

# Beam Spreading Methods

PTCOG 52

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# Goals of Radiotherapy

- *Deliver the Prescribed Dose.*
  - *What is Dose? How does a Dose get delivered?*
- *Deliver the Prescribed Dose Distribution.*
  - *What physical principles allow one to create a Distribution?(Spread out in a volume with the correct dose.)*
- *Deliver Dose to the Target.*
  - *How to position the relative relationship between the beam and the target.*



What do we know this morning?

We know enough about the particles to understand how to accomplish the above.

We need to know how to use the physical properties of these particles and which tools are needed to accomplish the above

# *Some Goals of a Beam Delivery System*

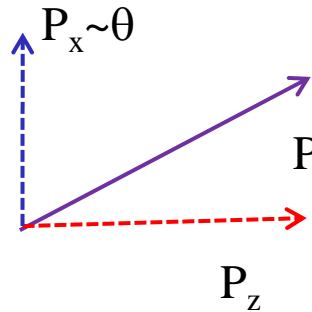
- Dose Distribution:
  - Direct the beam to the target and with the desired dose distribution
- Unwanted Dose:
  - Minimize Dose outside the target area (from any particle- e.g. neutrons) (*Penumbra, Distal Falloff, ...*)
- Treatment Time:
  - Allow for a Clinically Effective and efficient treatment
- Sensitivities
  - Use realistic tolerances of the incoming beam parameters (position, angle, timing)
- Implement a Operational Efficiency & low Cost
  - Patient Specific Hardware
  - Number of fields required
  - QA



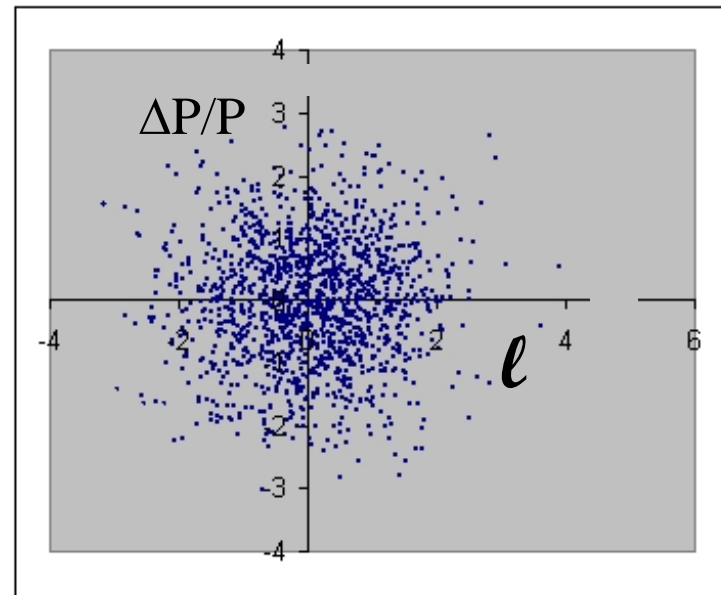
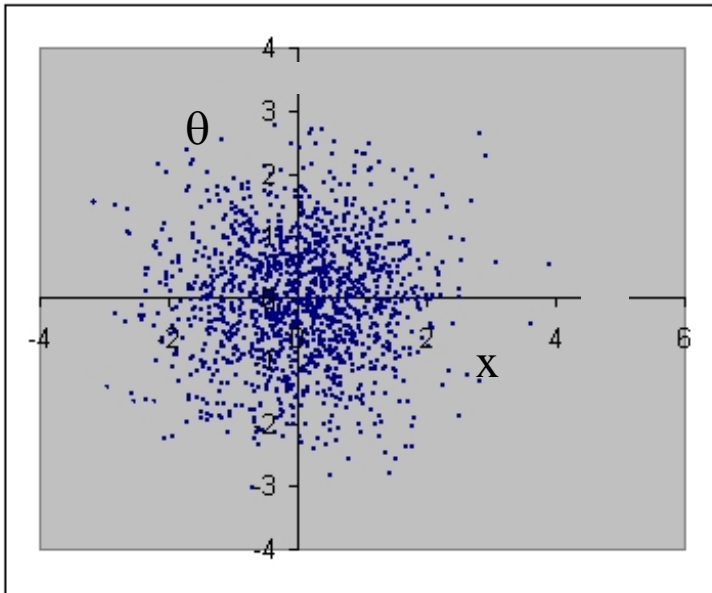
# What is a Beam?

- A beam is a collection of many particles all of whose longitudinal and transverse momenta are close enough and remain more or less close to each other.

One characterizes the Transverse properties of a beam by plotting the **phase space diagram** below in which the *transverse particle position* and *transverse momentum* of each particle in the beam is plotted.

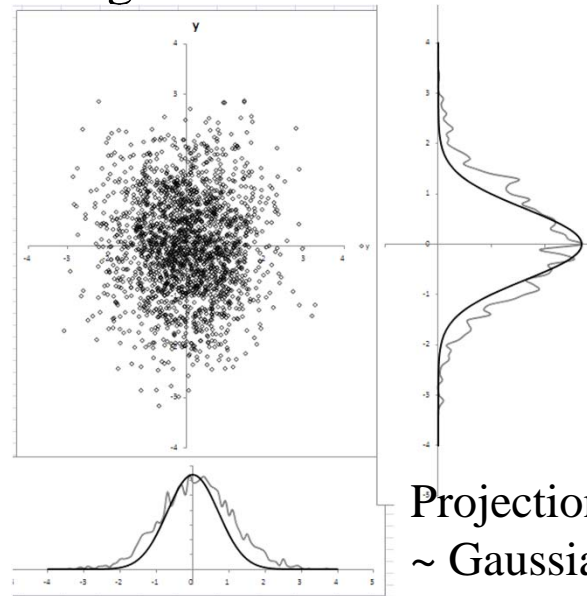
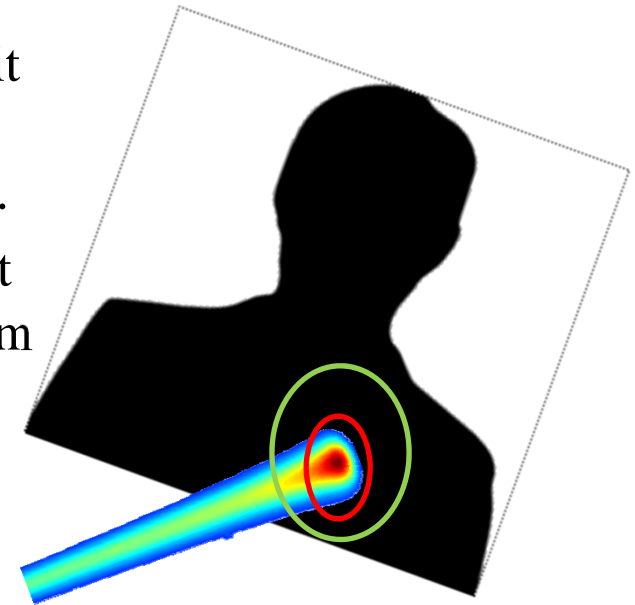
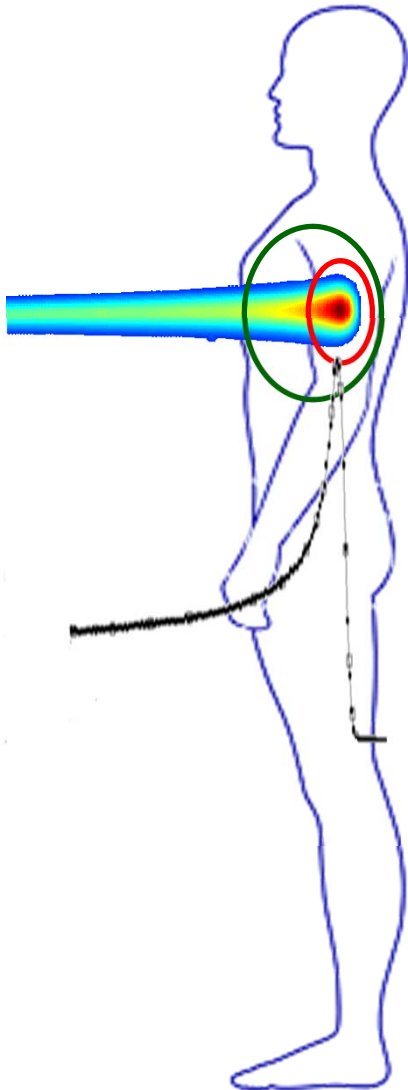


