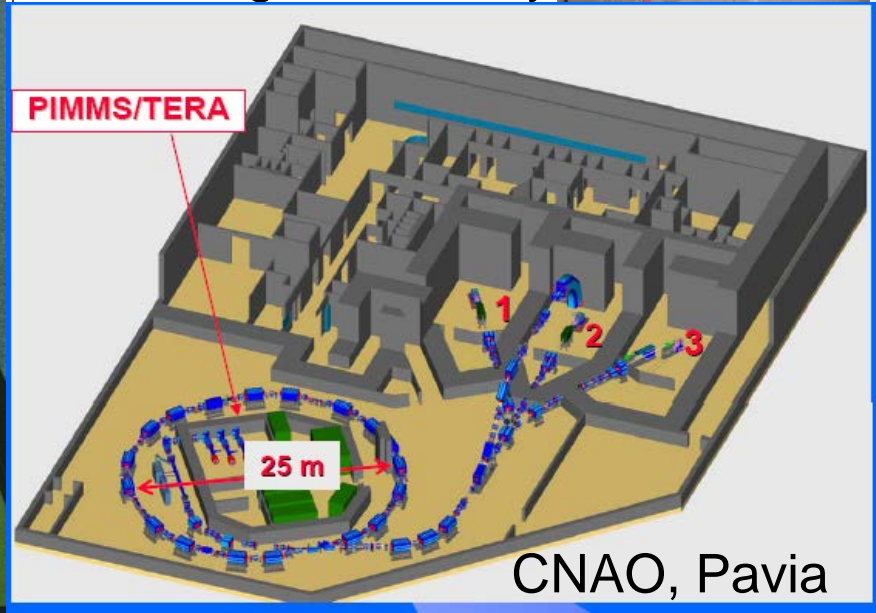
Heavy Ion Medical Accelerator in Chiba (HIMAC) stably supporting charged particle therapy



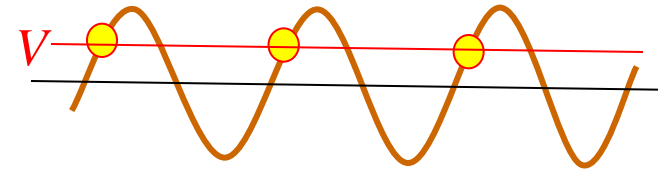
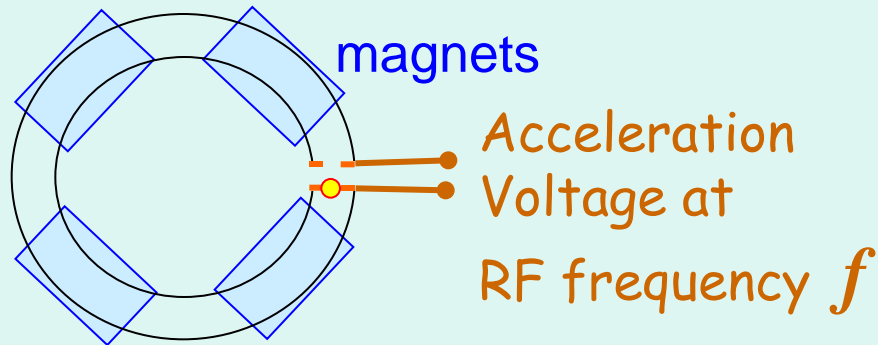
Heidelberg HIT facility



Hyogo Ion Beam Medical Center



CNAO, Pavia



At electrode slit crossing:  
Energy gain  $\Delta E = V \cdot q$

Energy increases:

→ speed ↑

→ RF frequency ↑

→ field in magnets ↑  $\frac{p}{Bq} = r = \text{constant!}$

Magnets and RF frequency  
change **Synchronous** to particle **revolution frequency**

Extraction into beam line

Ring:

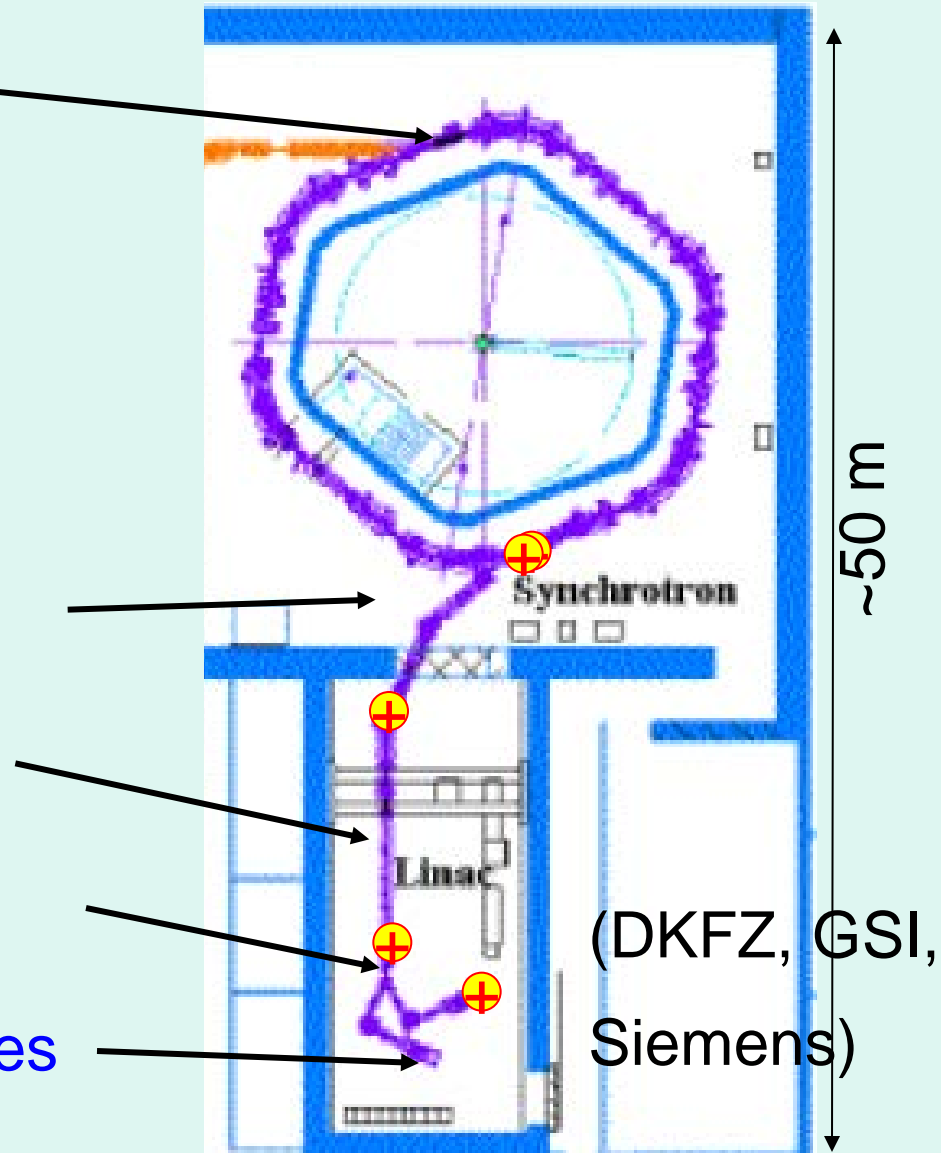
- collect  $10^{11}$  particles
- acceleration to desired E
- storing of the beam

