

PAUL SCHERRER INSTITUT



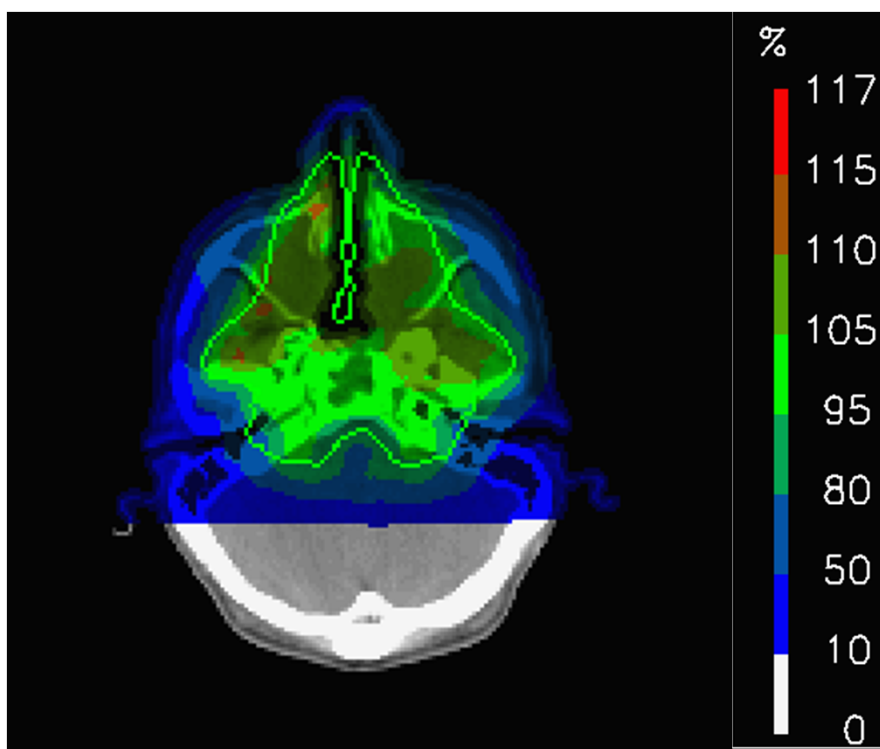
To promote excellency in patient care and innovative proton treatment

Paul Scherrer Institut

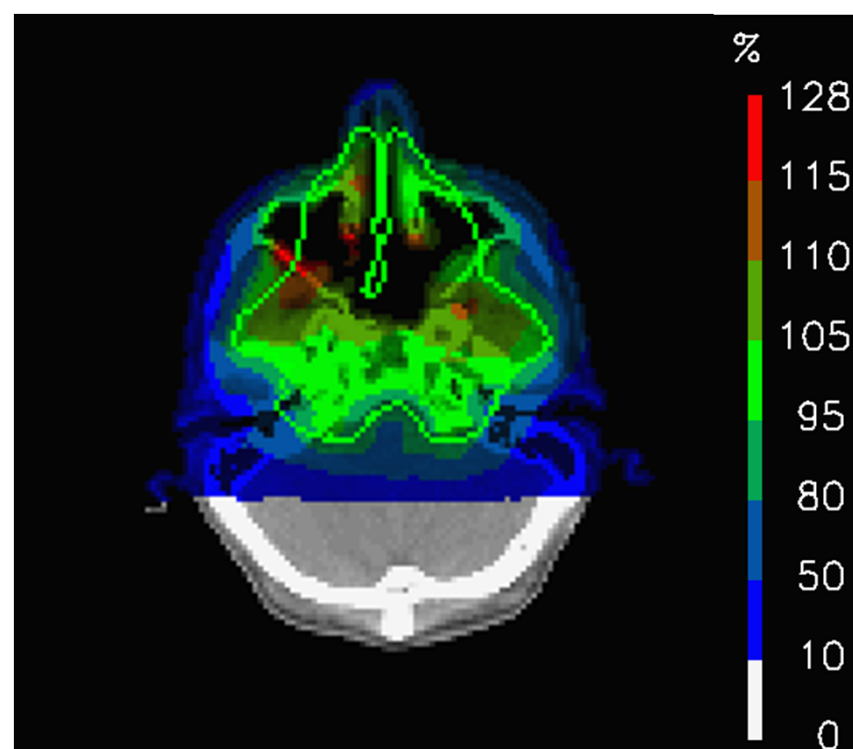
A.Bolsi

Uncertainties in the clinical practice

Nominal



Delivered on a single fraction



There are different kind of uncertainties:

a) Density uncertainties

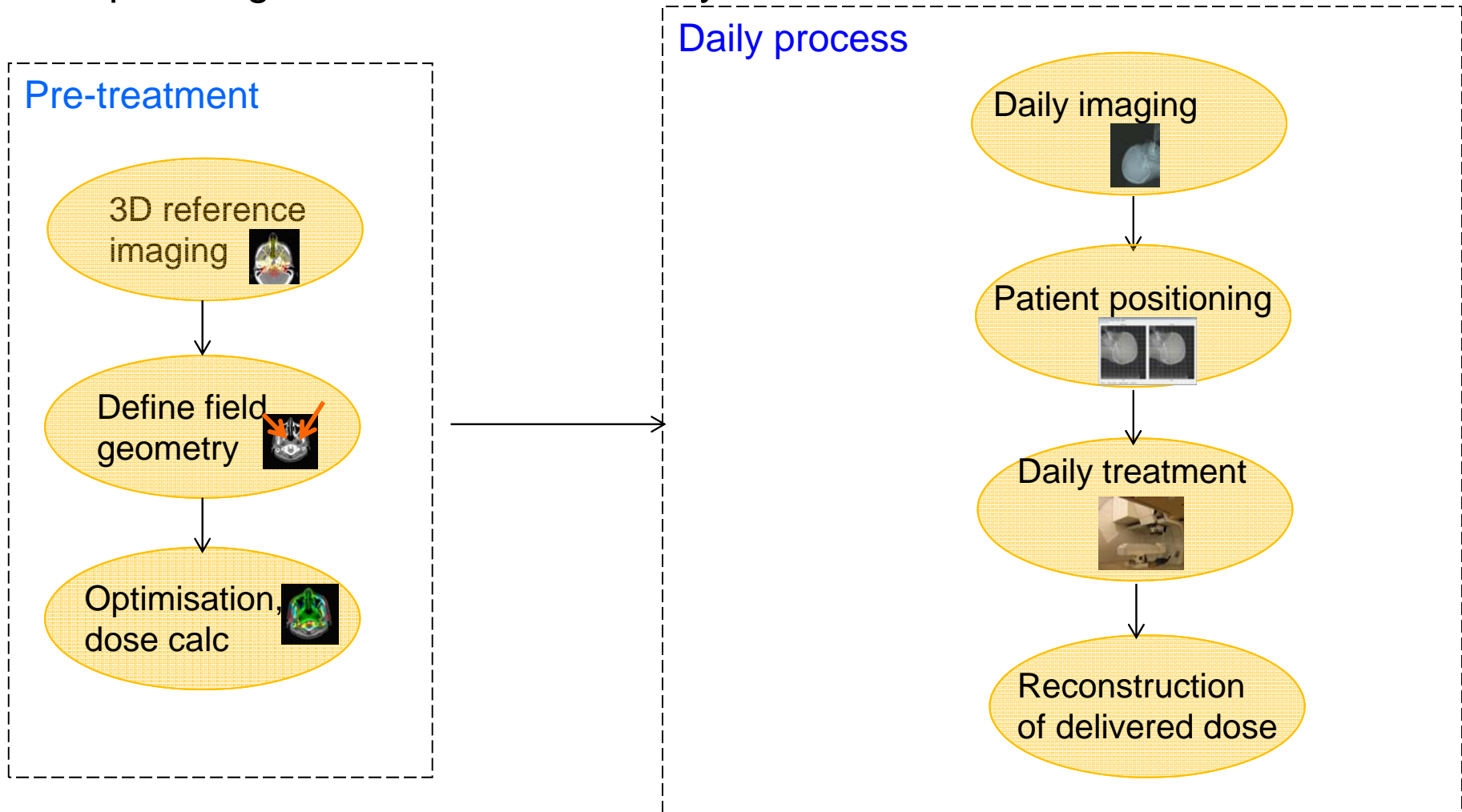
b) Range uncertainties

c) Set up uncertainties

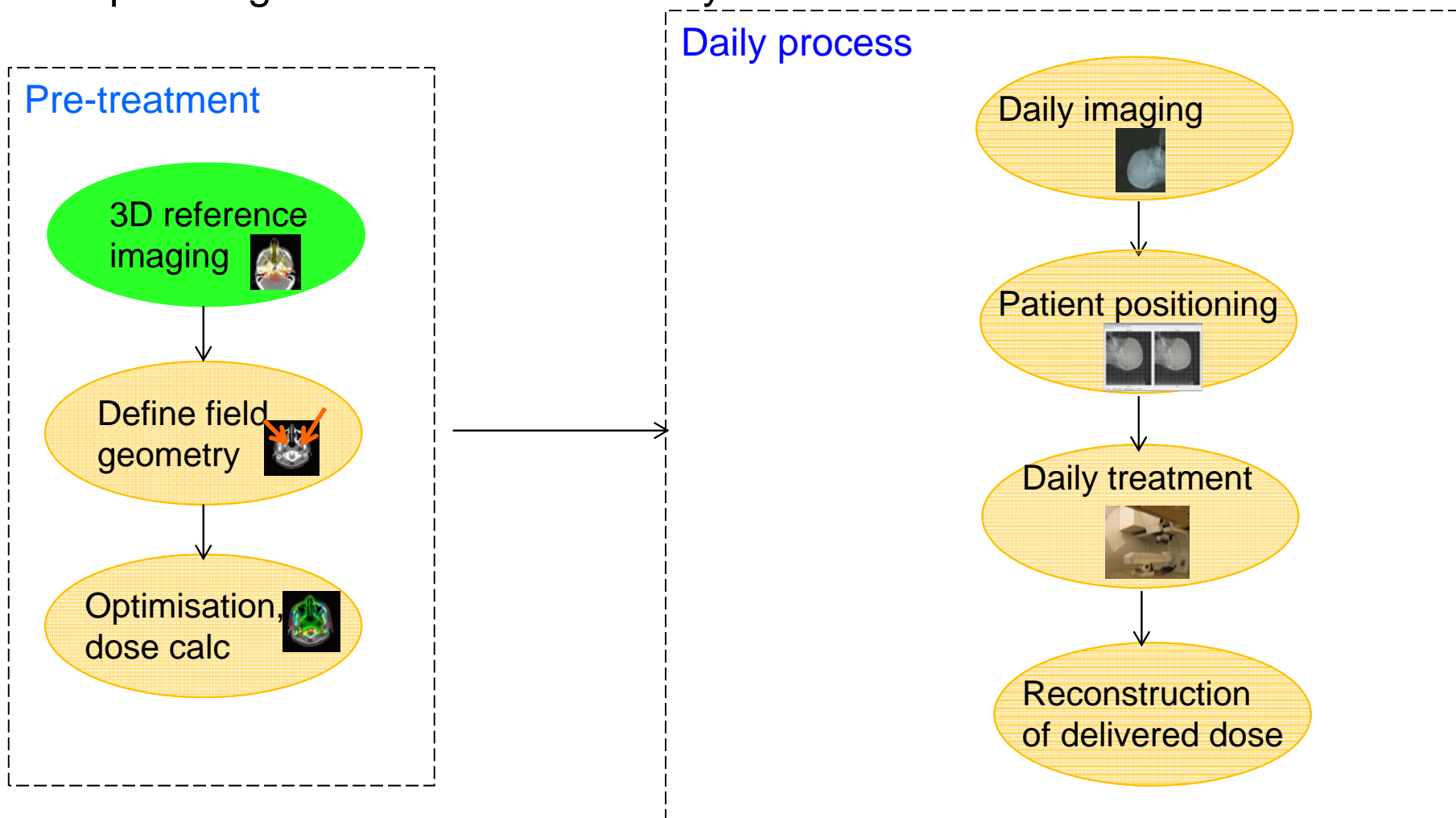
d) RBE

e) Beam delivery

They can appear in different step of the entire radiotherapy workflow:
from planning CT to the dose delivery.

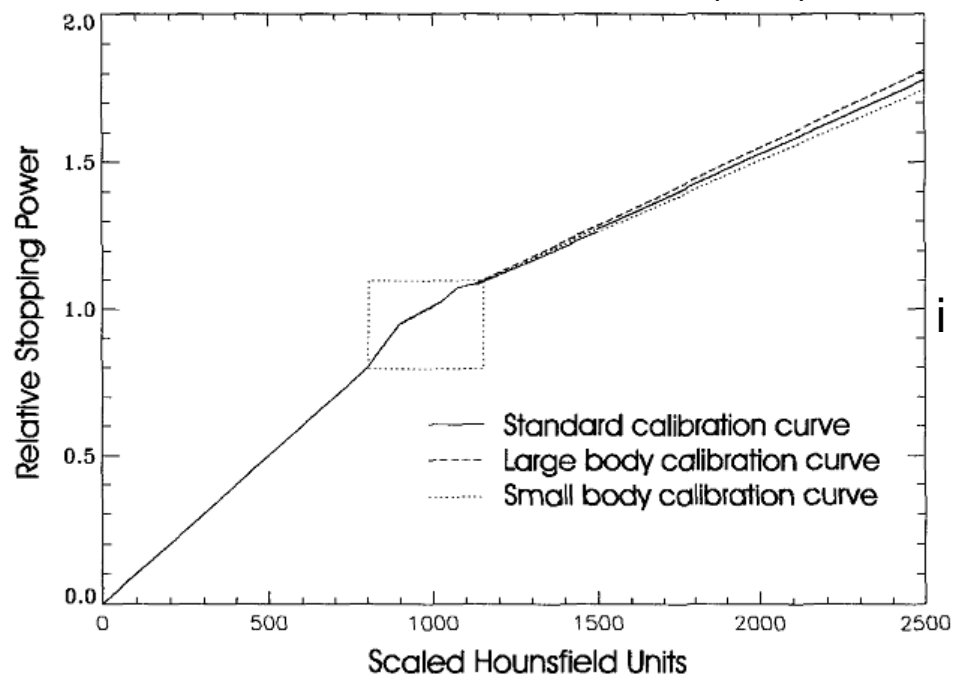


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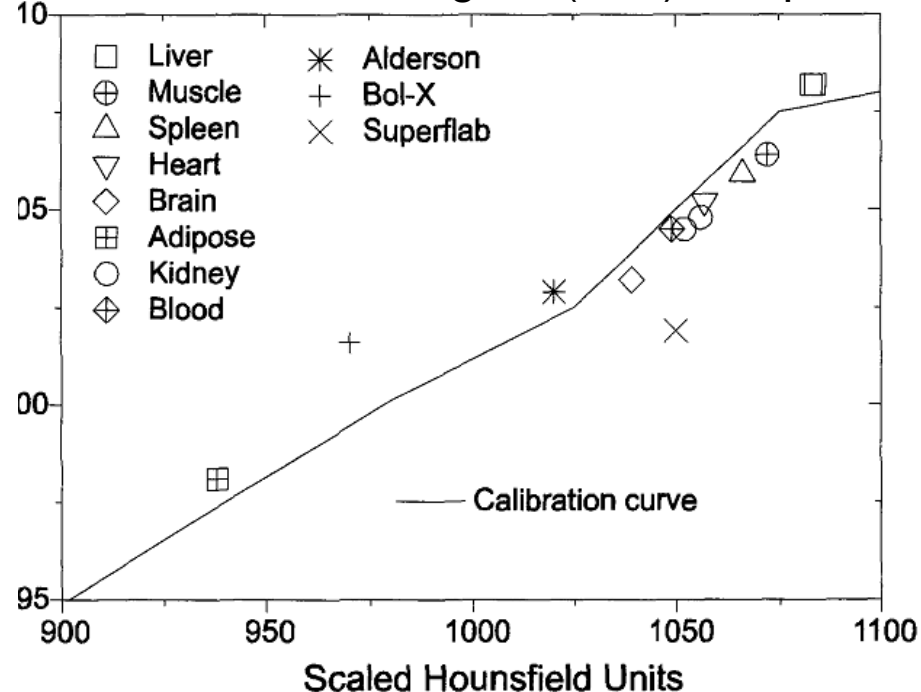