One can characterize the Longitudinal properties of a beam, similarly by considering the *longitudinal momenta* in the beam and the *length* of the beam.



# The need to “spread” a beam

- The beam from an accelerator is narrow (transversely and longitudinally) (a “Pencil”) –The distribution of that beam, even if it is defocused transversely is Gaussian, not conformal to an Rx.
- Doesn’t match the target shape. It is necessary to spread it to conform to the target



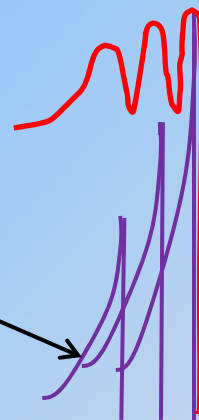
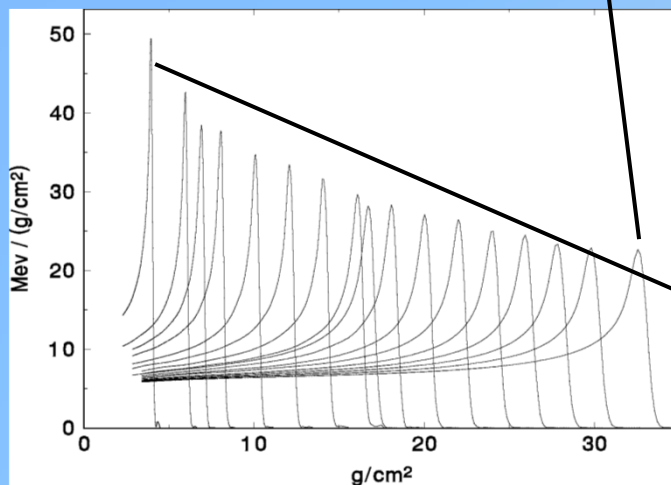
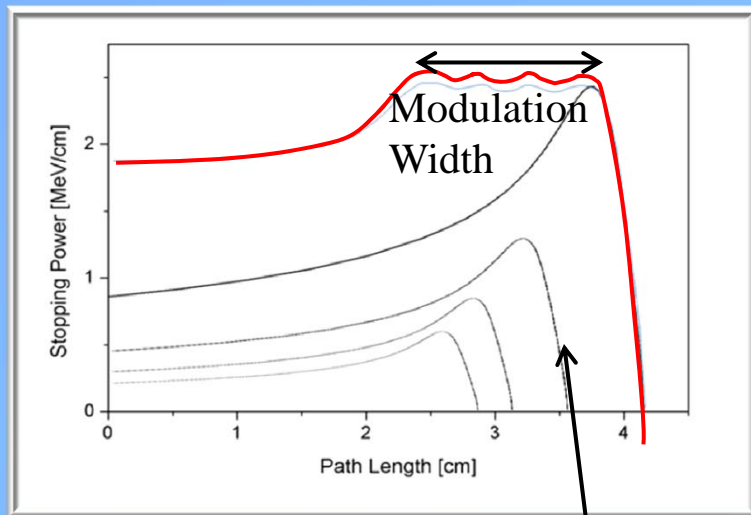
Projection is  
~ Gaussian Distribution



# *Longitudinal Spreading Options*

- Passive (do nothing) Spreading
  - Ridge Filter
- Active (do something) Spreading
  - Range Modulator Wheel
  - Energy Stacking
    - Beam
    - Mechanical

# Spread out Longitudinally (Spread Out Bragg Peak - SOBP)

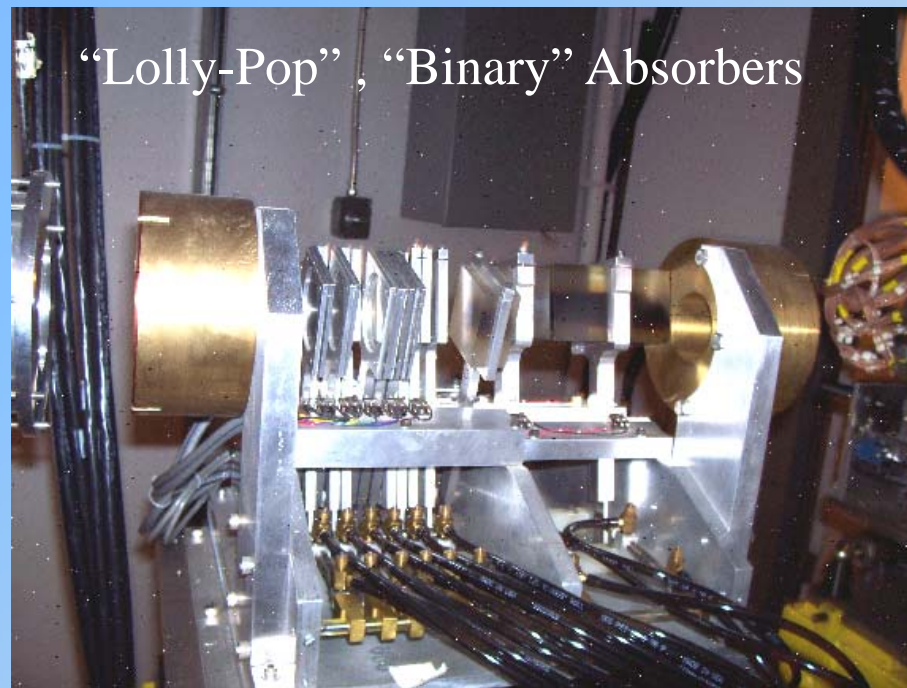
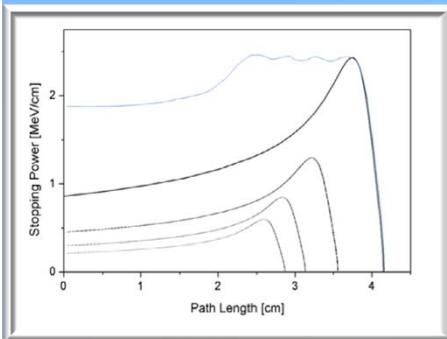