Injection in ring at 7 MeV/nucl

2 linear accelerators in series

Magnet to select ion source

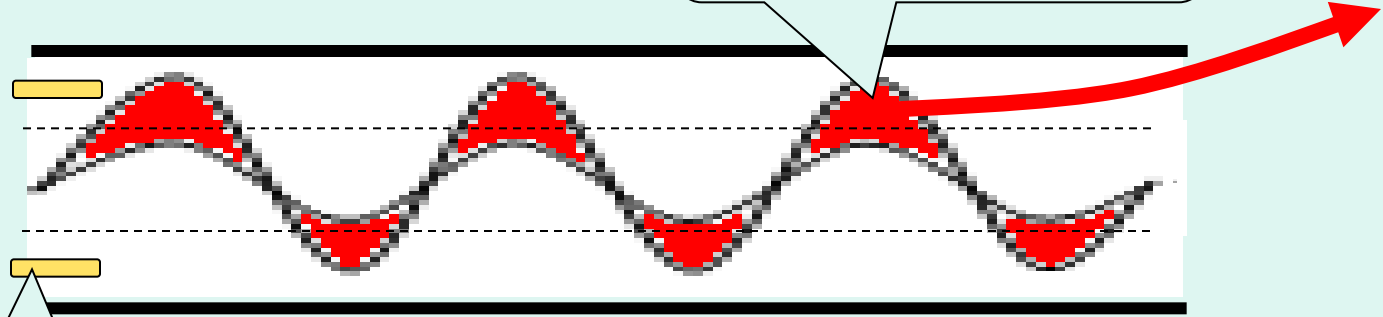
Ion sources for different particles



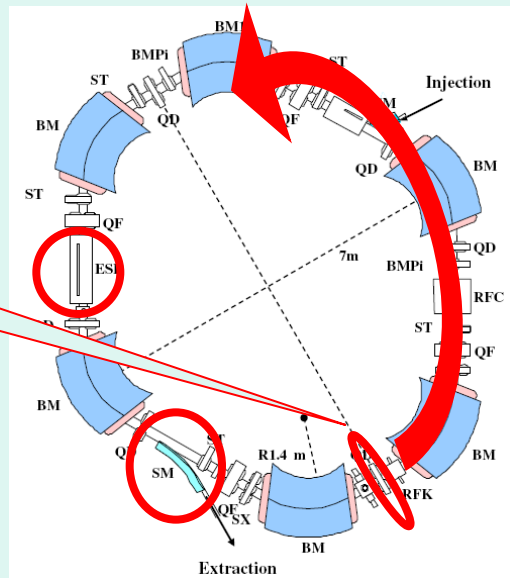
(DKFZ, GSI,  
Siemens)

## RF-Knock Out

Unstable orbits  
→ extracted



RF kicker: **increases** emittance (beam size)

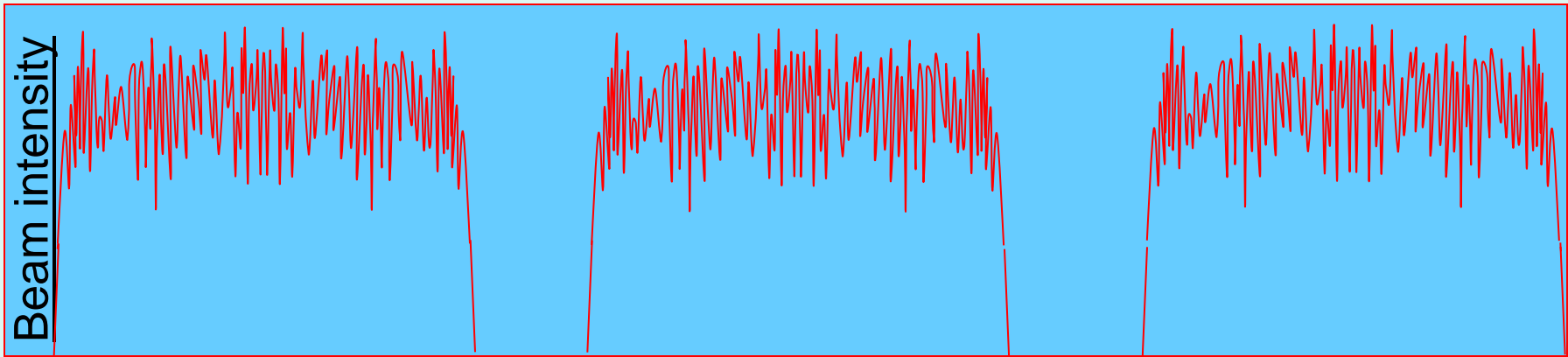


With RF-knock Out:  
Extracted beam  
**position and size**  
remain constant

Beam shape:



# Synchrotron beam: spills

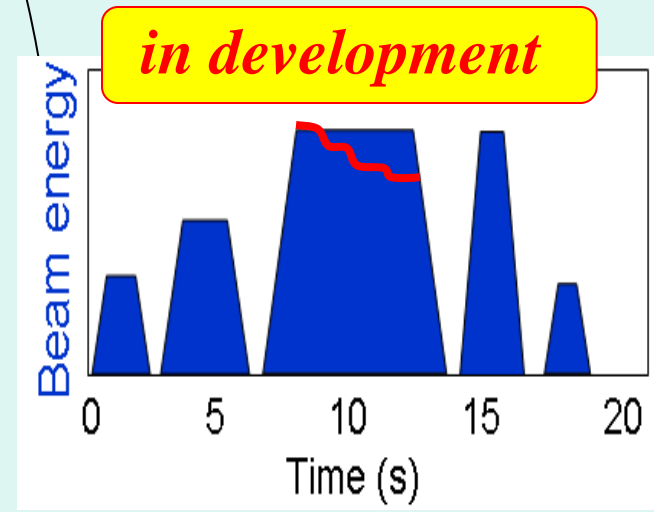


0.5-1 sec      1-10 sec

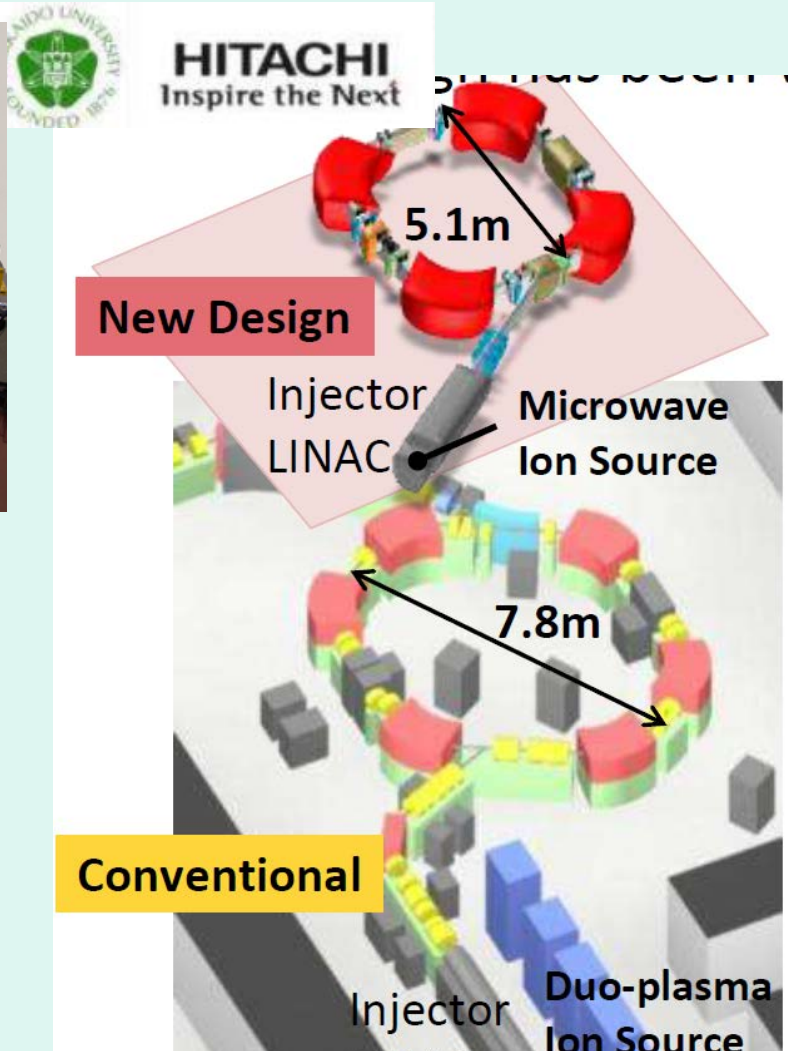
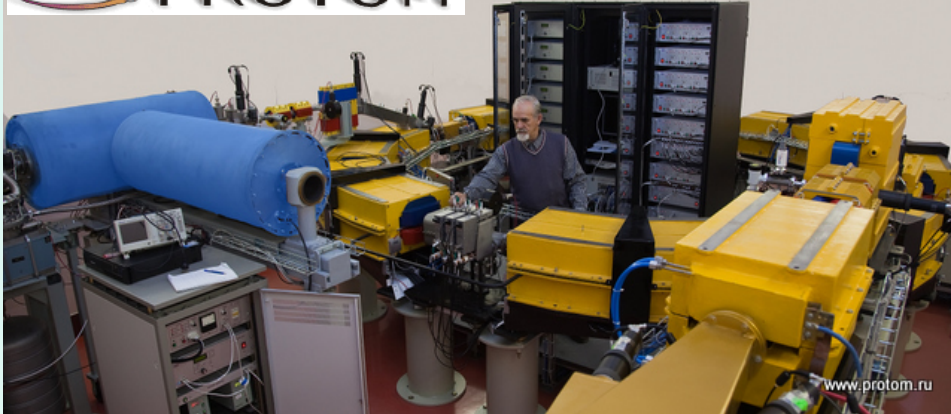
Time →

“spill” time

- fill ring with  $\sim 10^9$ - $10^{11}$  particles
- accelerate to desired energy
- extract slowly during 1-10 sec
- decelerate and dump unused particles



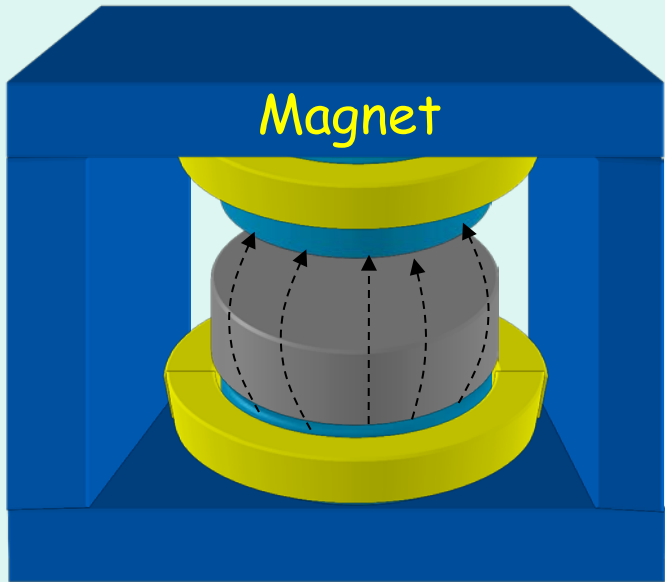
# Compact synchrotron



ProTom 330 MeV

2012: Installation at:  
McLaren, Flint (Mi)  
MGH Boston (Ma)