Inherent CT uncertainties: calibration from HU to RPSP

Stoichiometric calibration (PSI)¹



Validation with biological (cow) samples²



~1% range uncertainties through soft tissues, ~2% through bone
 ~1.5mm range uncertainty in brain, ~3.5mm for prostate (lateral beams)

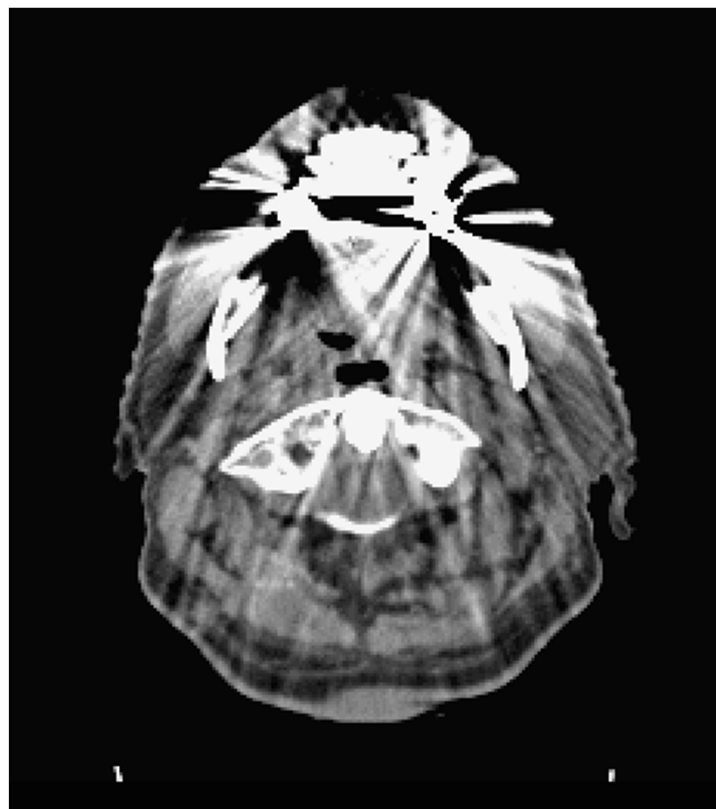
¹Schneider et al. 1996, ²Schaffner and Pedroni 1998

CT artifacts can compromise CT data quality

Artefacts along the spinal cord due to titanium implants



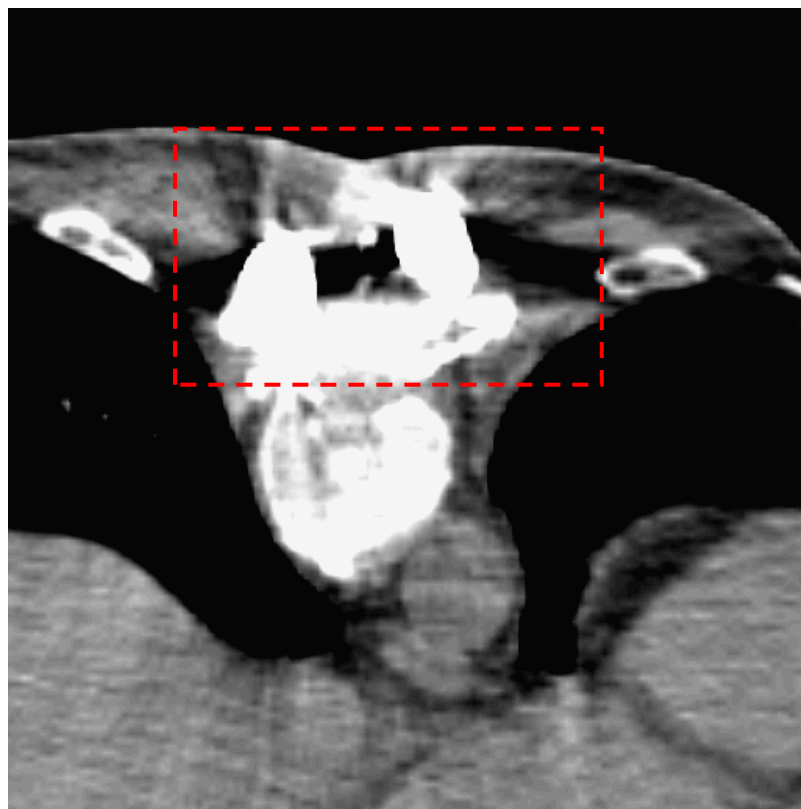
Artefacts due to metal implants in the Teeth (normally not titanium)



CT artifacts : how we can deal with them

CT data set with artefacts

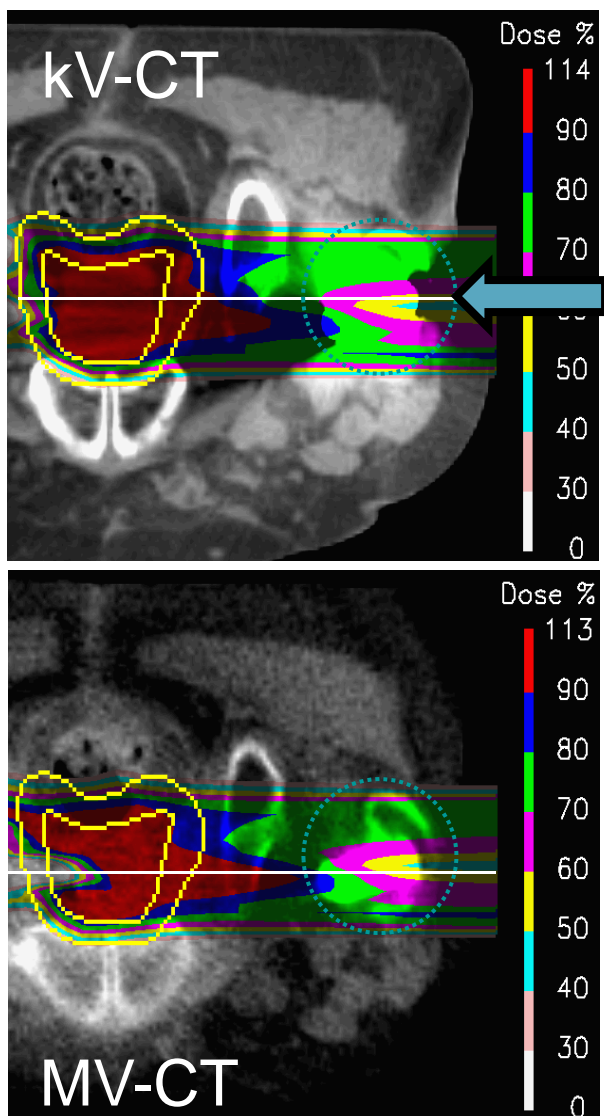
→ Manual delineation of the soft tissue areas, HU substituted



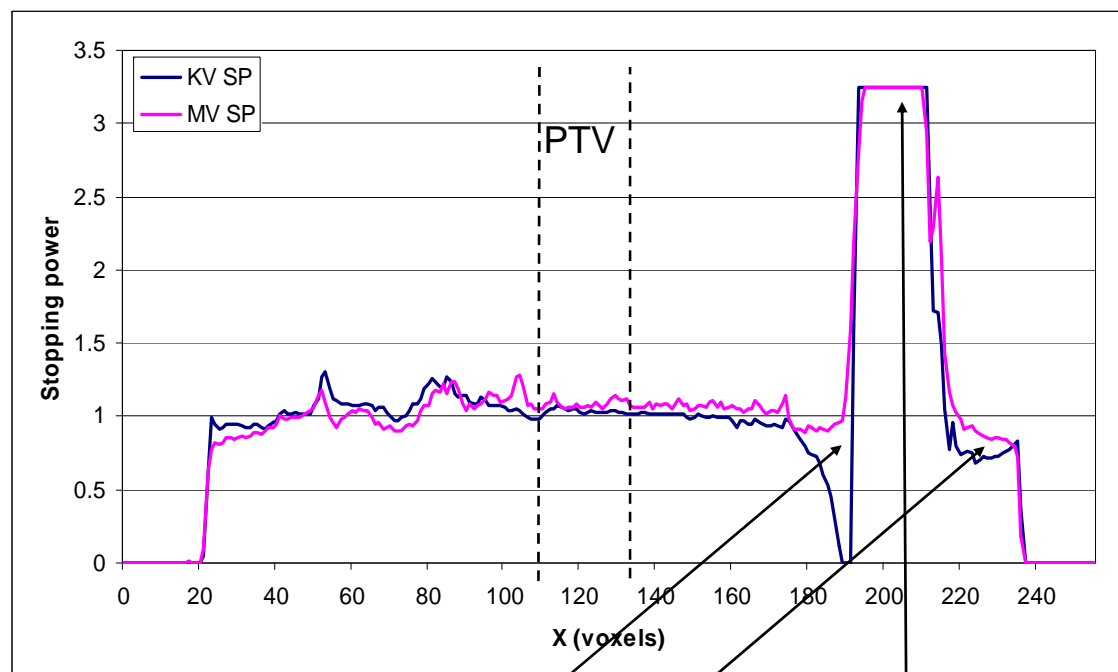
Additionally: beam hardening effect, noise and resolution.

Planning CT errors: they are systematic and contribute to range uncertainties.

Single field trough the metal implant: extreme case



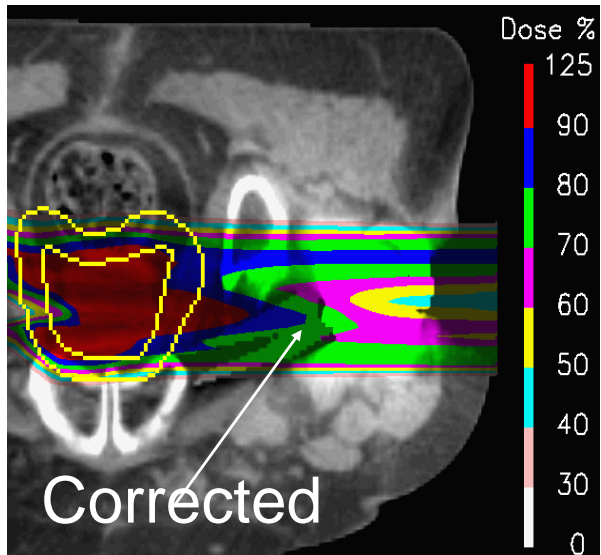
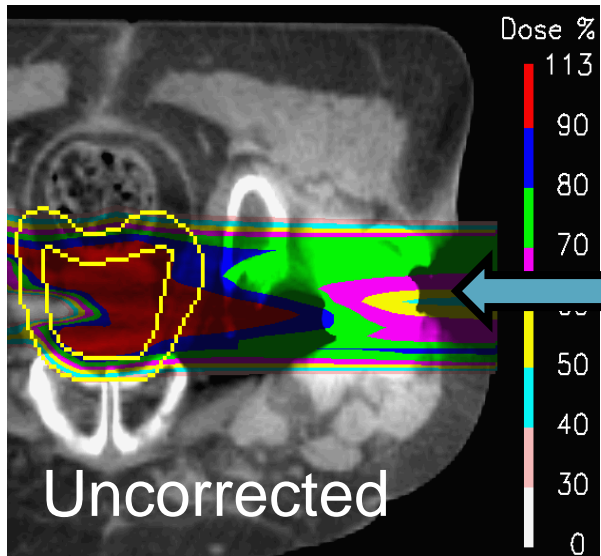
Stopping power profiles