- Spread out Bragg Peak
    - Sum up Bragg Peaks spaced apart
    - Adjust the relative amplitudes to create the desired SOBP (Does NOT have to be FLAT!)
    - The Bragg Peaks are NOT Gaussian and therefore the spacing is fairly sensitive.
    - Sensitivity is further enhanced at Low Energy! (It's harder to smoothly attach Sharp peaks.)
      - Reduced straggling
      - Reduced absolute energy spread (constant momentum fraction)
- If one pulls back a higher energy peak, the initial energy spread is included and the peak is less sharp + more straggling*



# *How to change the beam energy?*

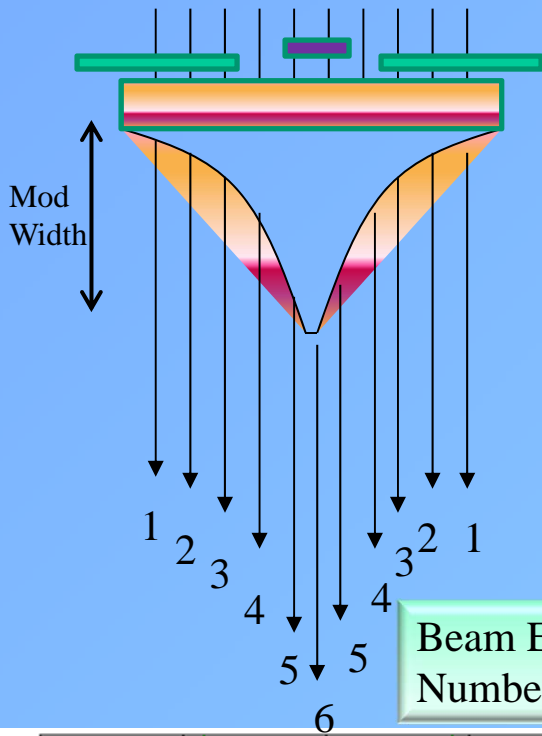
1. From the Accelerator (Before the Nozzle)
2. AFTER the accelerator (Degrader in Nozzle)
  - Binary Absorber



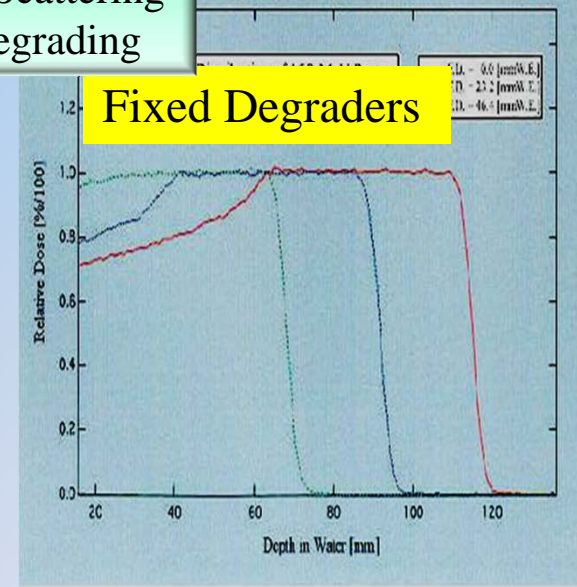
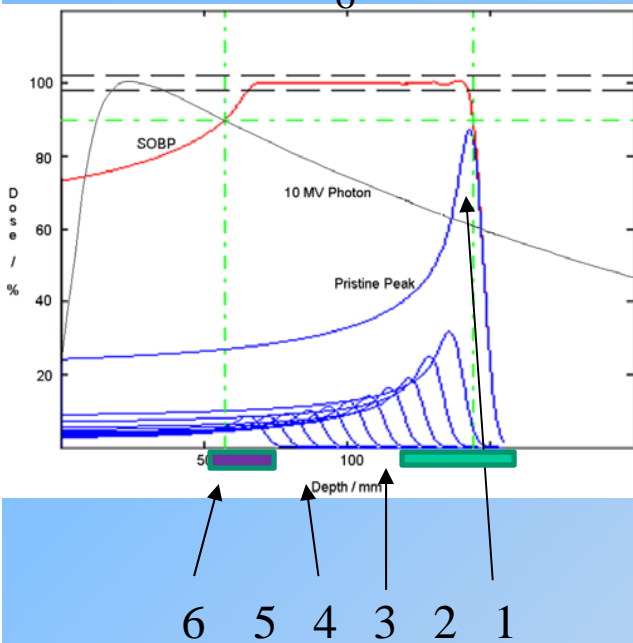
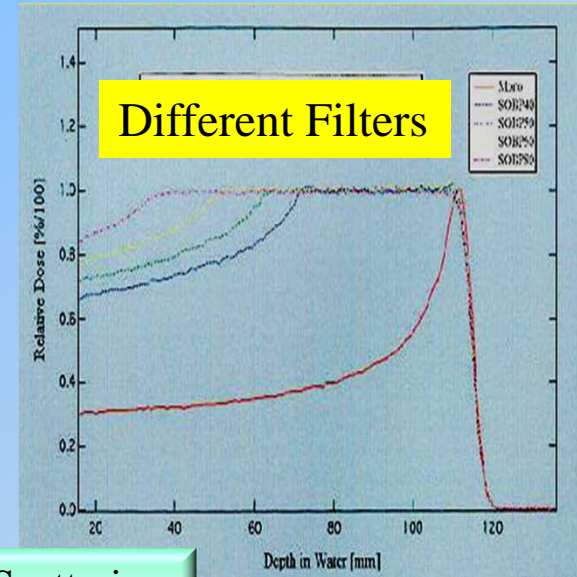
Control the NUMBER of Ions that enters the target at a given Energy



# - Ridge Filter



Beam Energy Variations is Mixed Transversely via Scattering  
 Number of Protons controlled by length of region degrading



# - Range Modulator Wheel

This is NOT "Passive"



Courtesy of  
B. Gottshalk, Ph.D.