- 220 MeV
- First facility in Hokkaido started 2013



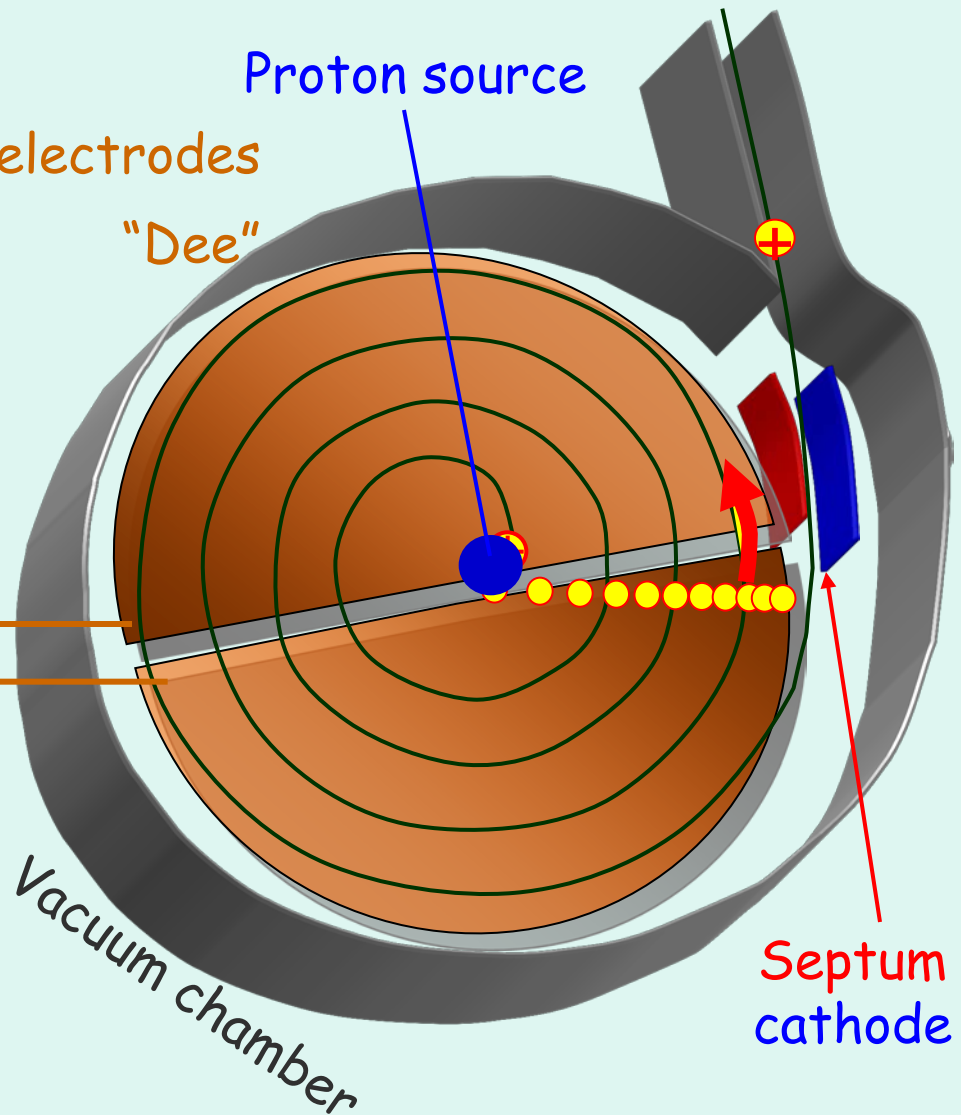
Magnet

Proton source  
RF electrodes  
"Dee"

RF-Voltage "V<sub>dee</sub>"   
RF frequency  $f$

At electrode slit crossing:

Energy gain  $\Delta E = V_{dee}$



Vacuum chamber

Septum cathode

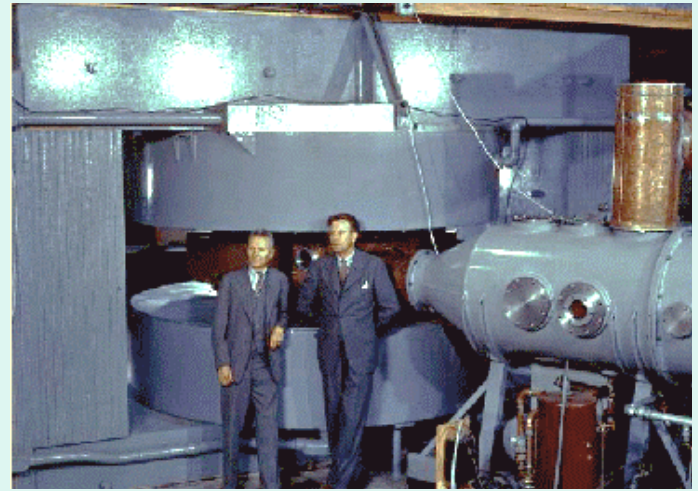
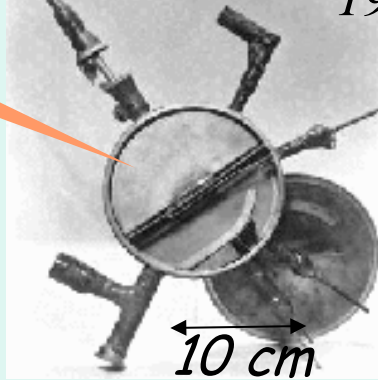
# Cyclotron