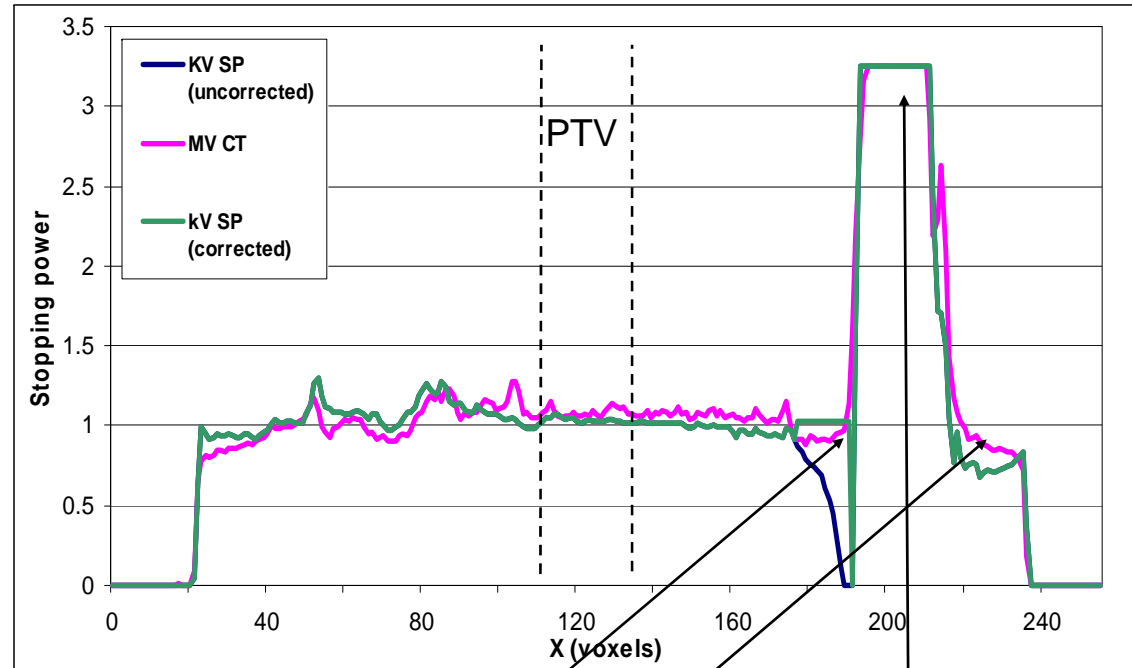
kV-CT artifacts

Prosthesis

Single field trough the metal implant: extreme case



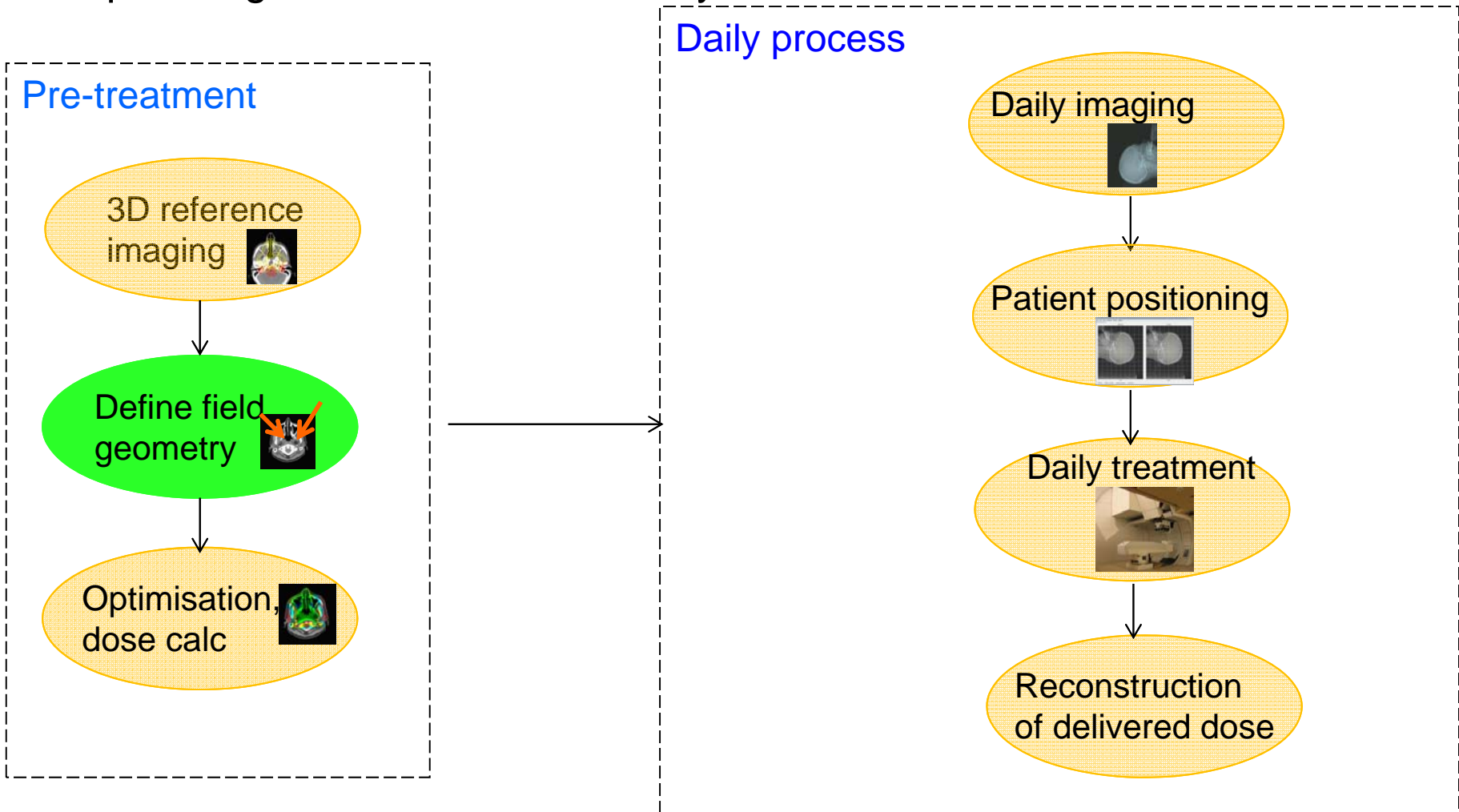
Stopping power profiles



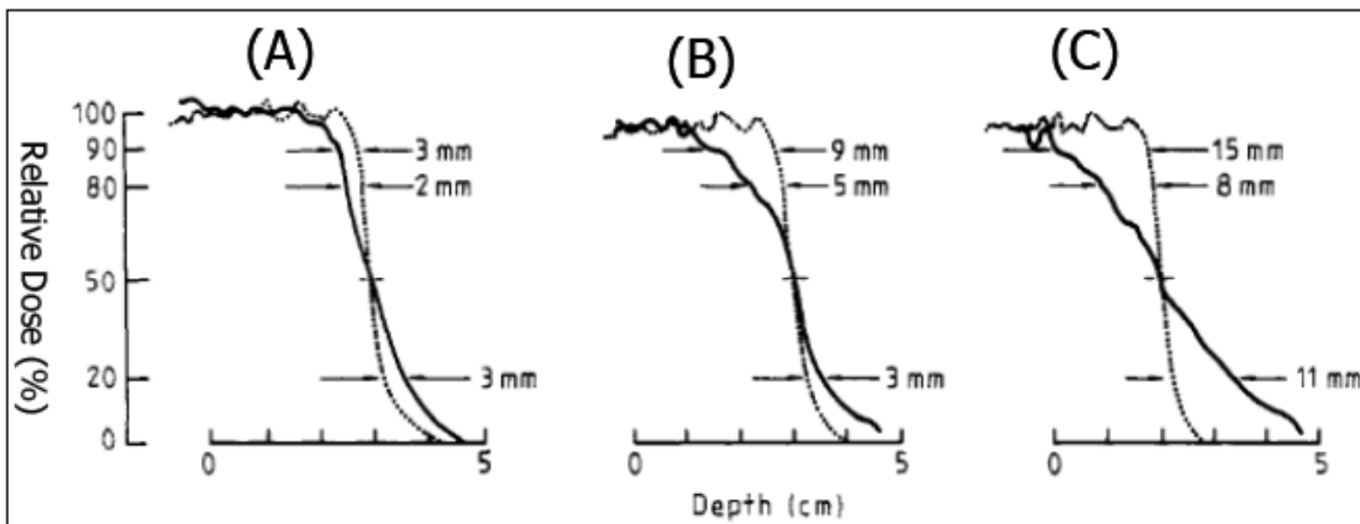
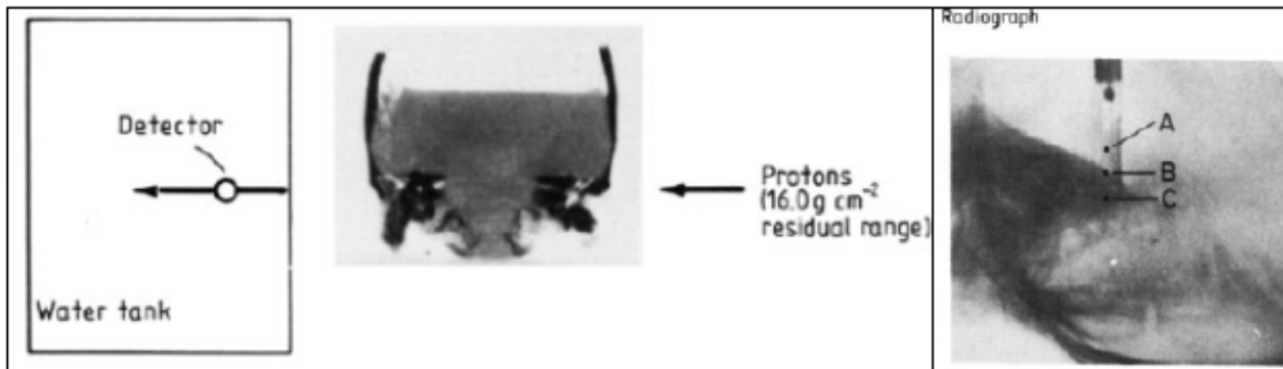
kV-CT artifacts

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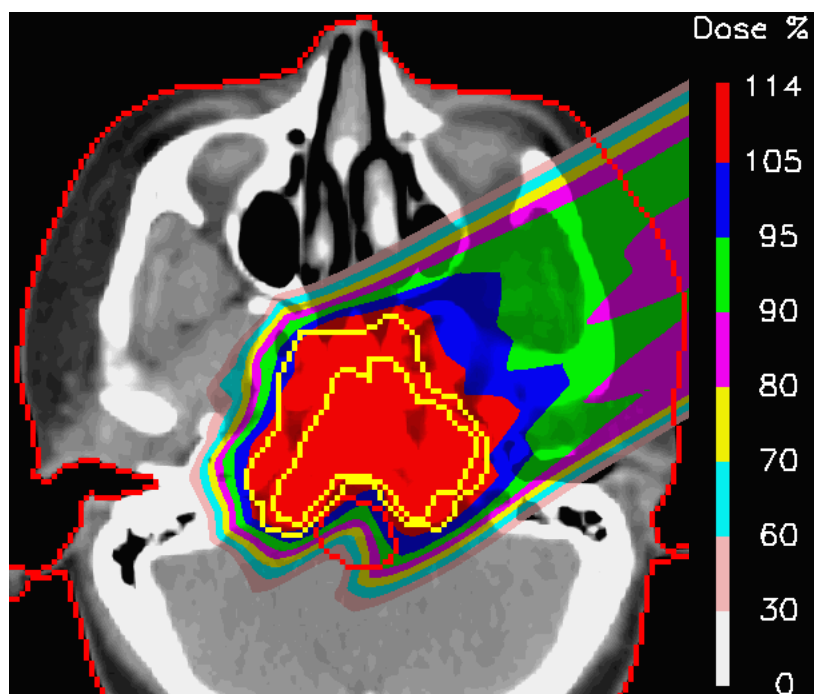


Density heterogeneities: degradation of the Bragg peak shape

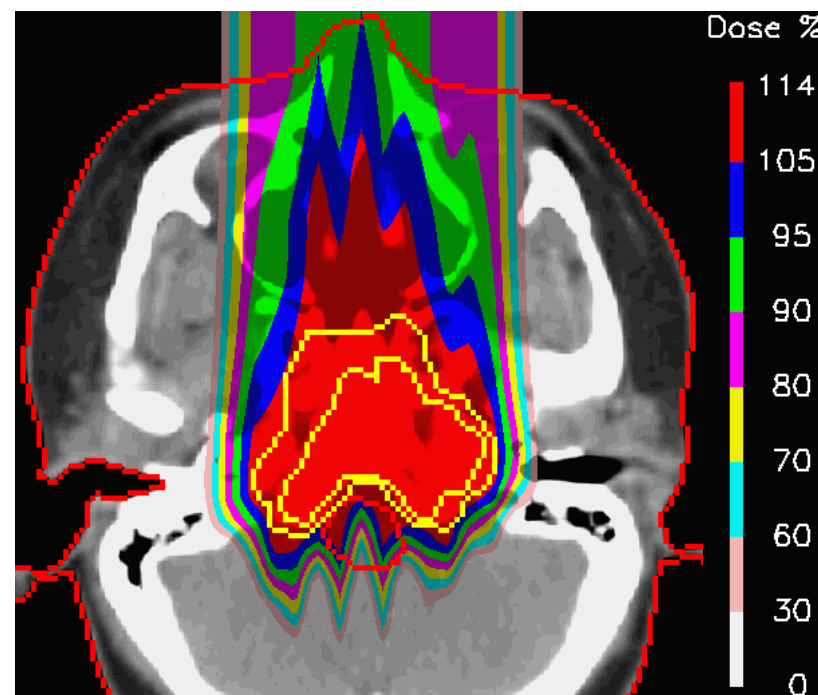


Protons Through Base of Skull: 90 to 20% fall of increases from 6 to 32 mm

Example field through relatively homogenous anatomy

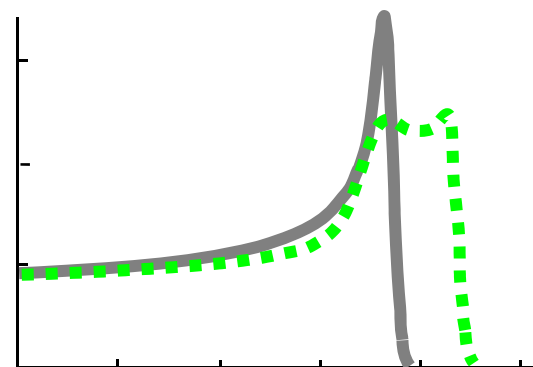
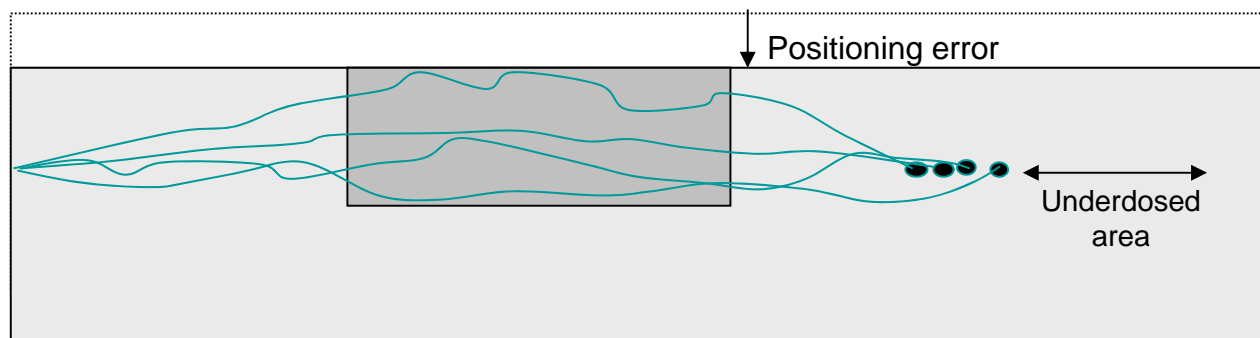
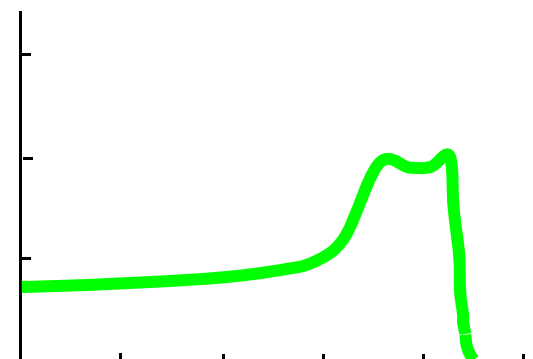
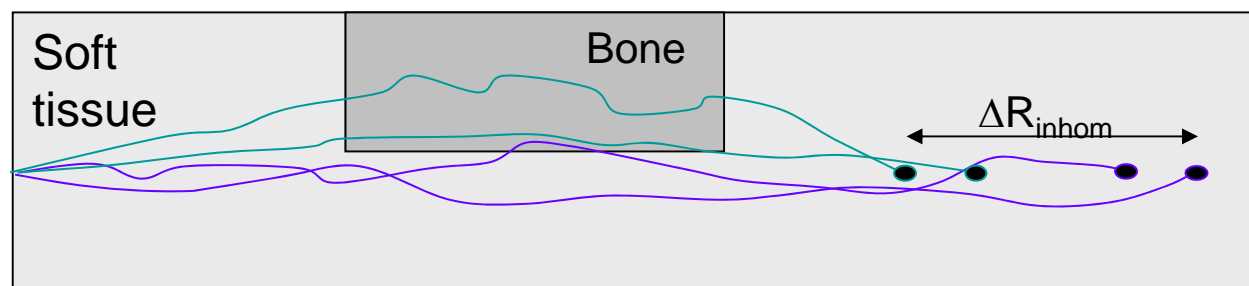