-Control the number of protons getting through at a given energy with the geometry

-Proton Rate x Time = # Protons

-Assume proton rate constant

-Assume rotation rate constant

- 360 degrees in e.g. 0.1 sec (600rpm)

- NO Degradation >1/3 of the time →

More of the beam at higher energy

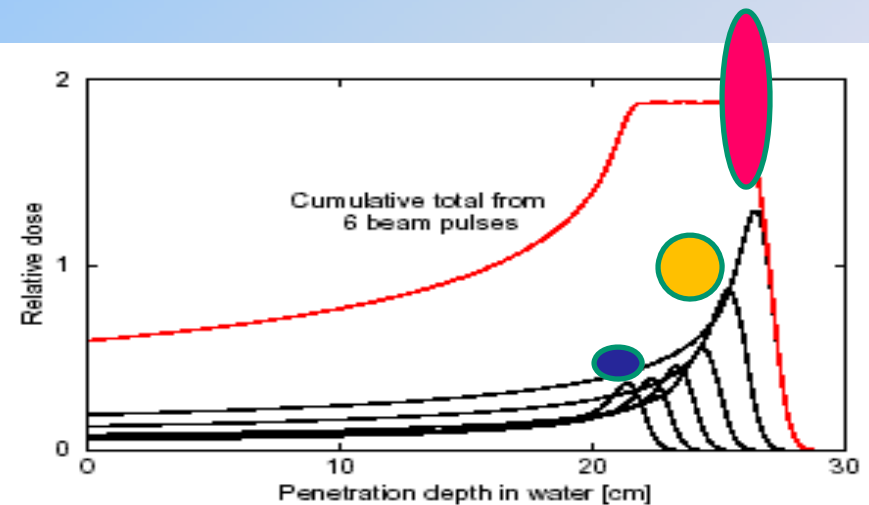
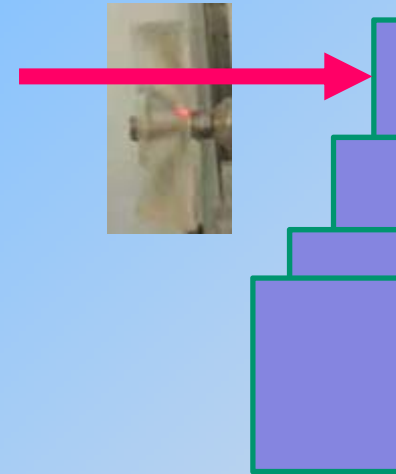
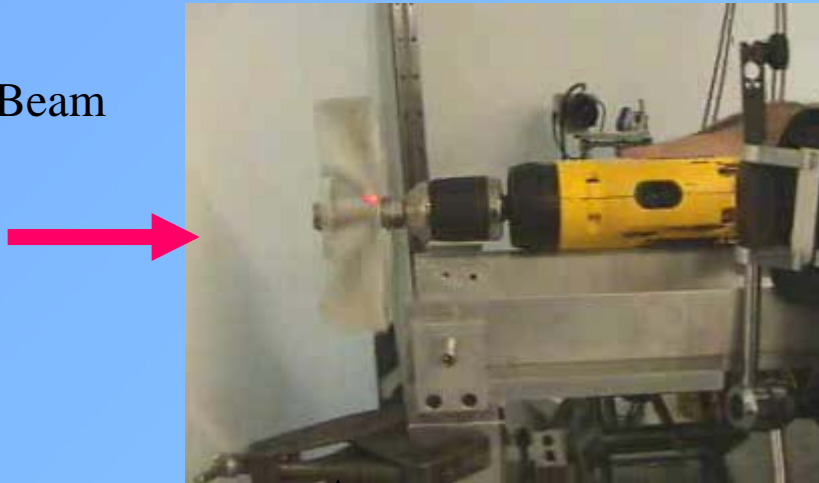


Figure 1: Spread out Bragg peak from 6 beam pulses.

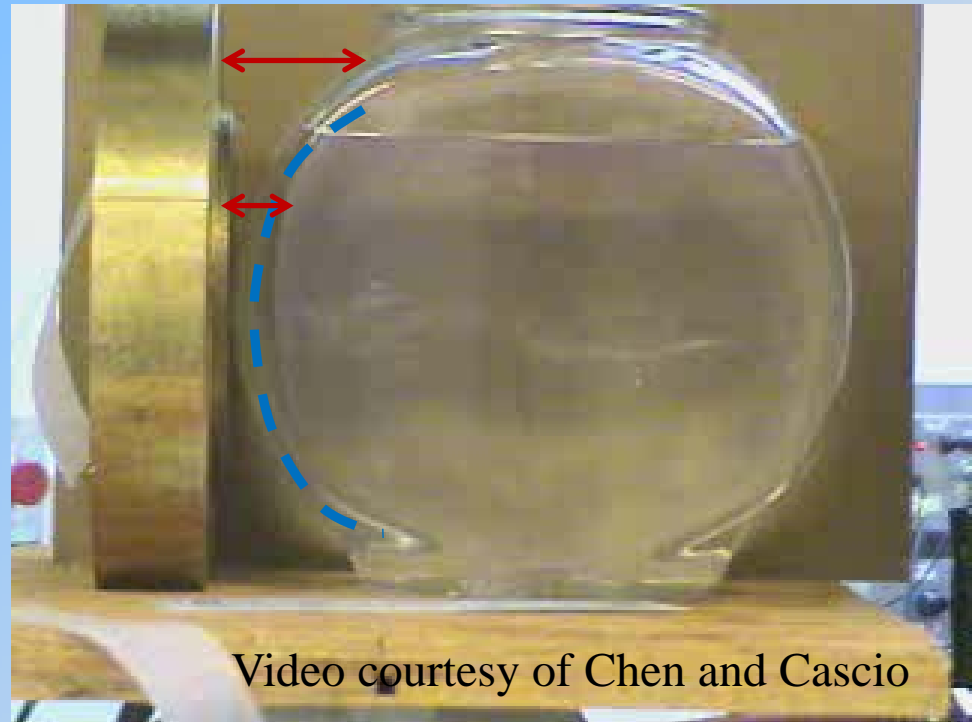
# *Range Modulating Wheel*

*Visualize the Proton Range using liquid scintillating material in a fish tank + Slower wheel.*