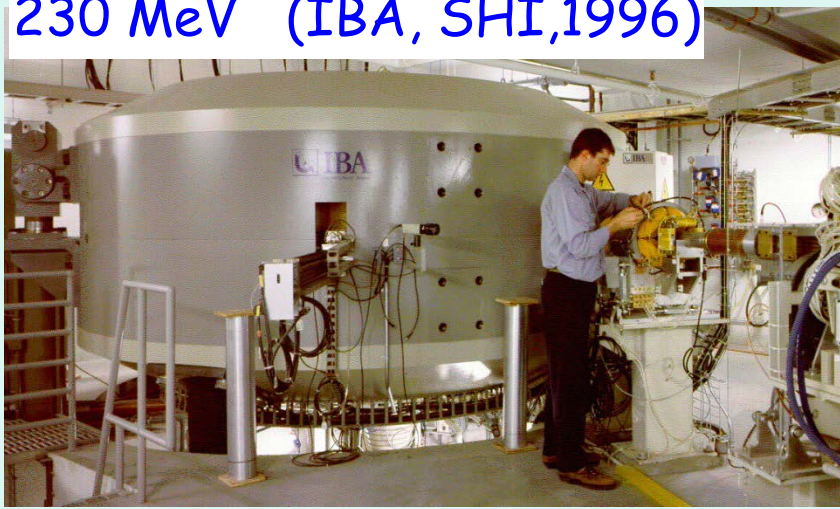
Ernest Lawrence

80 keV protons  
1930

Dee



230 MeV (IBA, SHI, 1996)



250 MeV (ACCEL/Varian, 2005)

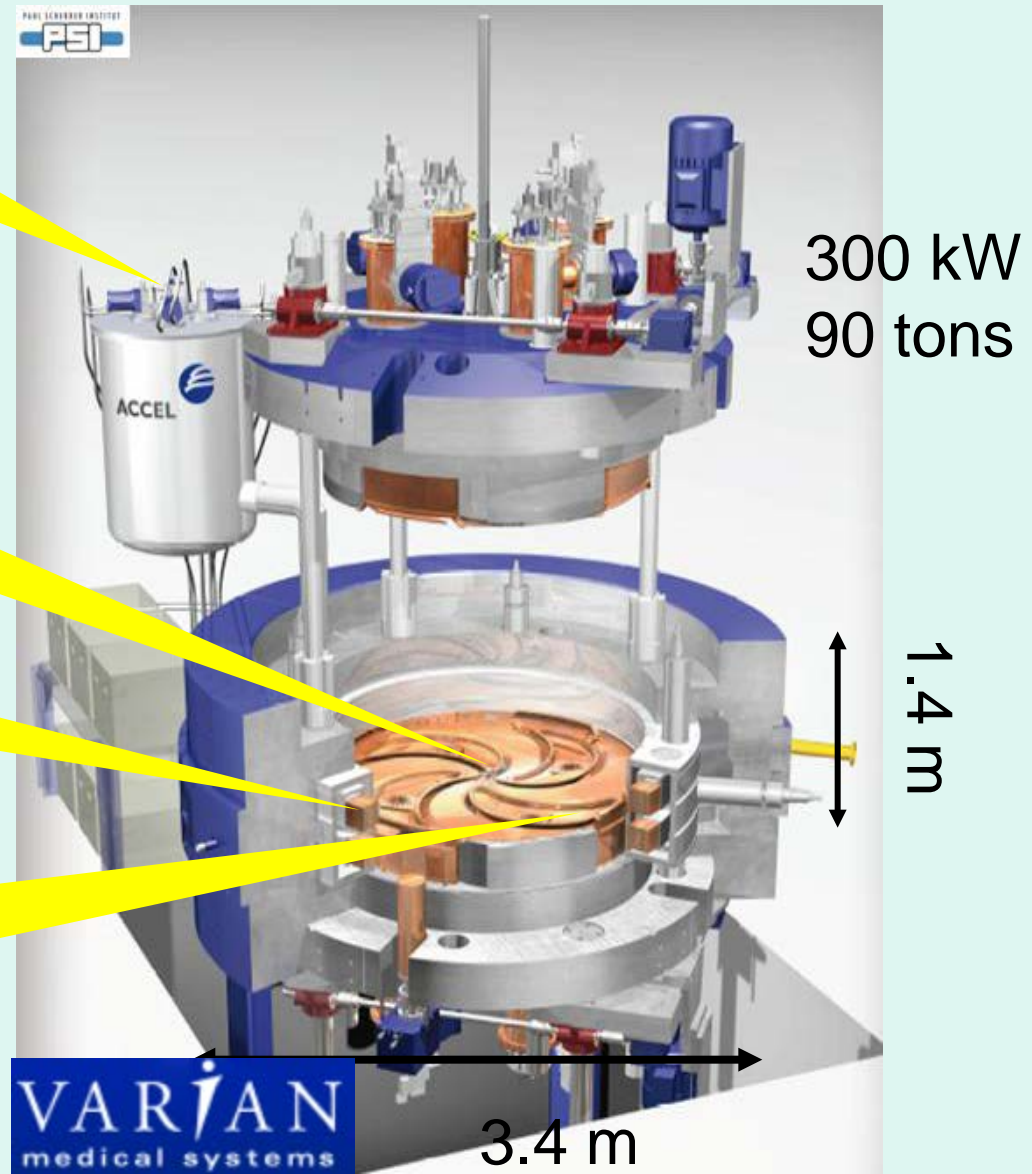


Closed He system  
4 x 1.5 W @4K

Proton source

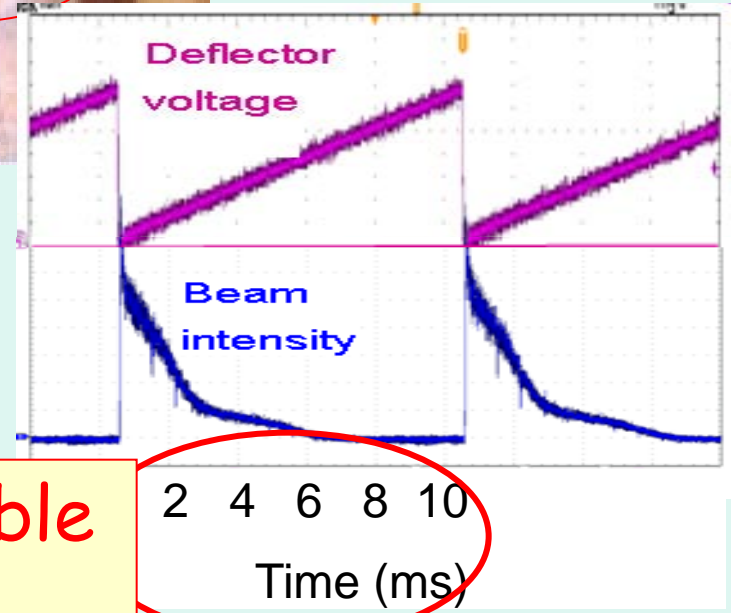
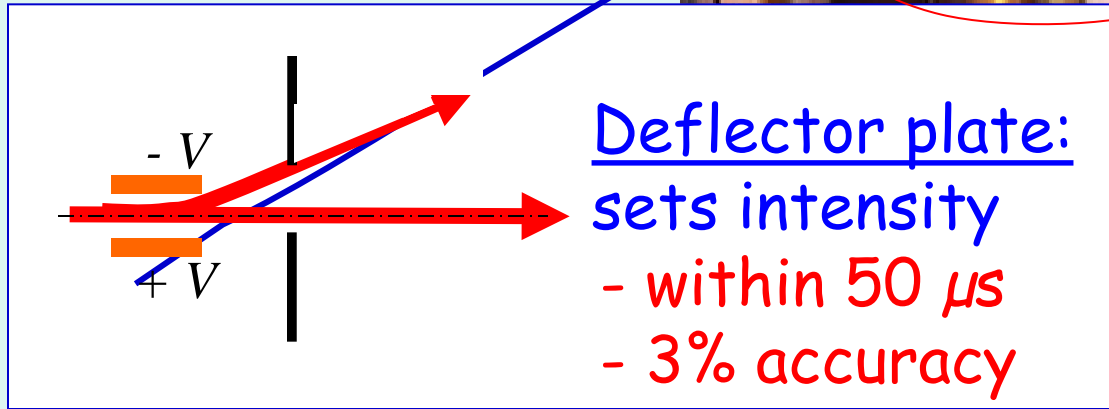
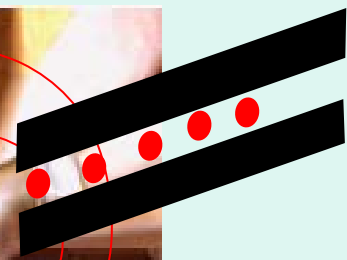
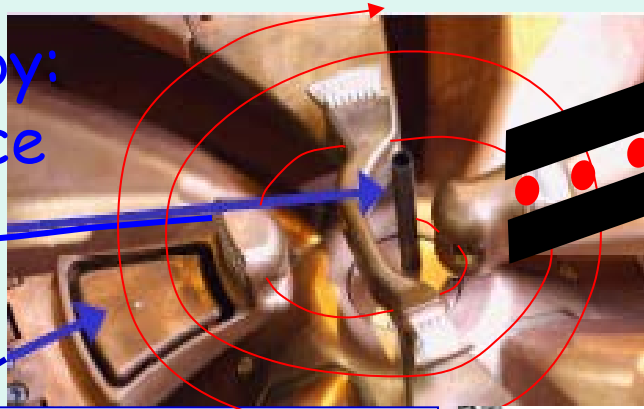
superconducting coils  
=> 2.4 - 3.8 T