Example field through very inhomogenous anatomy

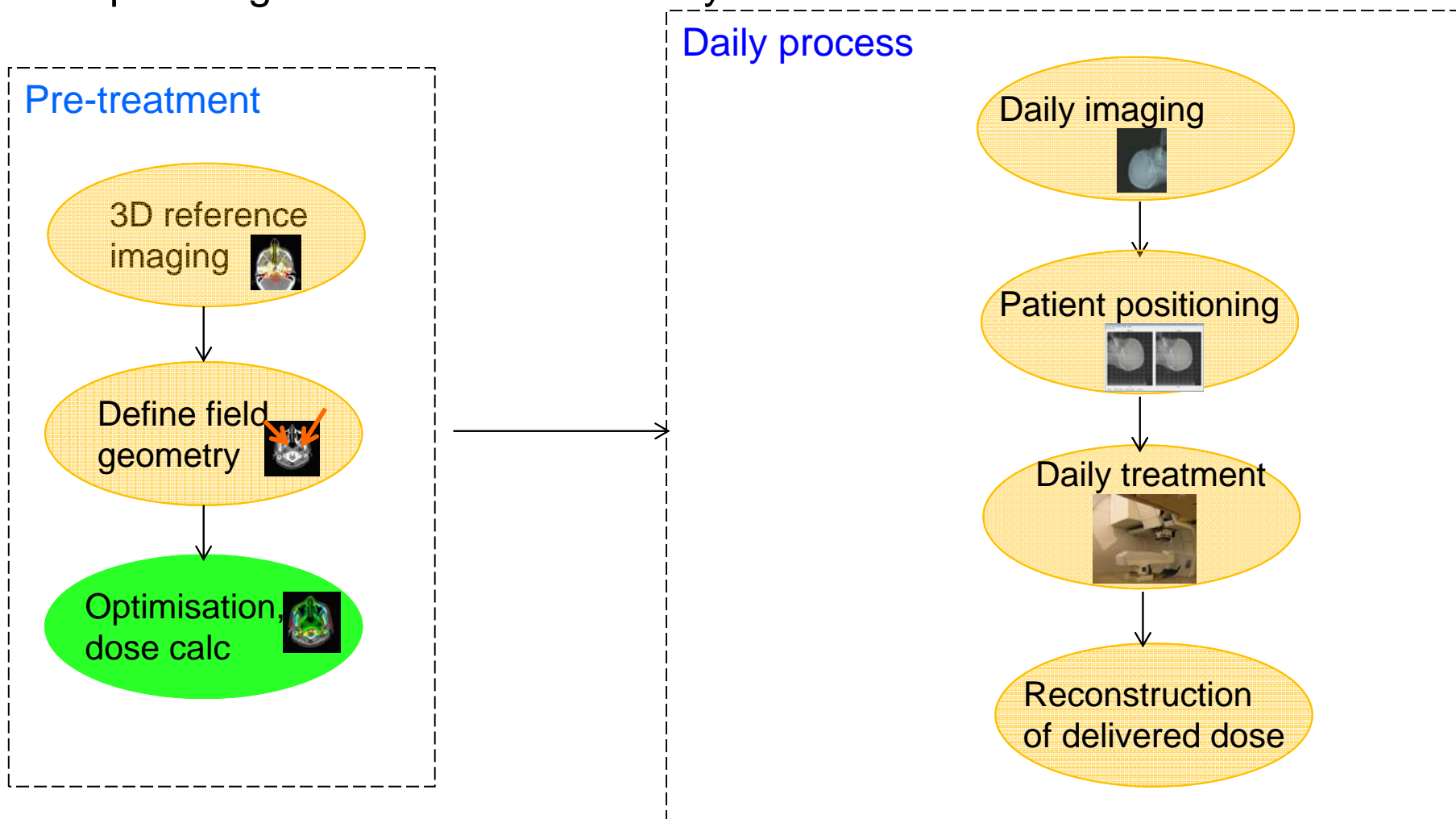


When planning it is important to select field directions which go through the minimum possible in-homogeneities.

They play also a role when we come to the positioning process

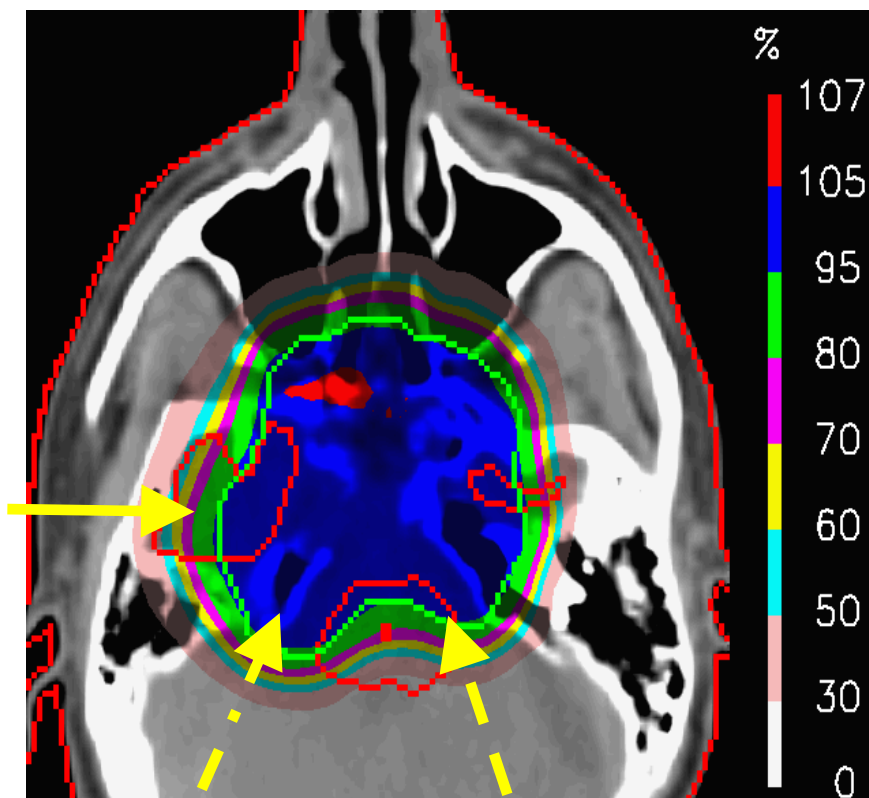


They can appear in different step of the entire radiotherapy workflow:
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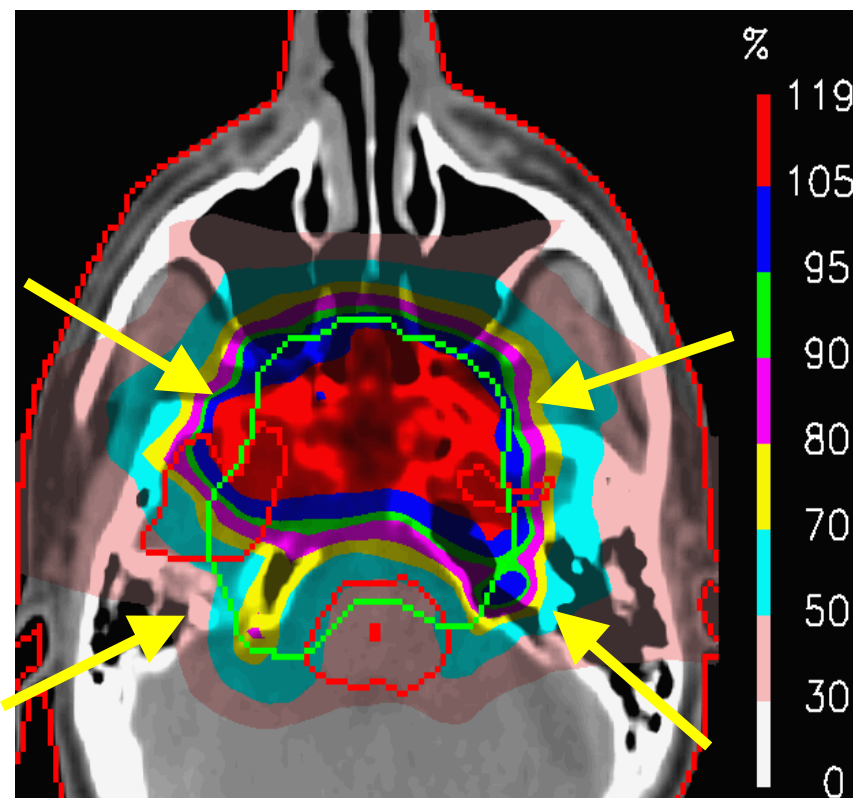


SFUD vs IMPT plans

SFUD



IMPT

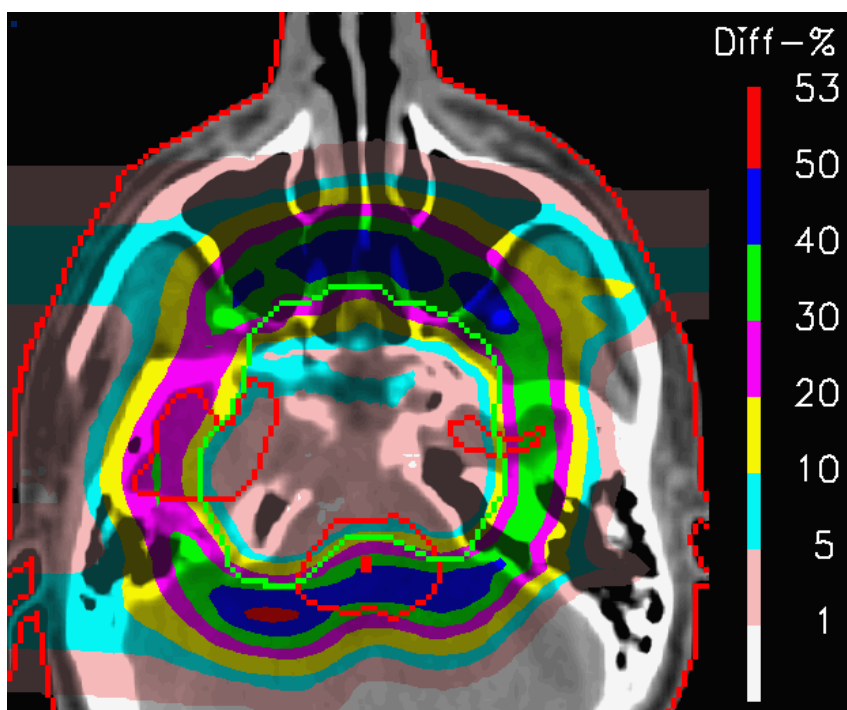


SFUD plans are generally more robust than the IMPT plans (highly inhomogeneous individual dose distribution are 'patched' inside the target volume)

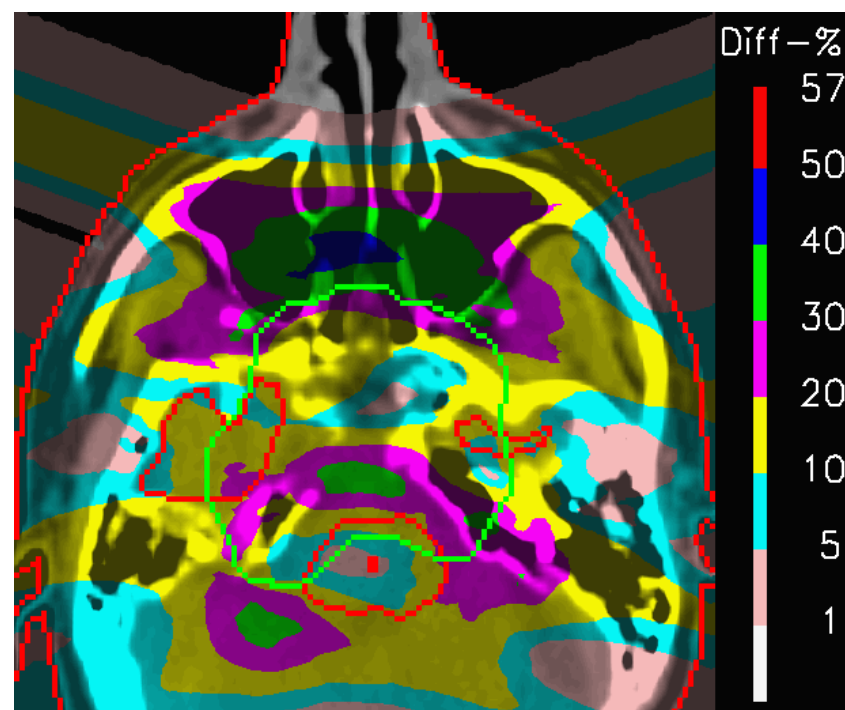
Evaluating uncertainties: max to min dose distributions

This indicates the maximum differences (~ error bars) expected in the plan due to set up errors (Albertini F. et al. Phys Med Biol. 2011)