Beam



Propeller  
Multiple thicknesses  
of plastic

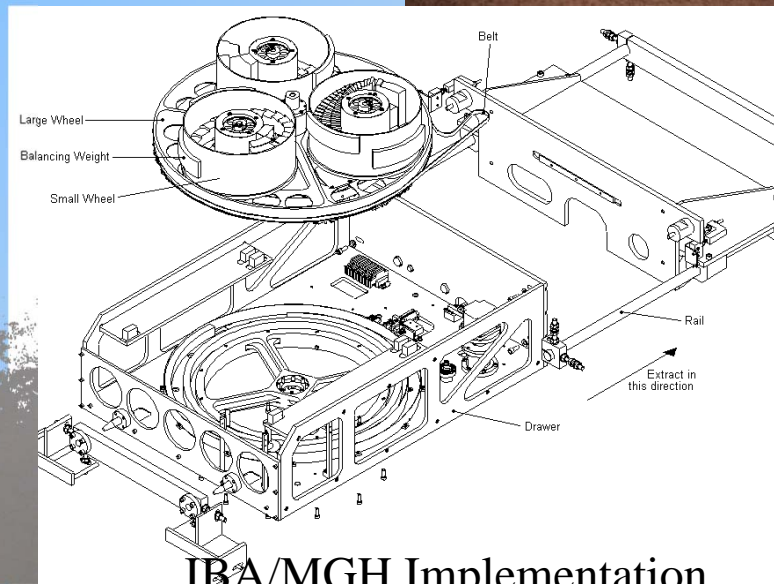
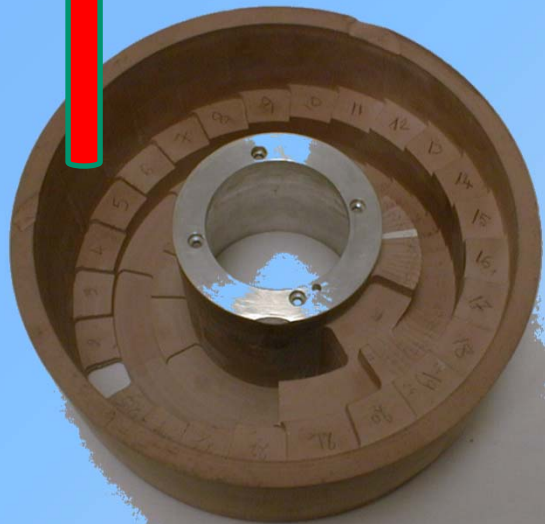
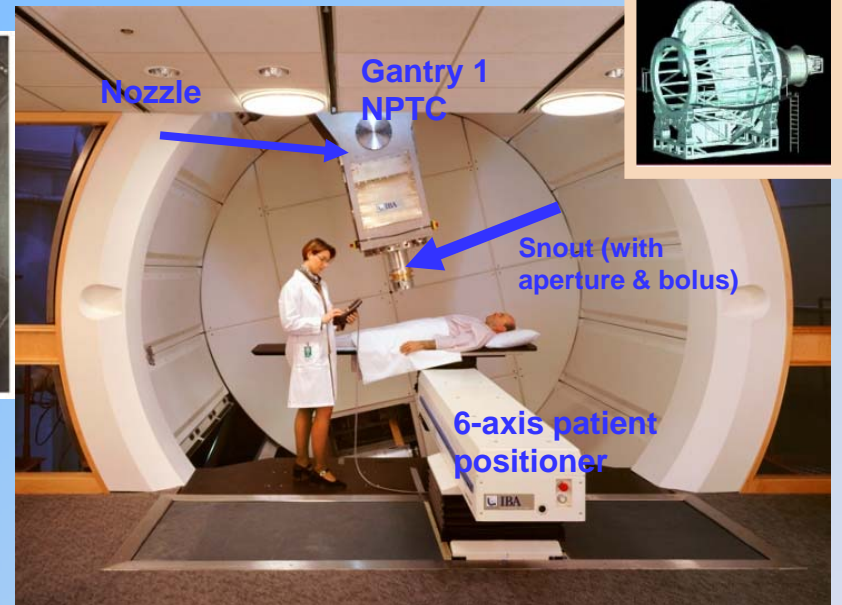
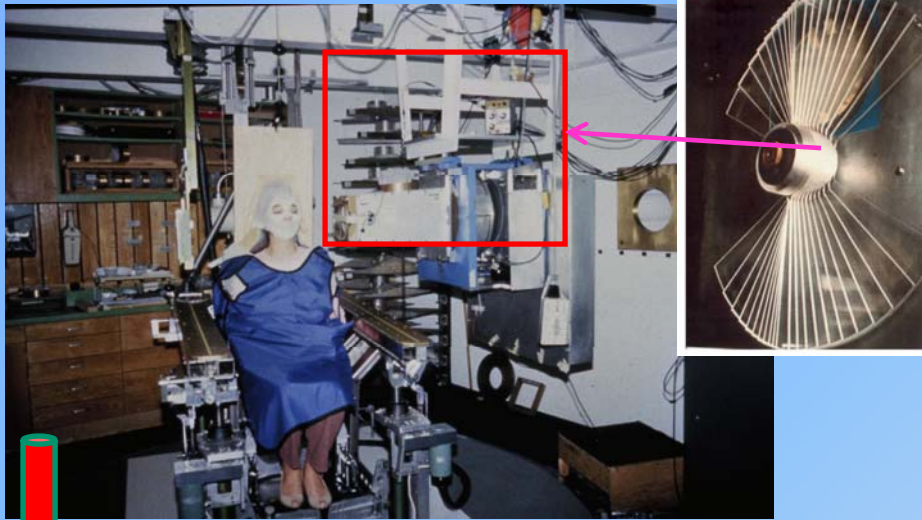