4 RF-cavities:  
72 MHz (h=2)  
~80 kV



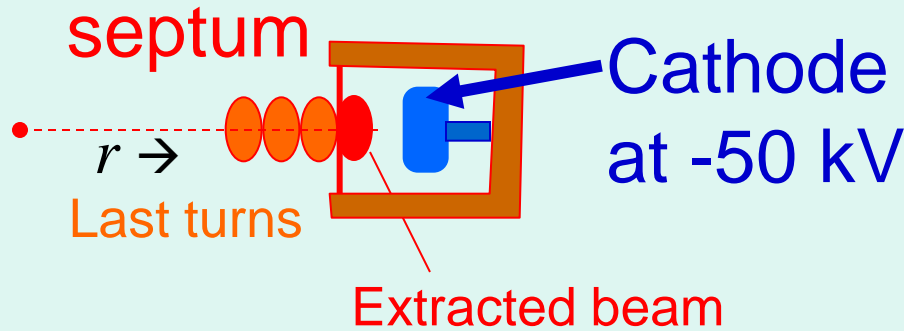
# intensity control

Max. intensity set by:  
proton source

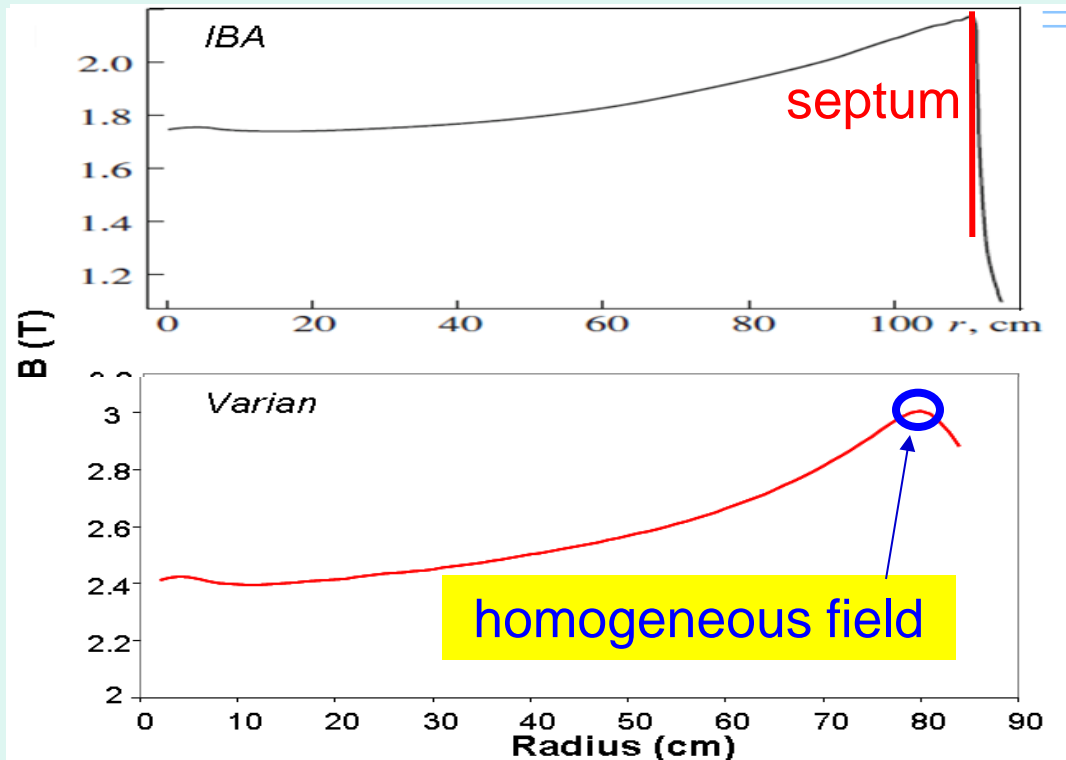


currently only possible  
with a **cyclotron**

# Extraction from cyclotron



- IBA and SHI: elliptical pole gap
- ⇒ Fast field drop at outer radius
- ⇒ Cathode + weaker field quickly pull the beam „out“