SFUD



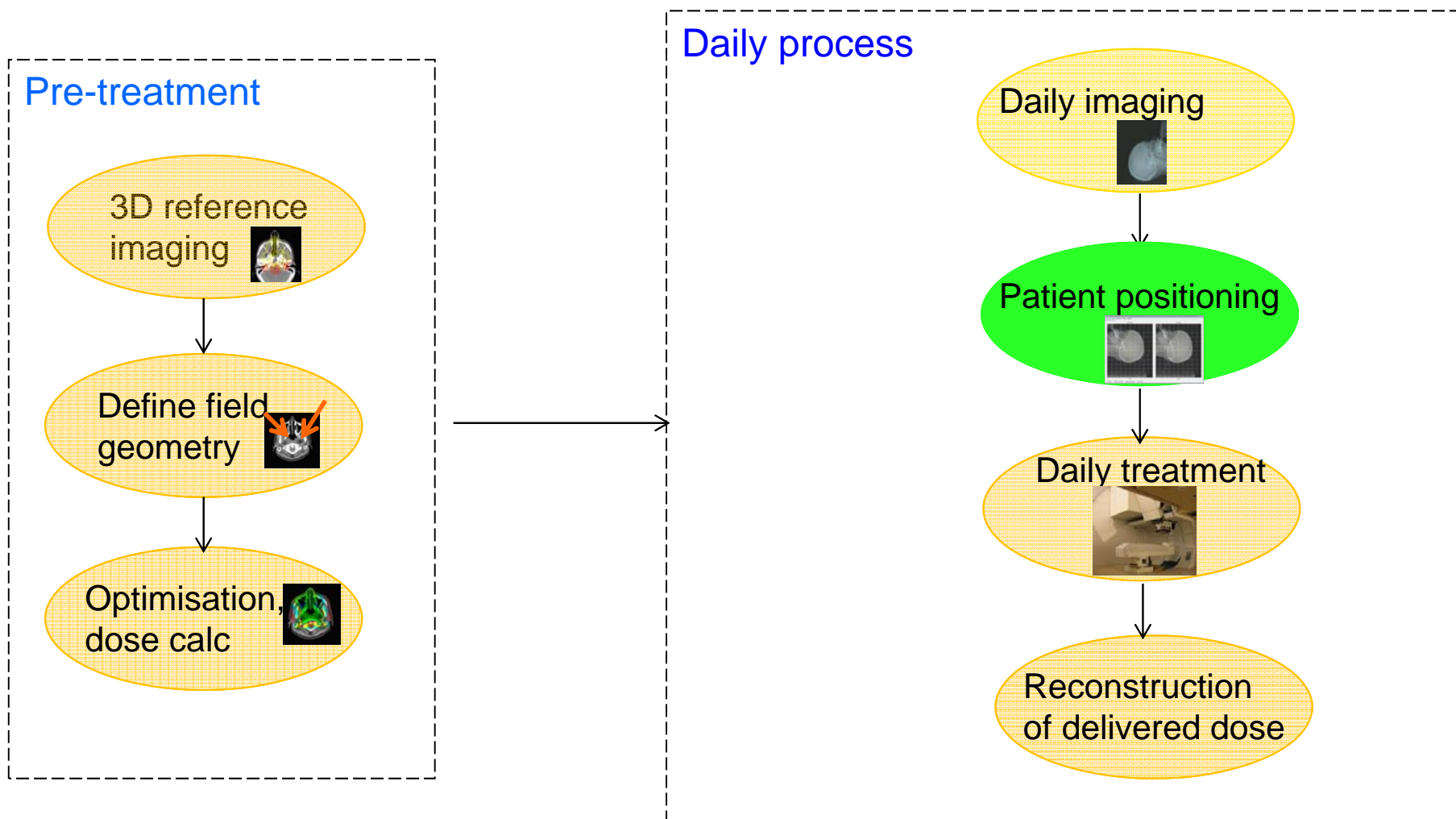
IMPT



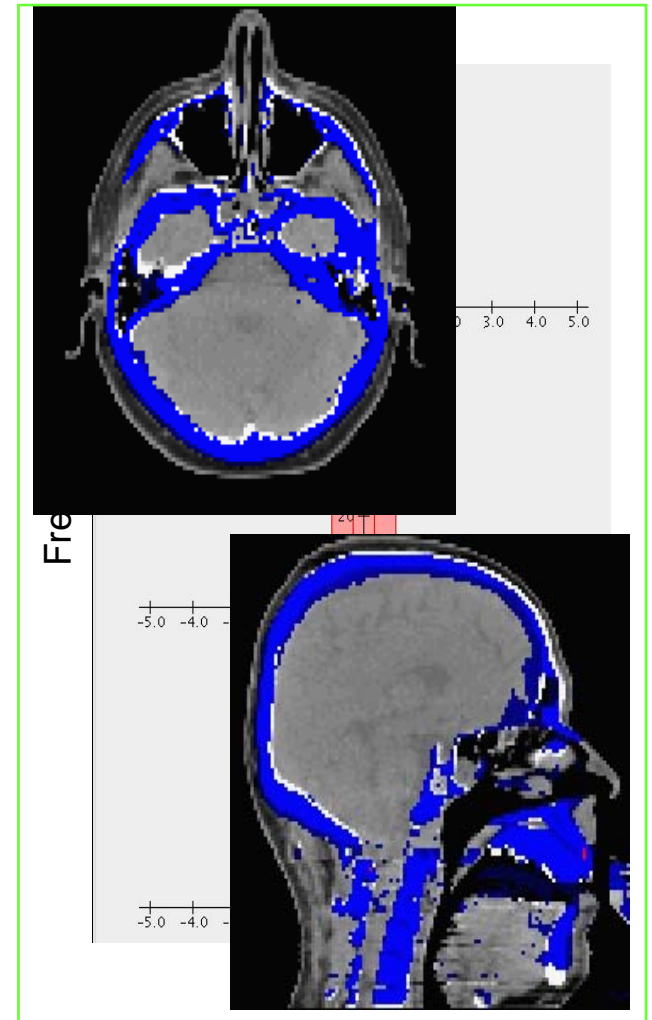
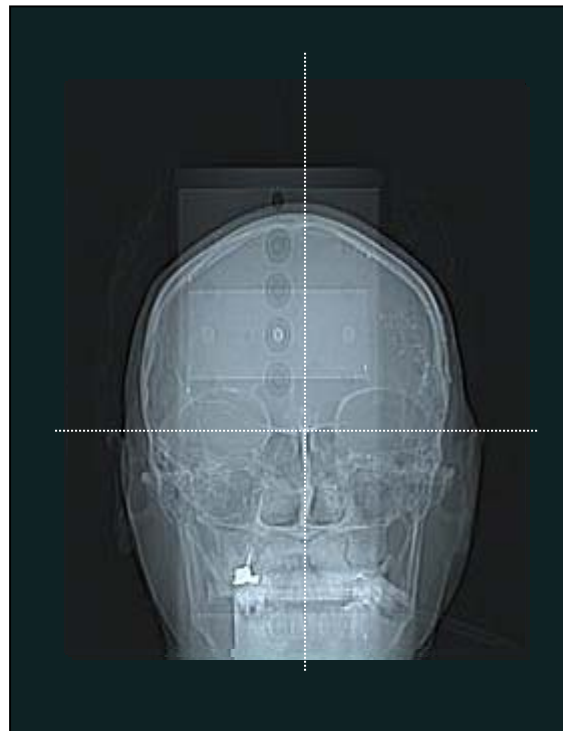
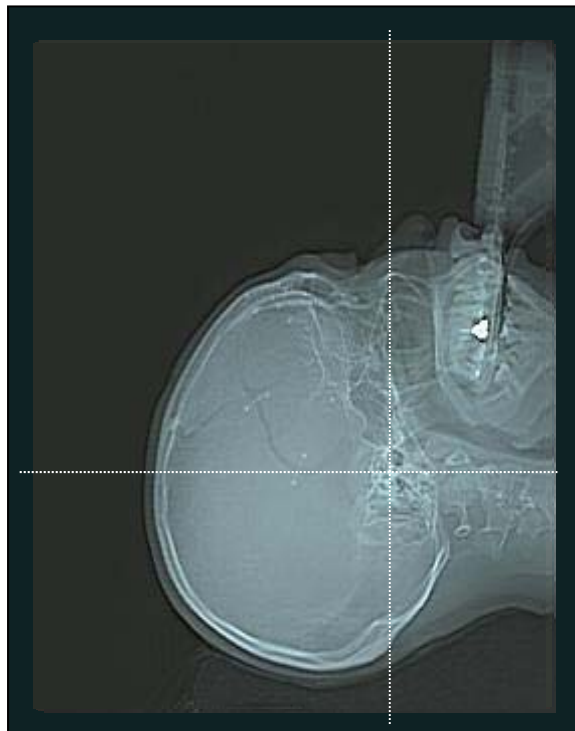
- SFUD more robust than IMPT in the target
- IMPT plan more robust for brainstem
- Margins increase robustness for SFUD, but not necessarily for IMPT.

Lowe et al "Incorporating the effect of fractionation in evaluating the robustness of proton plans to set-up uncertainties"

They can appear in different step of the entire radiotherapy workflow:
from planning CT to the dose delivery.

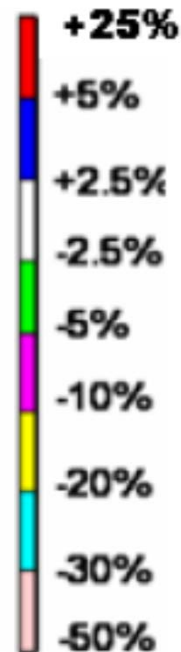
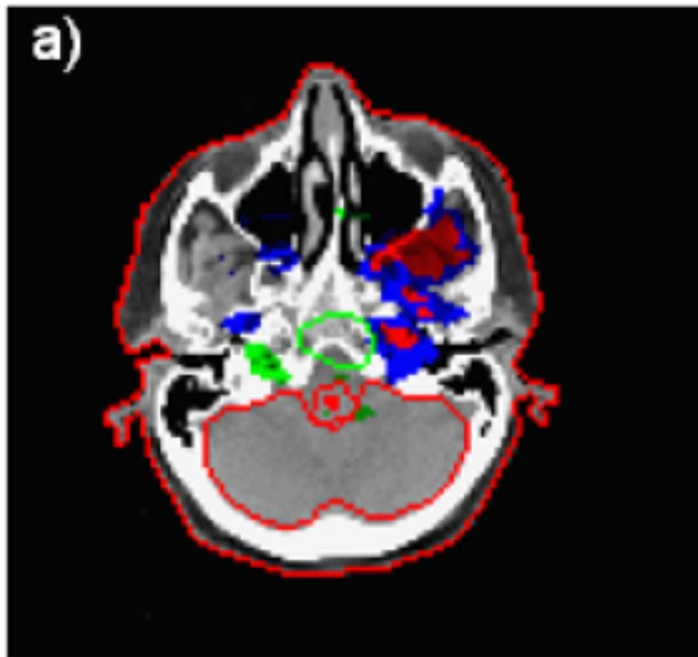


Daily positioning protocol significantly reduce patient misplacement

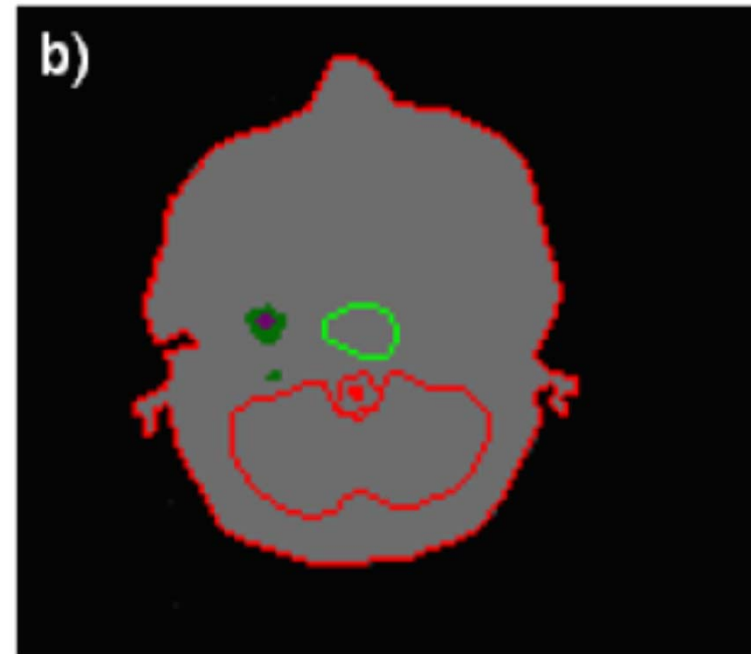


Set up errors combined with density heterogeneities

patient geometry

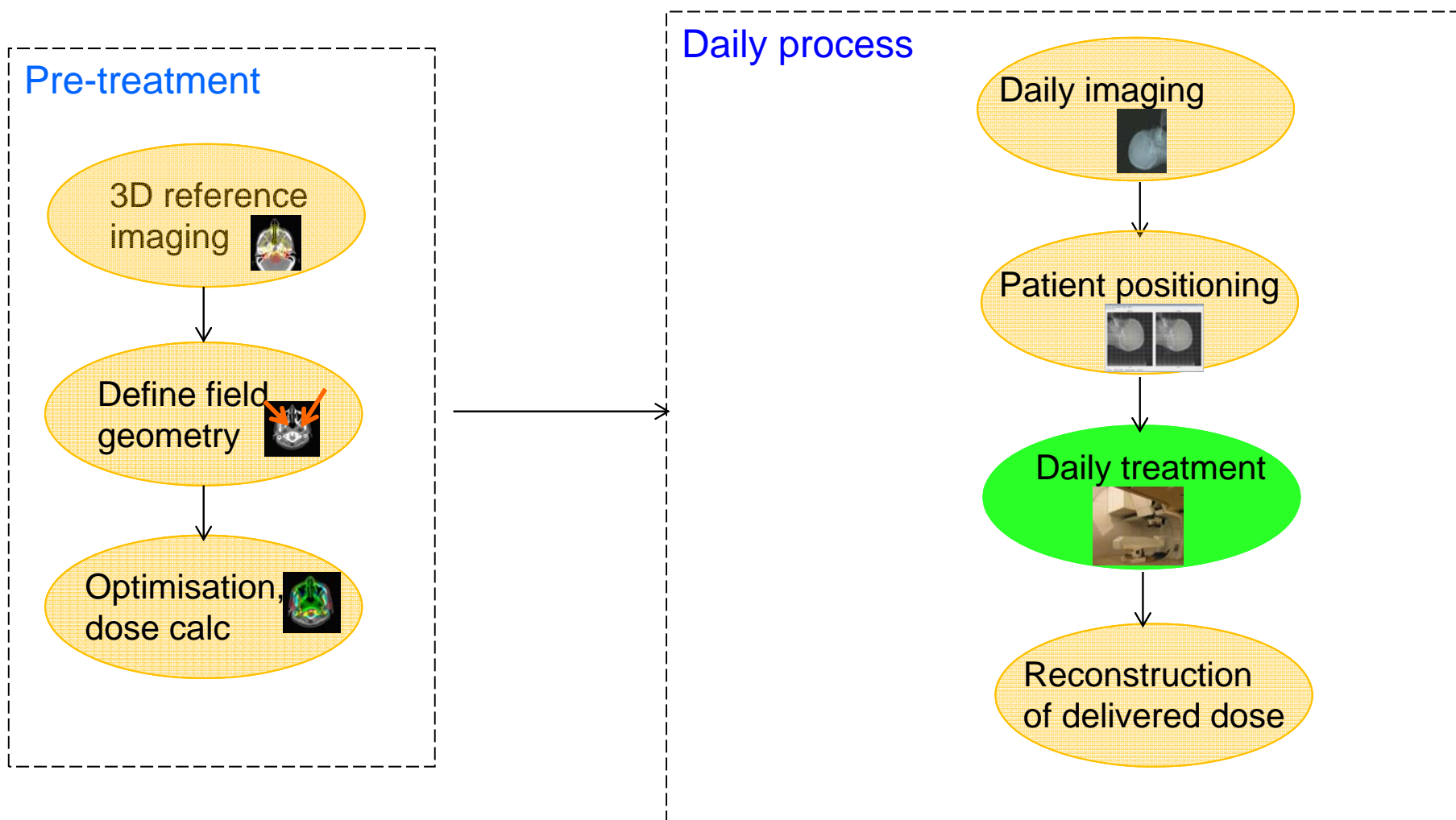


“water equivalent” patient



Even after image guided re-positioning, density heterogeneities can somewhat degrade the delivered dose due to residual positioning errors

They can appear in different step of the entire radiotherapy workflow:
from planning CT to the dose delivery.