Aperture + Fish Tank with  
Scintillating Fluid



# Evolution of Range Modulation

## MOD WHEELS ON THE WALL



IBA/MGH Implementation

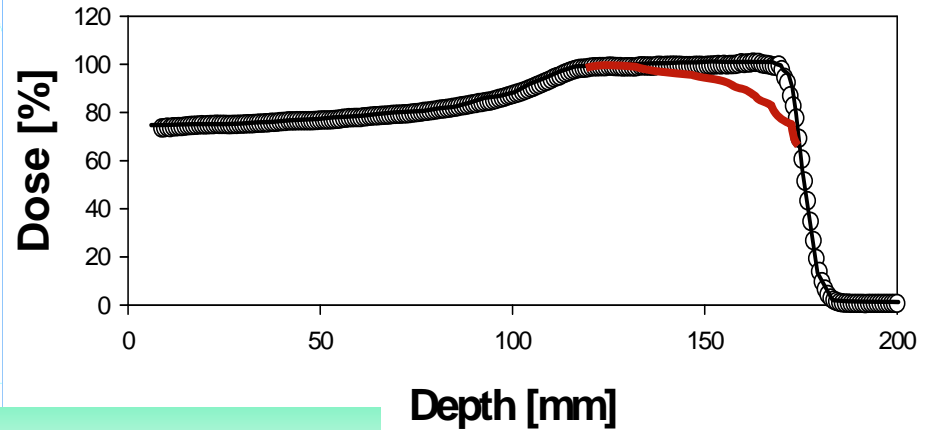
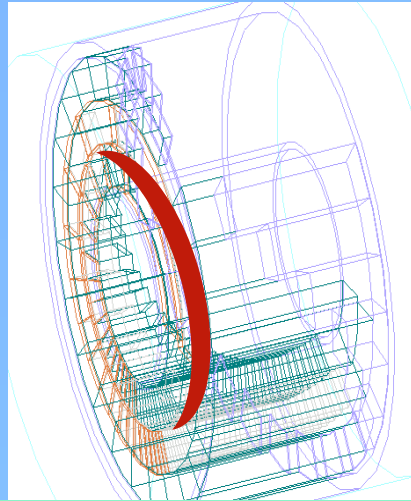
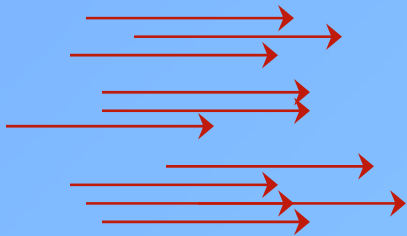
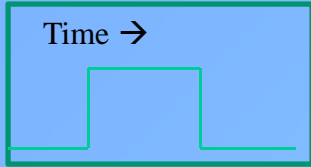
## MOD WHEELS IN THE DRAWER

Flanz 2013; PTCOG Educational

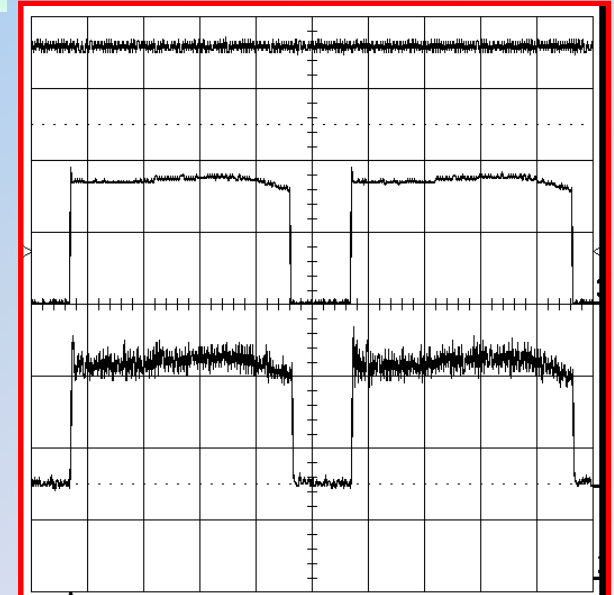
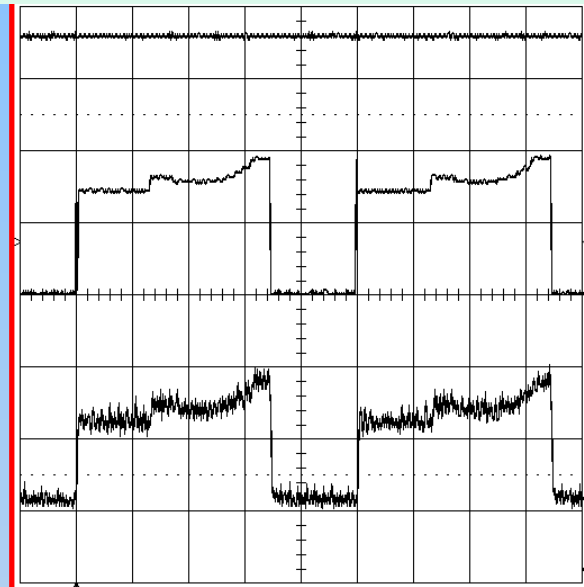
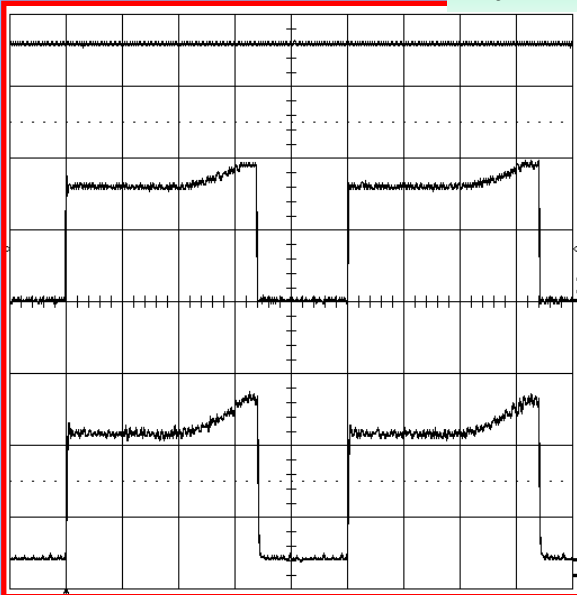
Courtesy: Paganetti