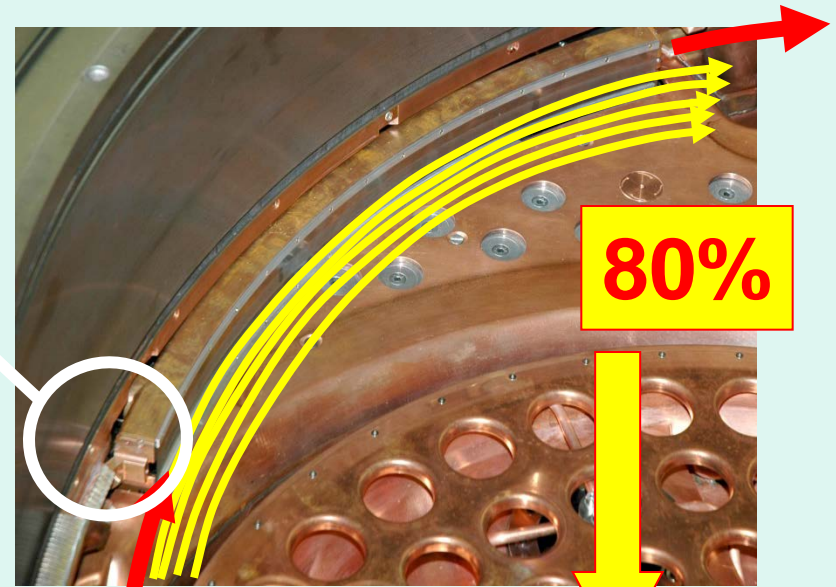
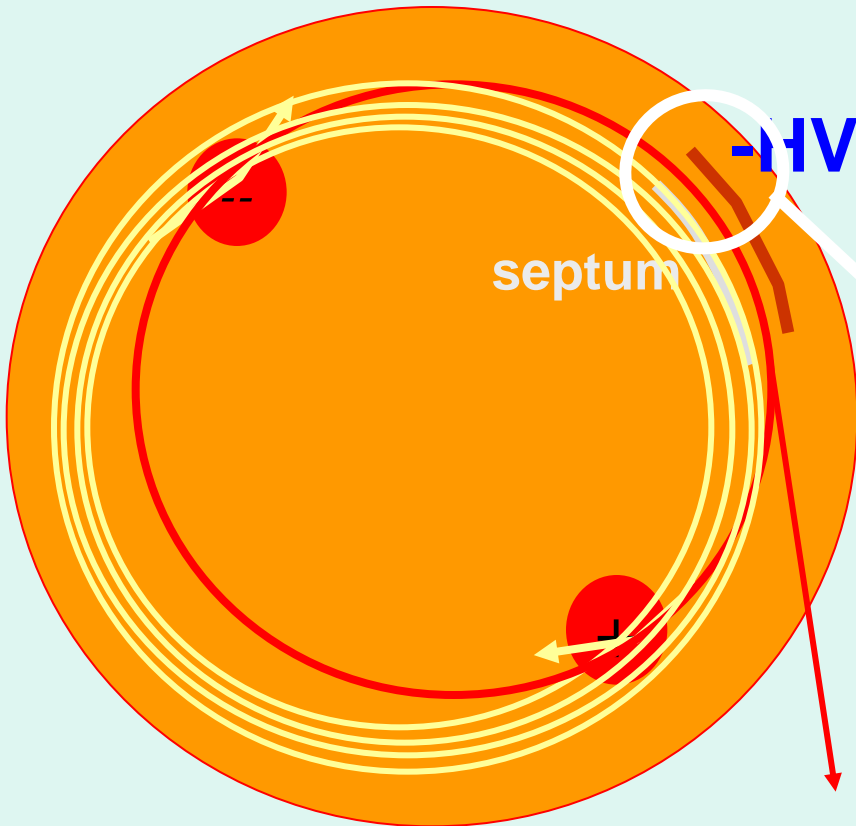
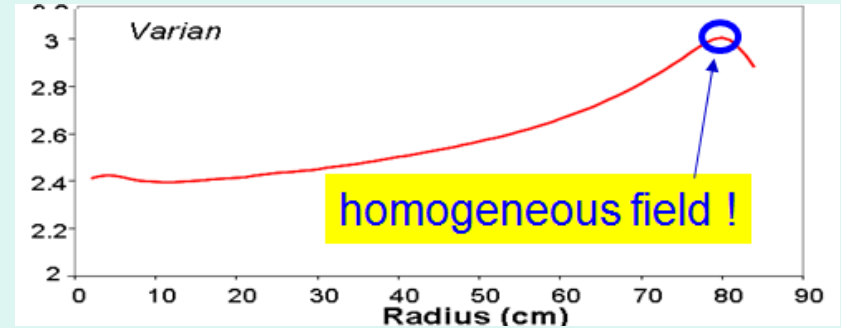


- Varian:
- flat poles & stronger field
- ⇒ Other method required

## Resonant extraction

uses homogeneous field !

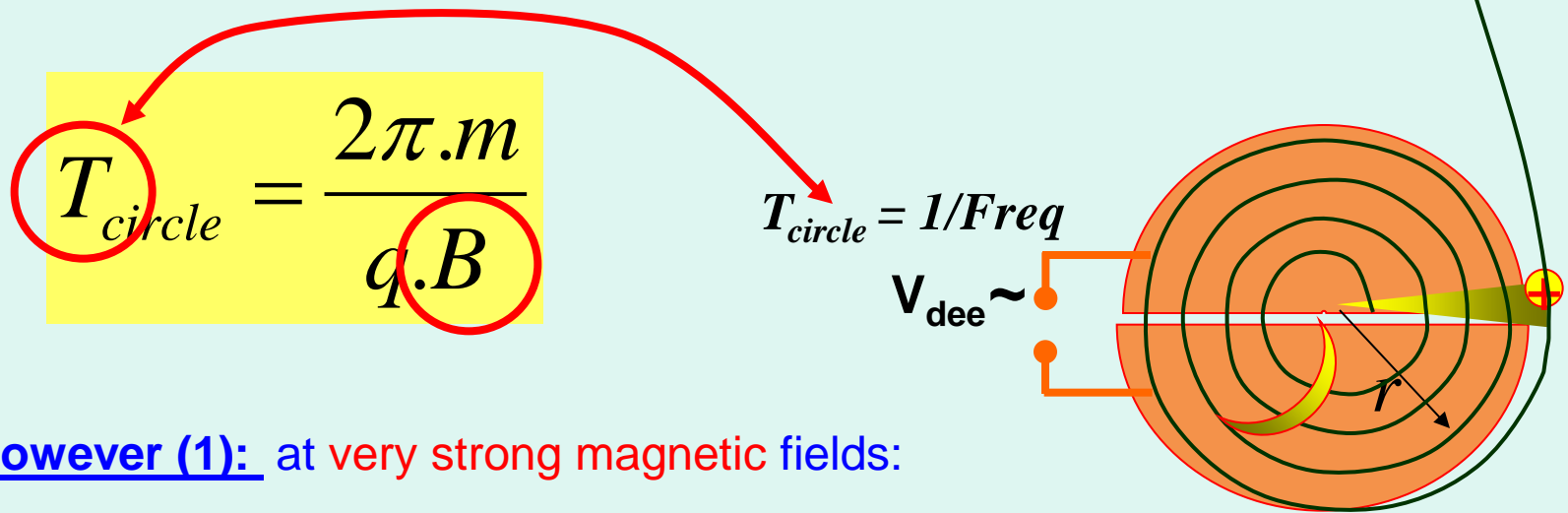
→ Field bump shifts beam:



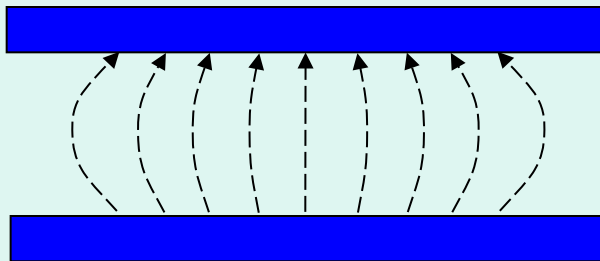
*Low radioactivity*



**Cyclotron works while:**  $T_{circle}$  independent from radius:  
(particles move in pace with  $V_{dee}$ )



**However (1):** at very strong magnetic fields:



$m$  = mass  
 $B$  = magnetic field  
 $q$  = charge

$\Rightarrow$  Magnetic field decreases with radius  $\Rightarrow T_{circle} \uparrow$