Nasal cavity fillings

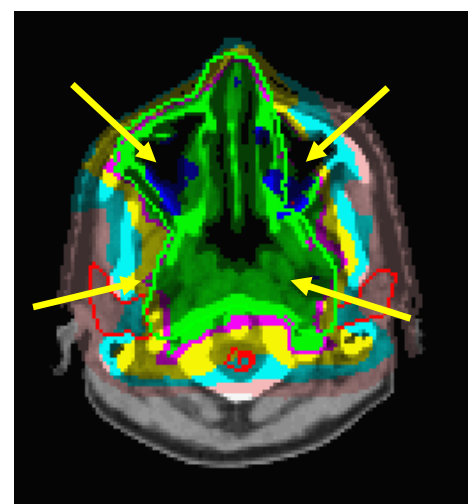
Planning CT



Repeated CT



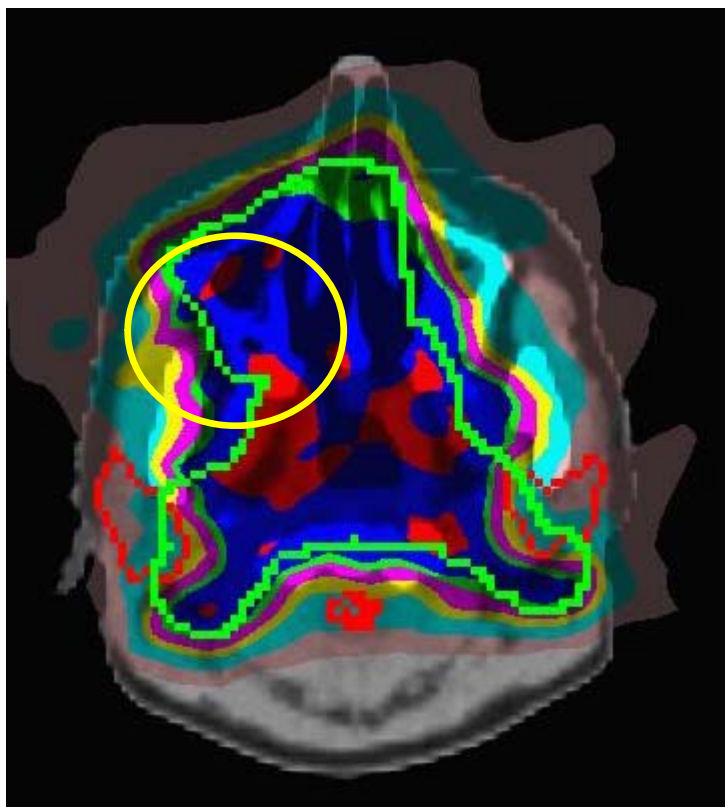
Nominal dose distribution



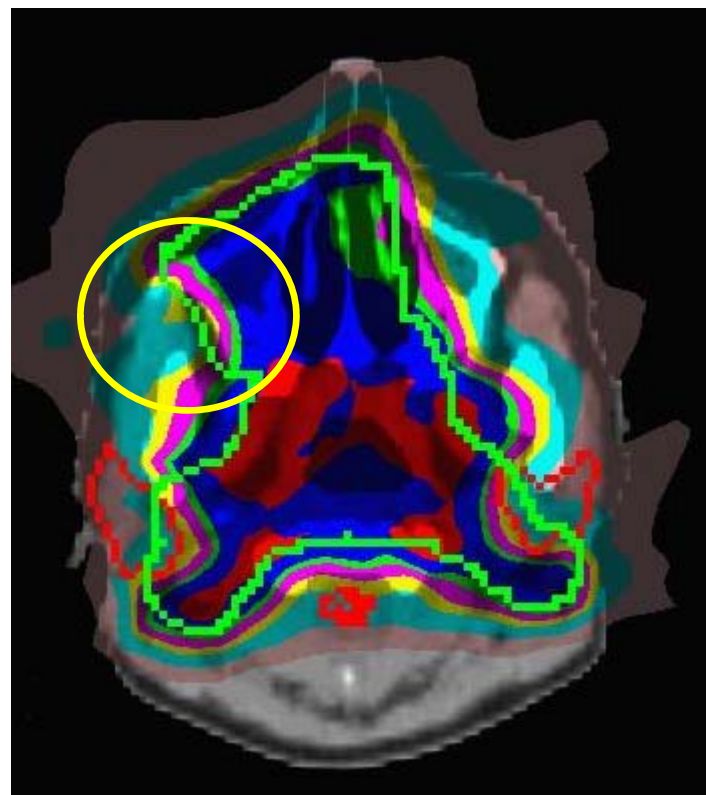
Every week the repeated CT slices acquired showed a significant different changing in the cavity fillings, with consequences on the delivered dose distributions.

Nasal cavity fillings

Nominal dose distribution (CTV in green, spinal cord in red)



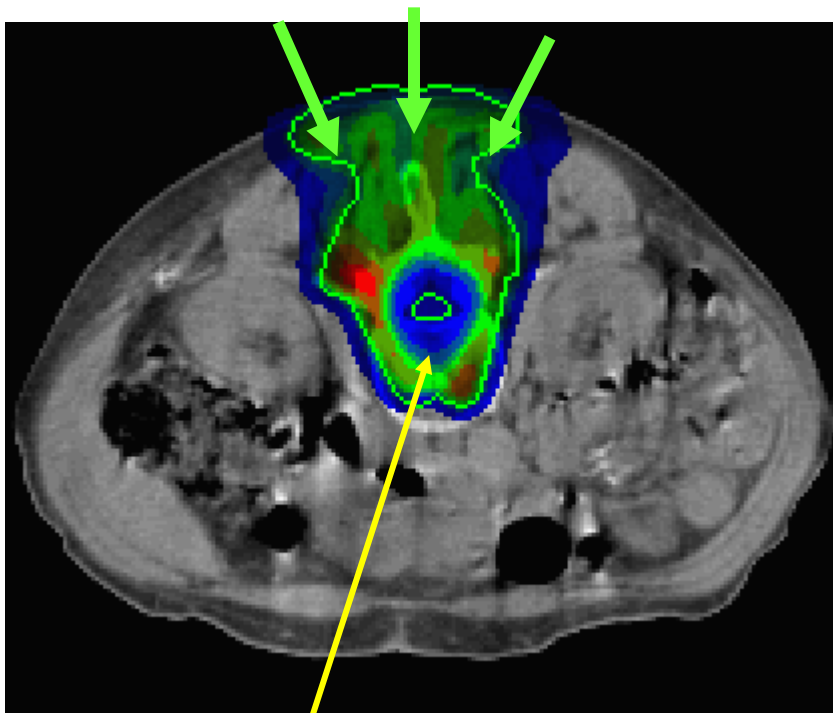
Recalculated dose distribution



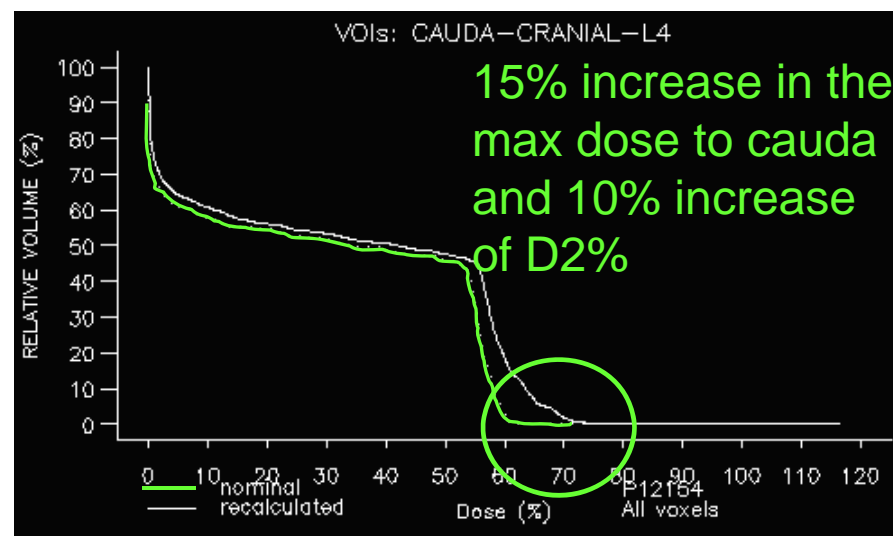
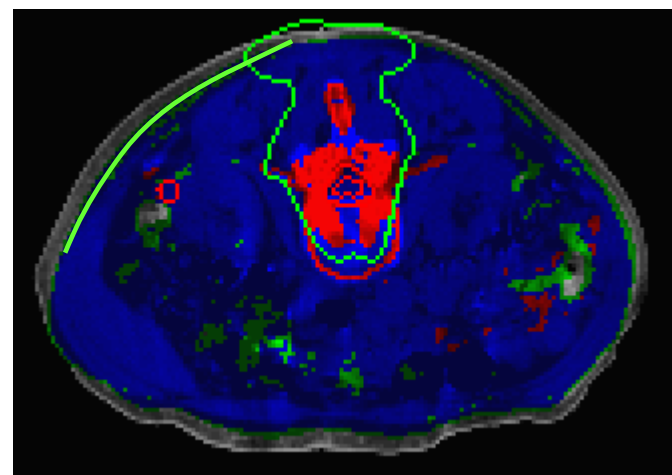
Placidi et al. "The effect of anatomical changes on PBS proton dose distributions: a retrospective review of 951 patients treated at PSI"

Weight changes

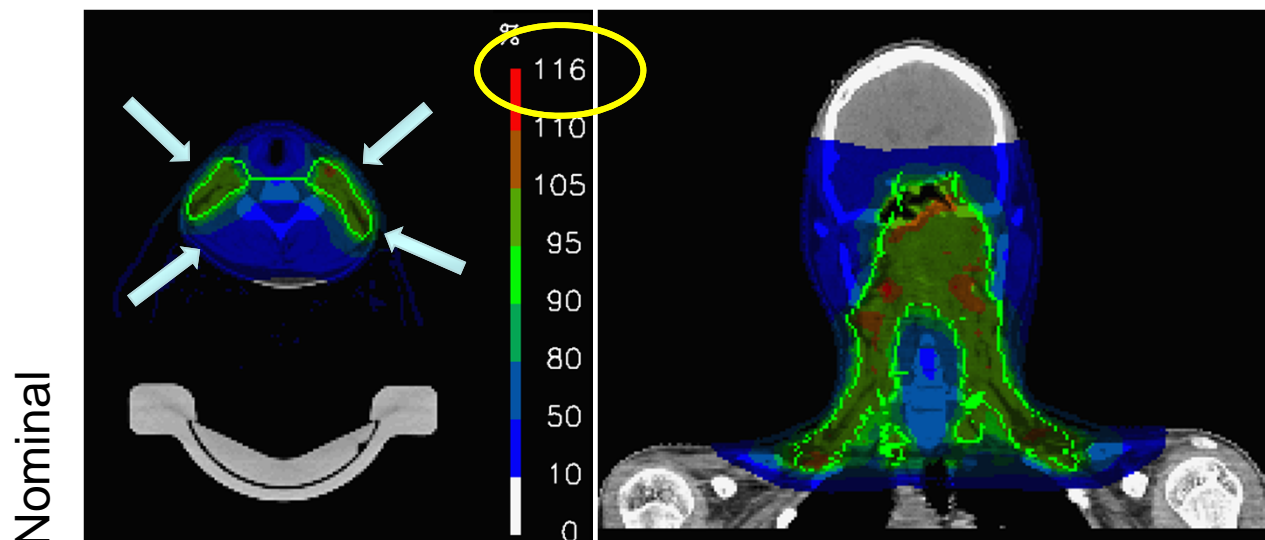
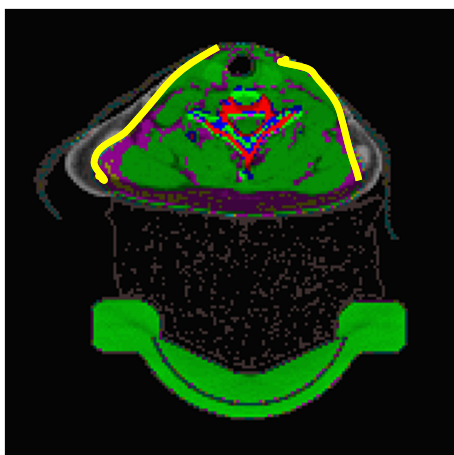
3 fields IMPT plan, pt lost 1.5 kg.