# Current Modulation

A **Requirement** of a multi-use Mod wheel based Proton Beam Delivery System

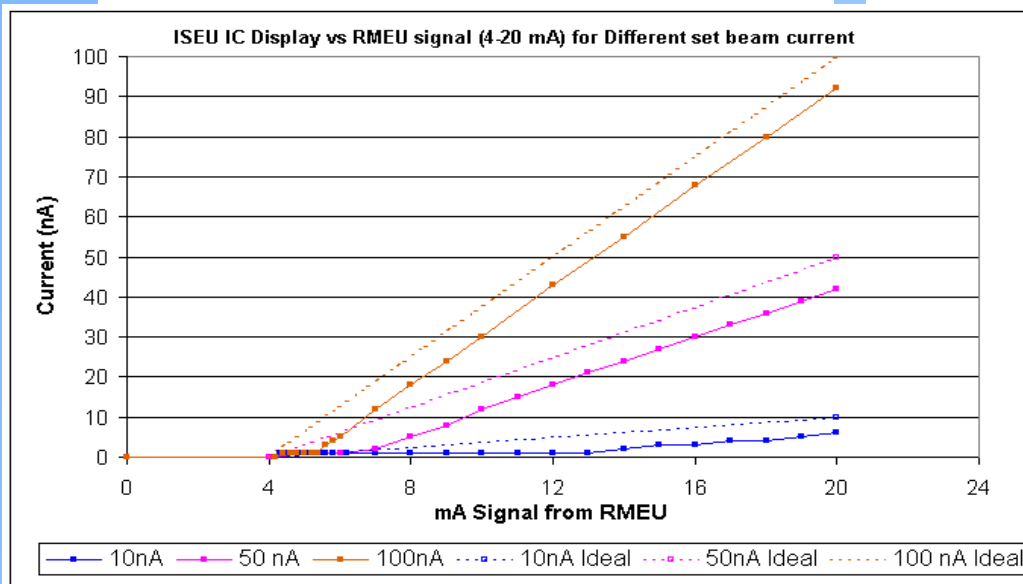
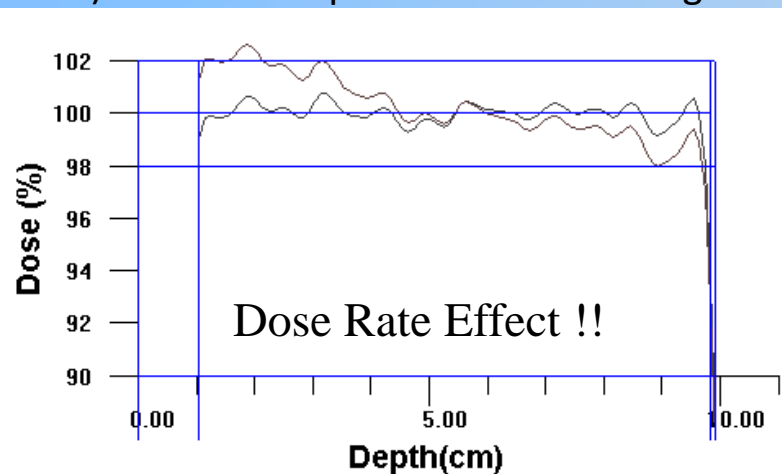
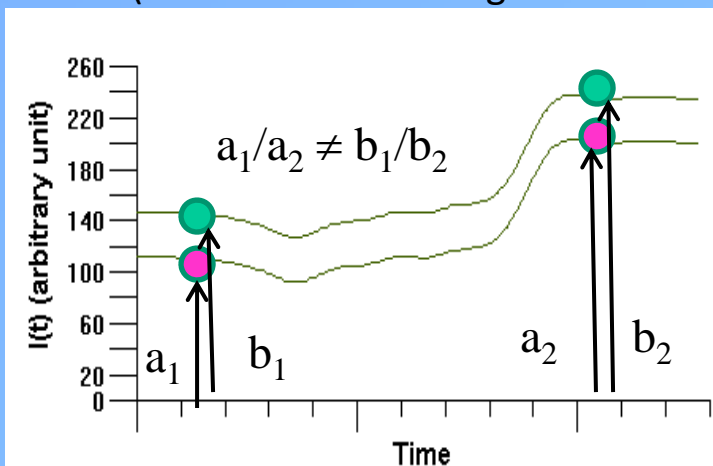


System is anything **BUT PASSIVE !!**



# Sensitivity: Current Modulation

If BCM current is shifted by a fixed amount, the ratio of the current from one time to another during a cycle will be different (and the relative weights of the Bragg peaks) AND the shape of SOBP will change.



We experienced lack of issues with the SOBP flatness in the beginning, until we investigated thoroughly and found (and FIXED) an offset in the requested vs. delivered current.

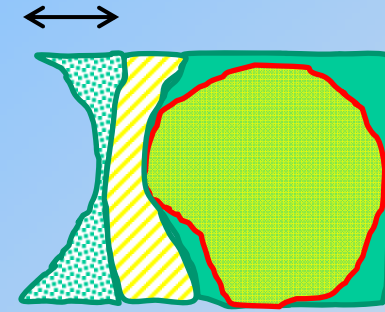
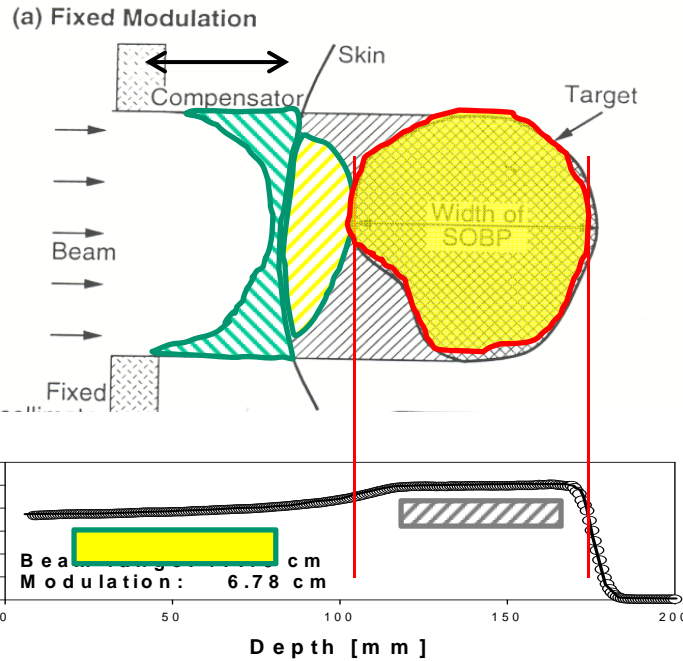
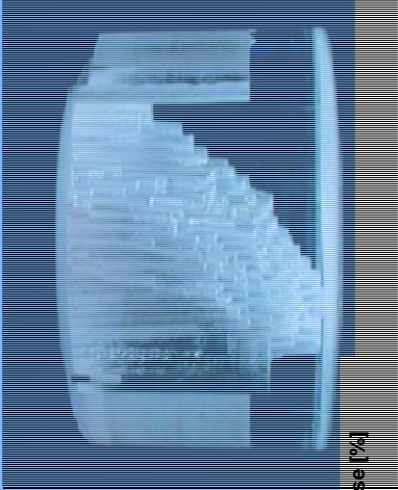
Hsaio-Ming Lu, Robert Brett, Martijn Engelsman, Roelf Slopsema, Hanne Kooy, and Jay Flanz, "Sensitivities in the Production of a Spread-Out Bragg Peak", Med Phys 34 (10), 3844, 2007