**stronger magn.fields → Smaller machines !**

Remedy to **compensate**

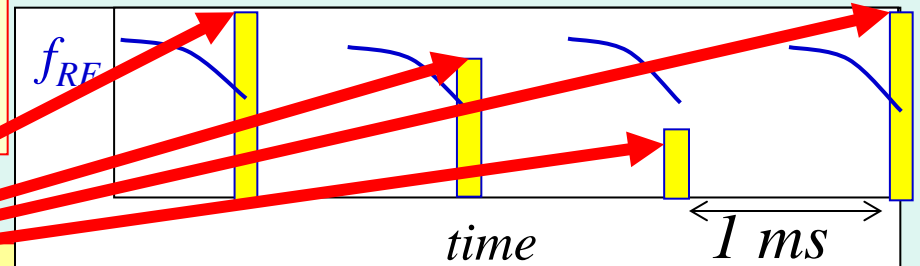
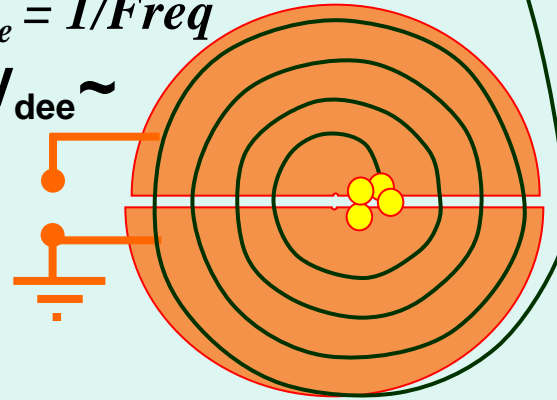
increase of  $T_{circle}$  :

Decrease  $f_{RF}$  with radius and extract

Repeat 1000 x per sec

$$T_{circle} = 1/Freq$$

$$\sim V_{dee} \sim$$



Each pulse: set intensity at source **within ms**

(=> typ 10-30% accuracy)

=> Spot scanning requires >2 pulses per spot.

## Proposal of

*H. Blosser, F. Marti, et al., 1989:*

- 250 MeV
- SC, 52 tons, **on a gantry**
- $B(0)=5.5$  Tesla

*H. Blosser, NSCL (~1990):*

SC-cyclotron for **neutron therapy**;  
30 MeV p, mounted on a gantry in Detroit

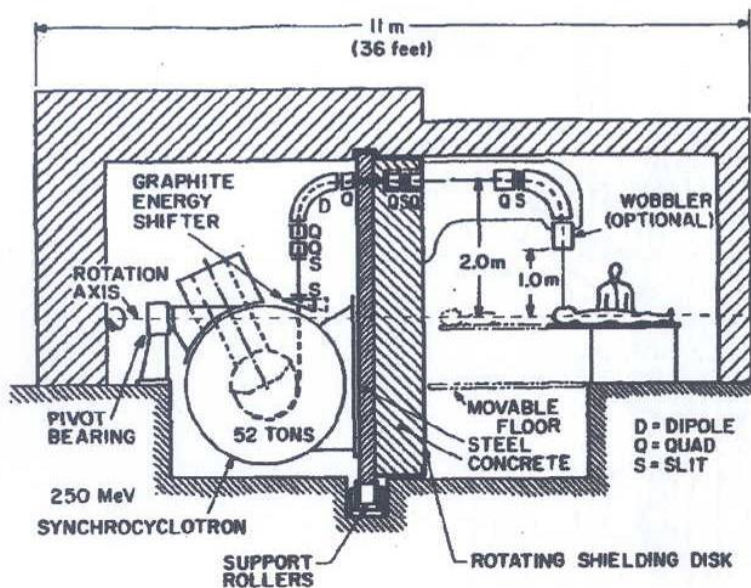


FIG. 9 -- Drawing showing synchrocyclotron rotating gantry arrangement with energy shifting wedge just after the cyclotron. Energy shifting can optionally be accomplished just ahead of the patient.

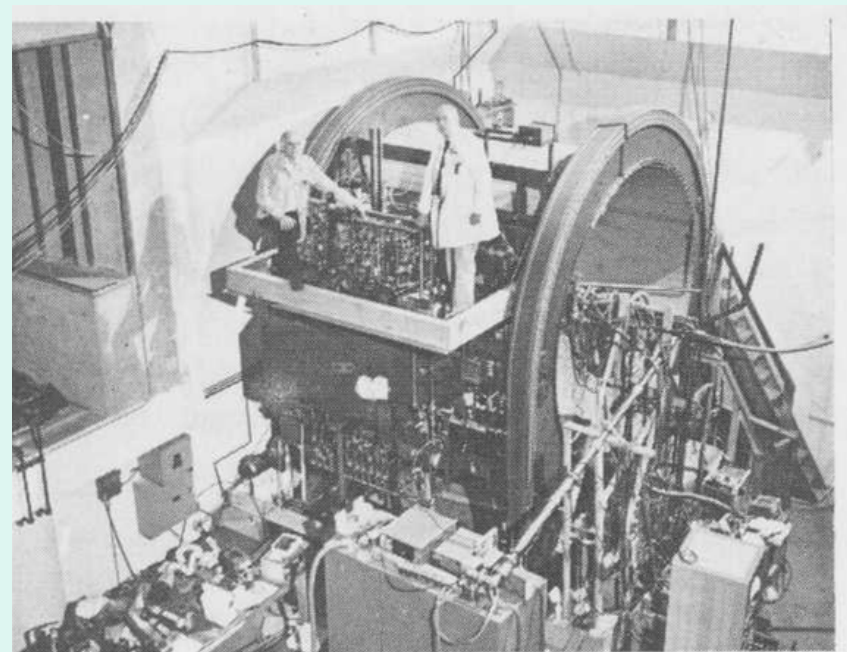


Fig. 2 Photo of the superconducting medical cyclotron on its gantry. Dr. William Powers and

# Synchro-Cyclotron



First beam extracted in May 2010



First beam at IBA in 2013

	(syn-)cyclotron	synchrotron
--	-----------------	-------------

Carbon ions	in development	easy
Change particle	in development	easy
Time structure	continuous(SC:pulsed)	spills
Fast E-scanning	degrader	next spill +developm.
Activation degrader	to be shielded	no
Intensity	“any”(SC:low),	limited, per spill
Intensity stability	3-5%	15-20% +developm
Size $\varnothing$	3.5 - 5 m ( <b>SC&lt;2</b> )	6-8 m ( C: 25 m)
Scattering	ok	ok
Spot scanning	<b>ok</b> (SC: >2 pulses/spot)	<b>ok</b>
Fast continuous scanning	<b>ok</b> (SC: no)	difficult

New types of accelerators, e.g.:

FFAG, Linac based acc, Laser, Laser-Plasma ....

## Great developments

But do **not** only **check** price!

**BASIS of  
Particle Th.**

- treatment quality  $\geq$  now ?
- organisation:  
medical device, service, upgrades