Cauda equina,
included in the PTV
was spared

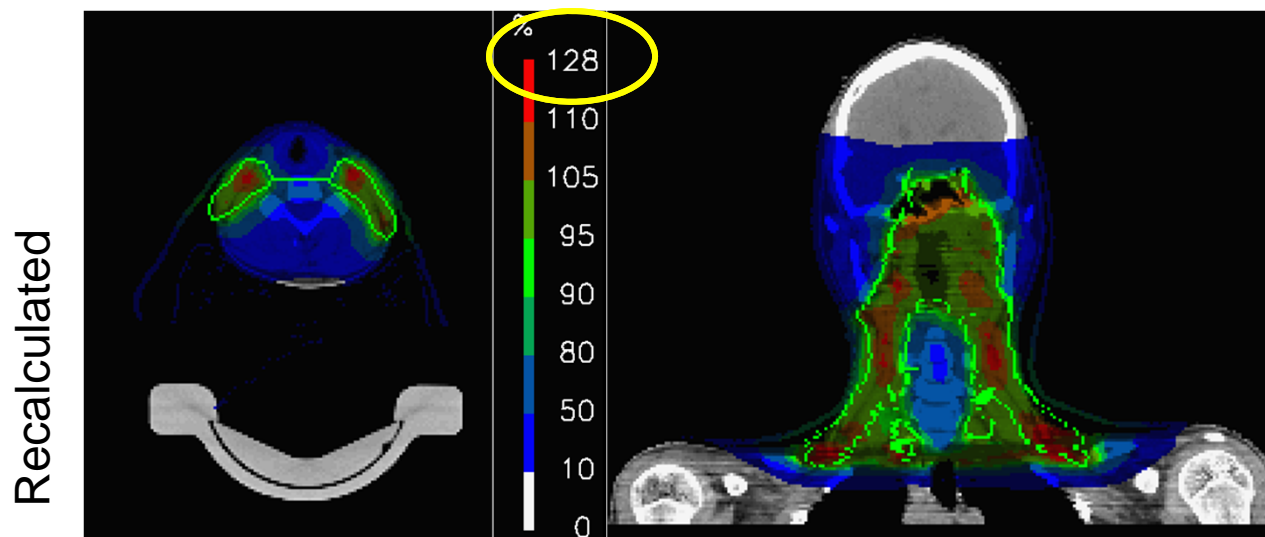


Volume shrinkage (neck lymph nodes)

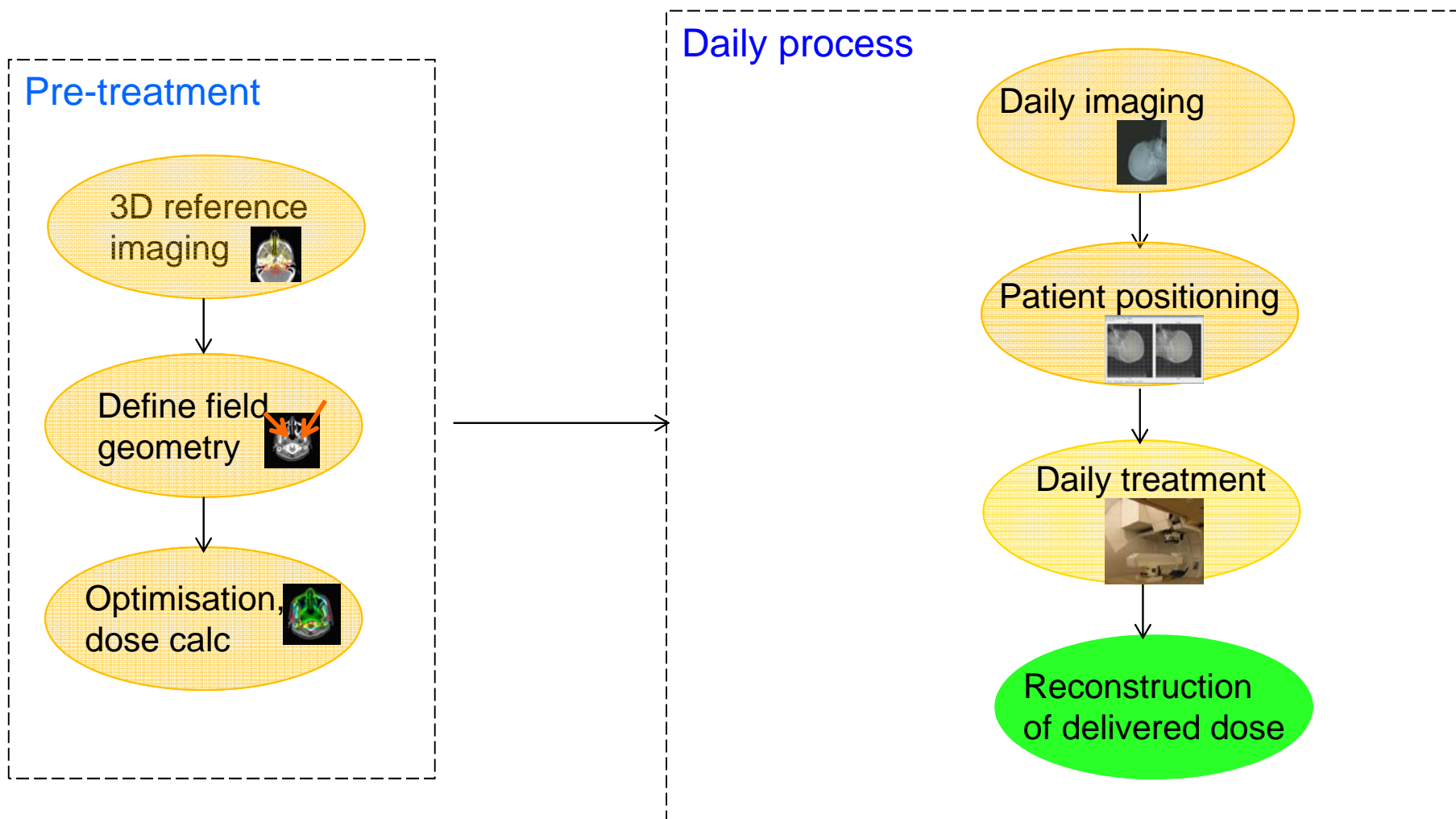


Node shrinkage of about 1 cm;
It was detected during the course of treatment.

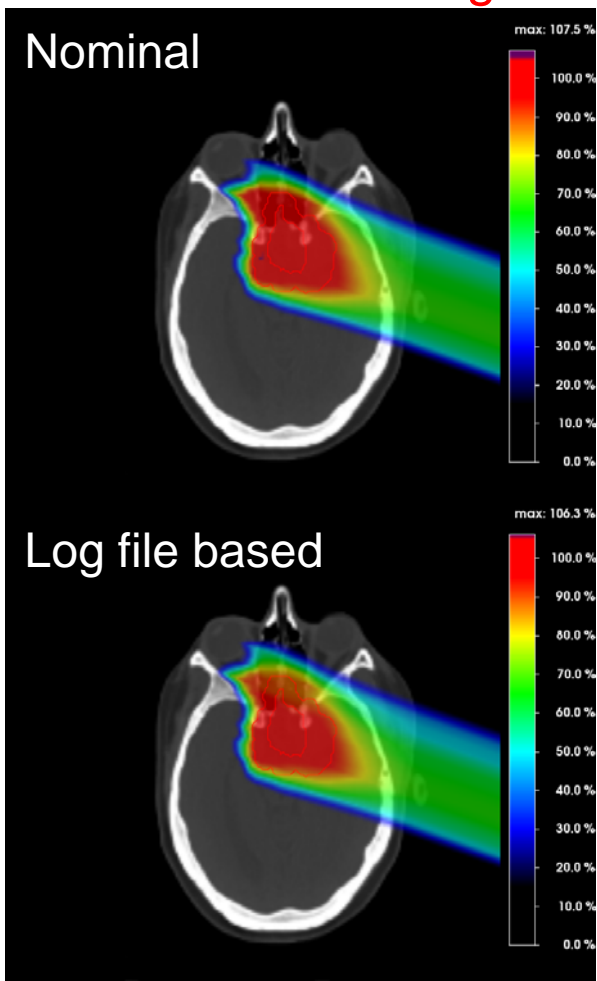
Replanning was done due to the overdose



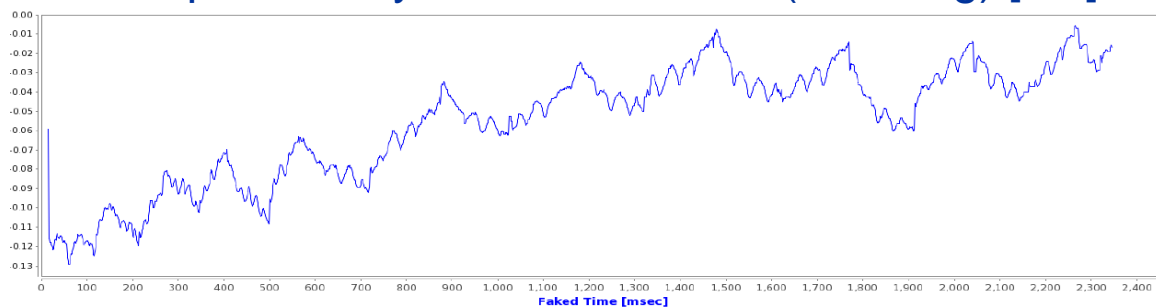
They can appear in different step of the entire radiotherapy workflow:
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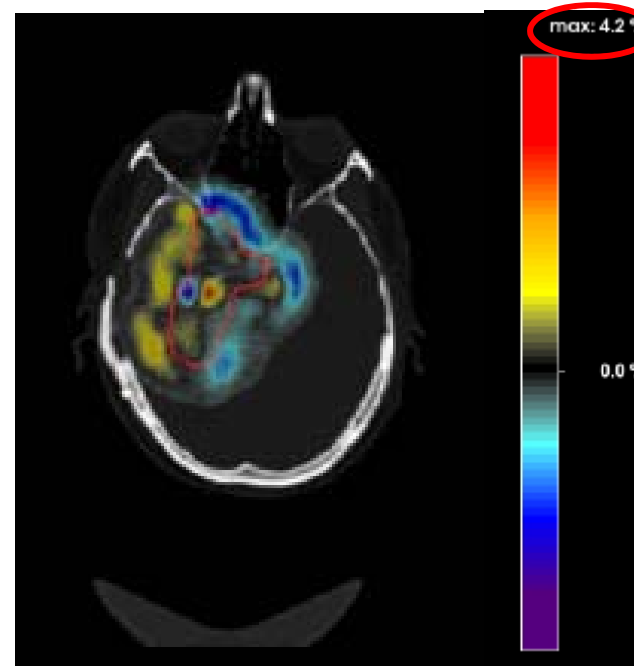
Calculation from log files



U position dynamic correction (teaching) [cm]



Meier G. et al.
Independent dose
calculations for
commissioning, quality
assurance and dose
reconstruction of PBS
proton therapy. Phys
Med. Biol 2015 Apr 7;
60(7): 2819-36



Scandurra et al. "Is what we plan what we actually deliver? Using machine log-files to analyse delivery of 20 clinical PBS plans on PSI Gantry 2". Poster at PTCOG 54

Different ways to deal with the (range and set up) uncertainties:

1. patient monitoring

(detect range differences as soon as possible
ideally daily)

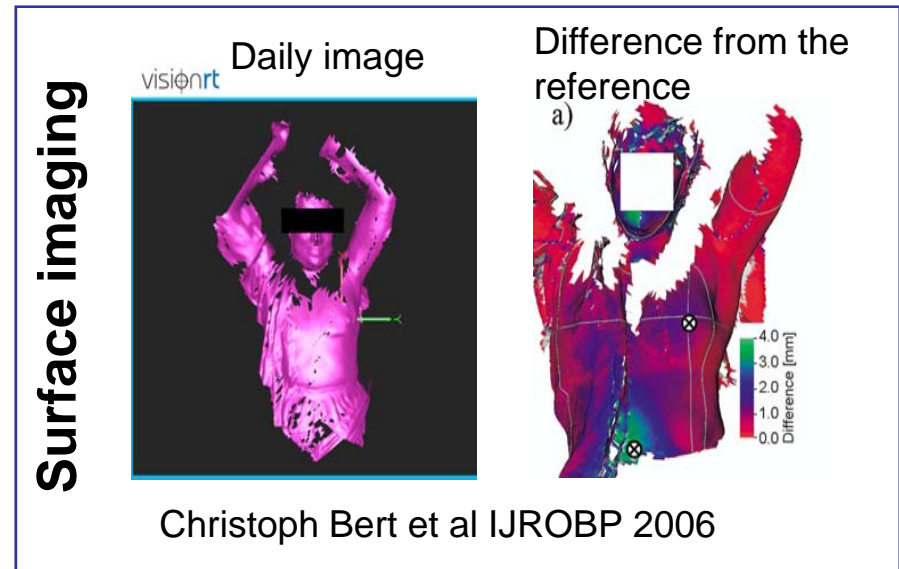
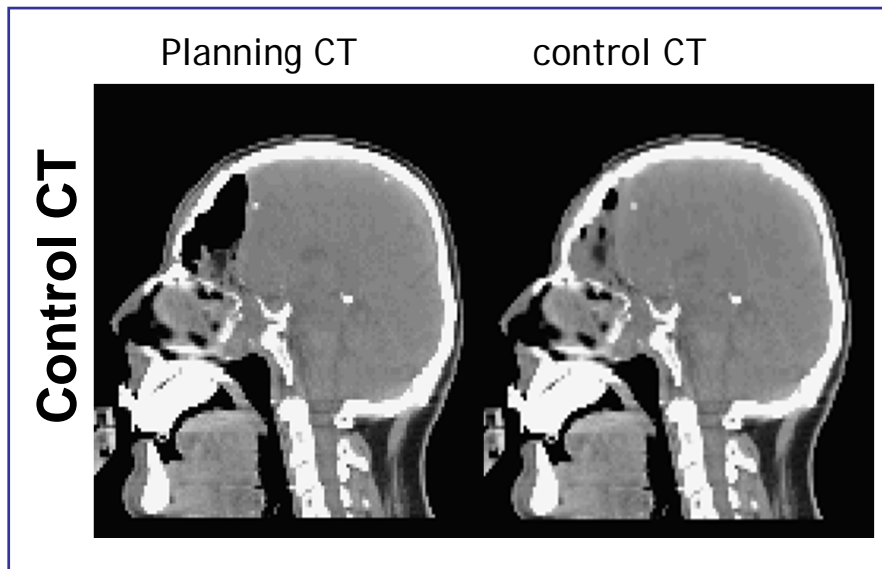
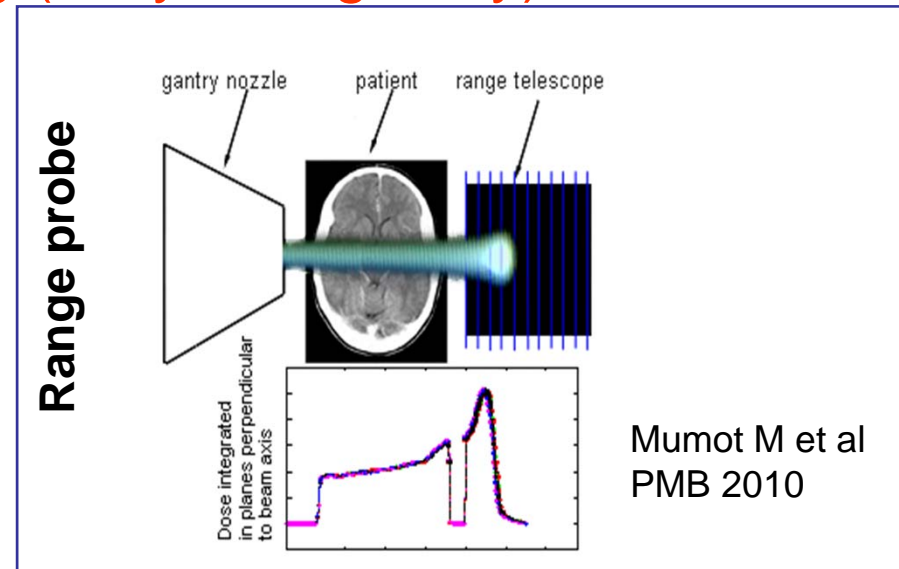
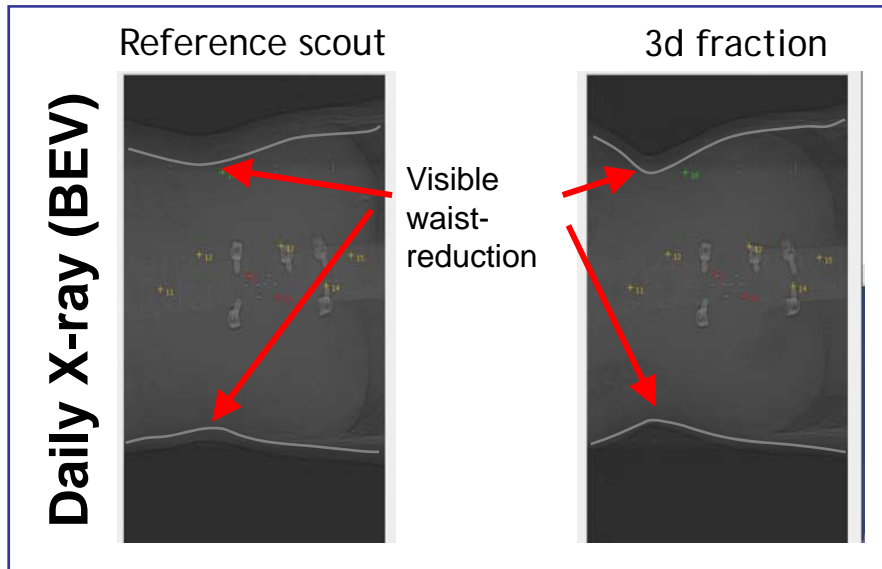
2. adaptive therapy

(adapt the plan, as soon as possible
ideally daily)

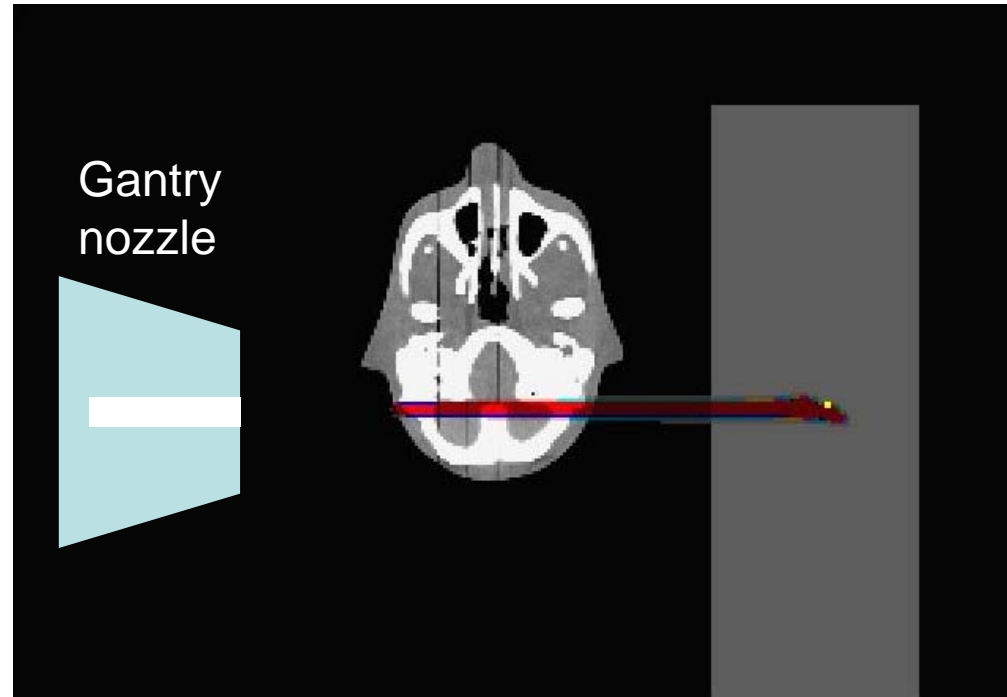
3. robust planning

(reduce **a-priori** the impact of range uncertainties)

1. Patient monitoring (daily or regularly)



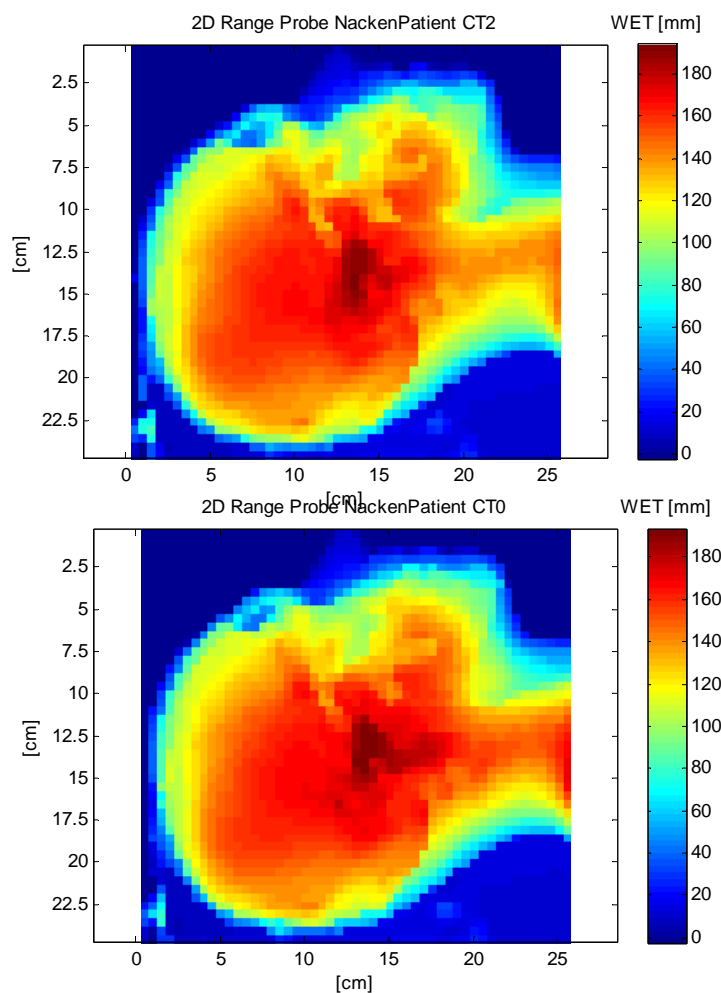
1. Range probe



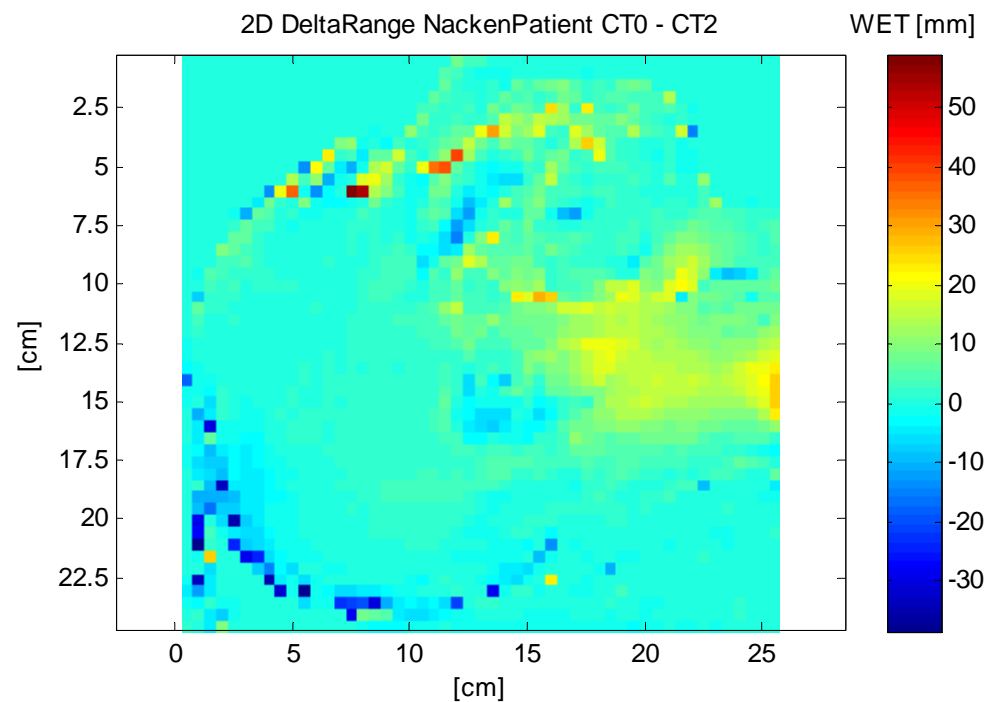
Single pencil beam with going through the patient
residual range measured in the MLIC

1. Range probe 2D

2D RP 5x5mm spacing.



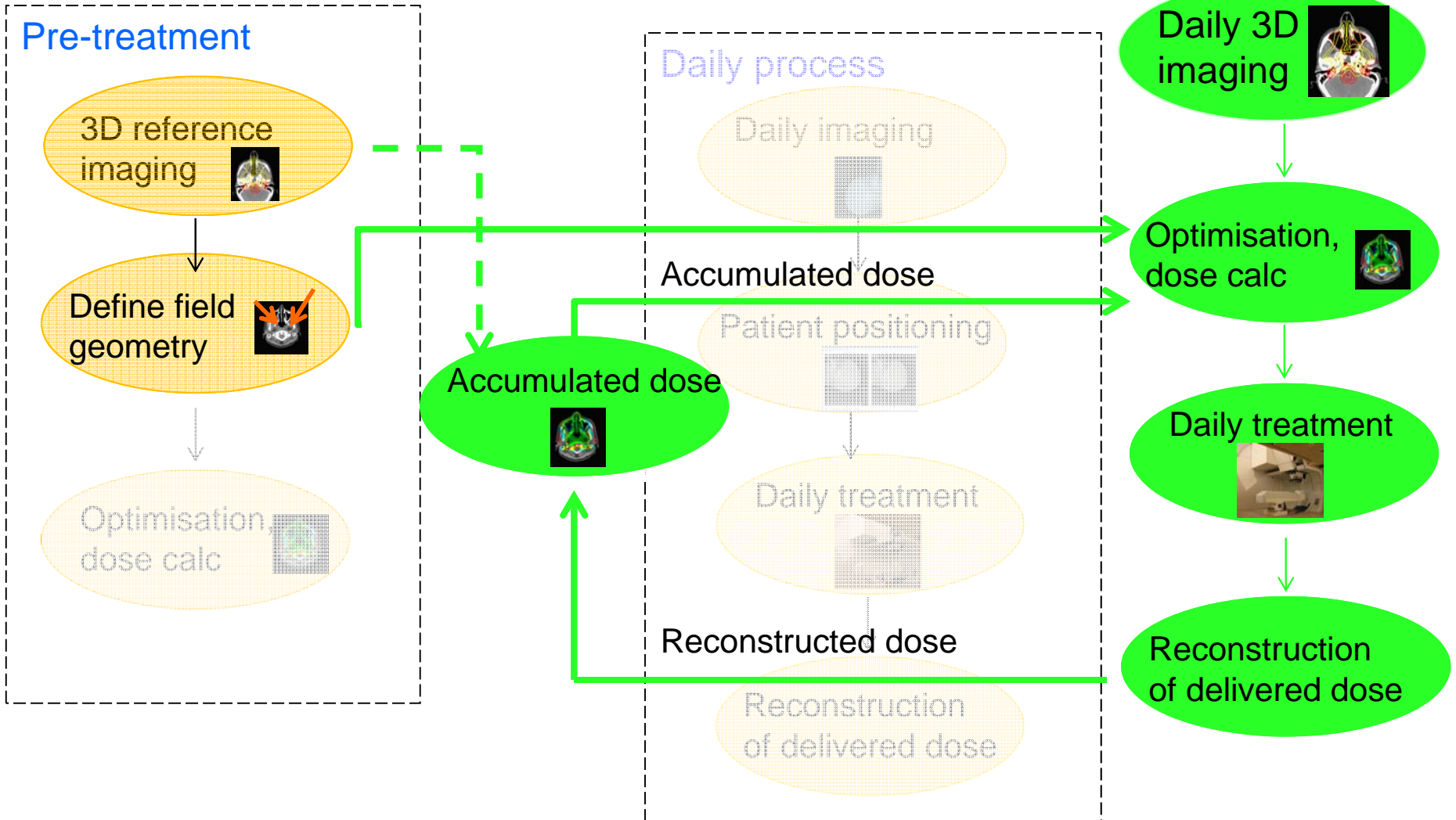
Residual positioning error and anatomical changes



PhD work of Abdel Hammi (PSI)

2. Adaptive therapy

Adaptive Daily process



Courtesy of Tony Lomax

3. Robust planning

1. Careful **selection of field incidences** and planning techniques (as IMPT and SFUD)
1. Automatic incorporation of all the errors (range, set-up) in the **optimization process** (change of the cost-function)

Unkelbach J et al 2009 Med Phys. ; Unkelbach J et al 2007 PMB; Maleike, Flynn (Ex Raysearch)

3. Changing the **optimization starting condition**:
 - a. manual selection of beam angles avoiding or penalizing path going through sensitive areas
 - b. changing the initial beamlet fluences

Lomax A et al, 2001 Med Phys; Albertini F et al, 2010 PMB

There are different kind of uncertainties (i.e. heterogeneities, positioning, range, delivery, RBE...)

They come into play during the entire workflow

Different possible solutions are based on:

- a. Image guidance
- b. Daily adaptive
- c. Robust optimisation

The simplest and cheapest solution is based on:

Multiple fields with optimised directions

Thank you!

..a special thank to Tony Lomax , Francesca Albertini and all my CPT colleagues



Uncertainties in the clinical practice:

Head and neck cases very challenging due to many concomitant problems:

- denti, artefatti, eterogeneità patient positioning, shrinkage of the nodes...(satangunantan)
- Organ motion (slide di Tony..ma questo merita talk a parte)
- Referenze a poster di Dan e gabriel (eventuale slide su log file calculation)**

Differenza di uncertainties in SFUD/IMPT!!!!!!

Sostituire range adaptive con plan adaptation

Immagine su artefatti denti, eventualmente tagliare ancora una slide di Stefania.

Summary

Dynamically Adapted Radiotherapy (DART)

PAUL SCHERRER INSTITUT



The concept...