Flanz 2013; PTCOG Educational

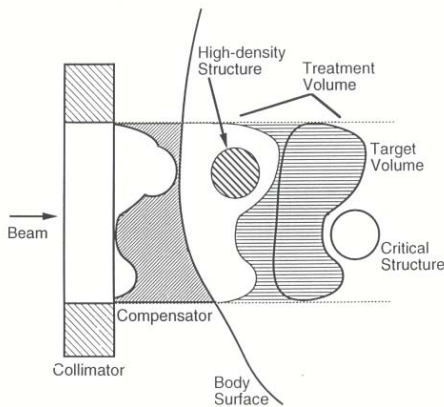


# Distal Edge Conformation

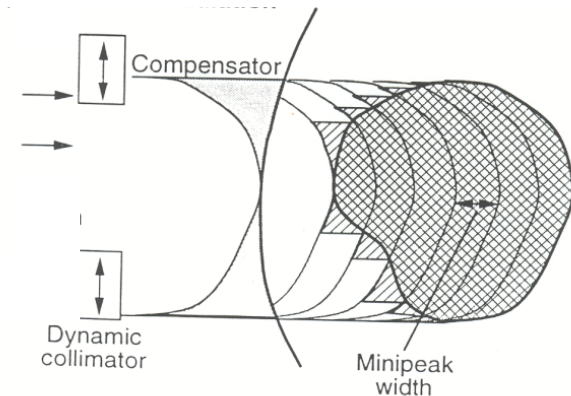
Compensator/Bolus



Mod Width **Fixed** ACROSS target !!  
 Thickness of Compensator  
 determines Bragg peak "pull back"



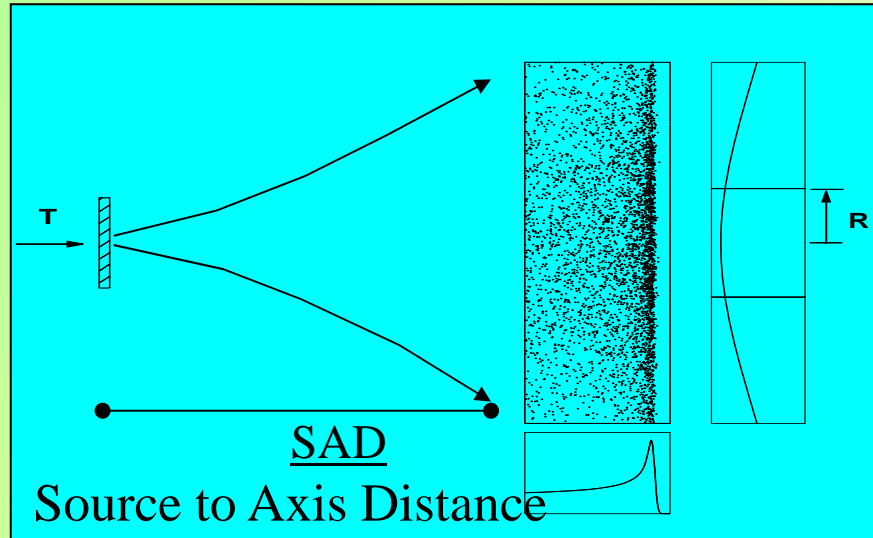
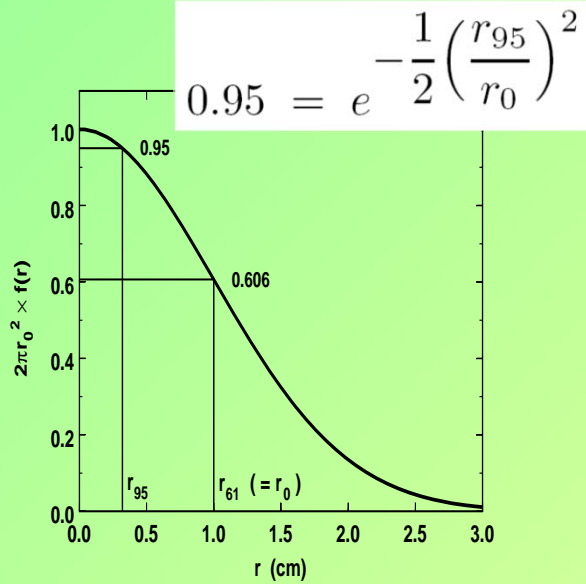
Energy Stacking with **Variable Collimation + Compensator**



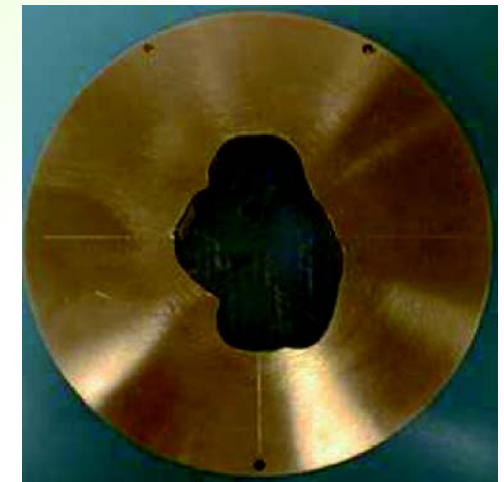
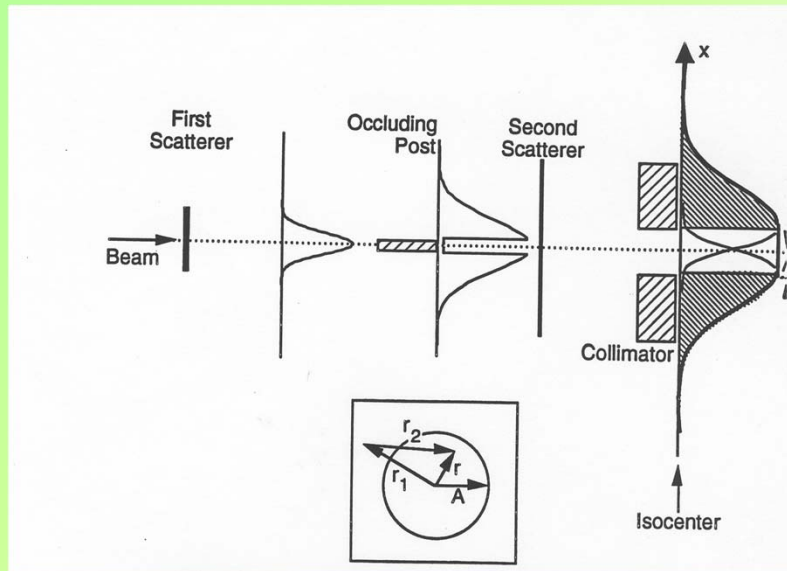
# *Transverse* Spreading Options

- Passive Scattering
  - Single Scattering
  - Double Scattering
- Wobbling (Beam Scanning with Scattered beam)
- Pure Magnetic Scanning
- Combined Magnetic and Mechanical Scanning
  - Moving Magnet
  - Moving Patient

# Scattering – Start with Gaussian Beam

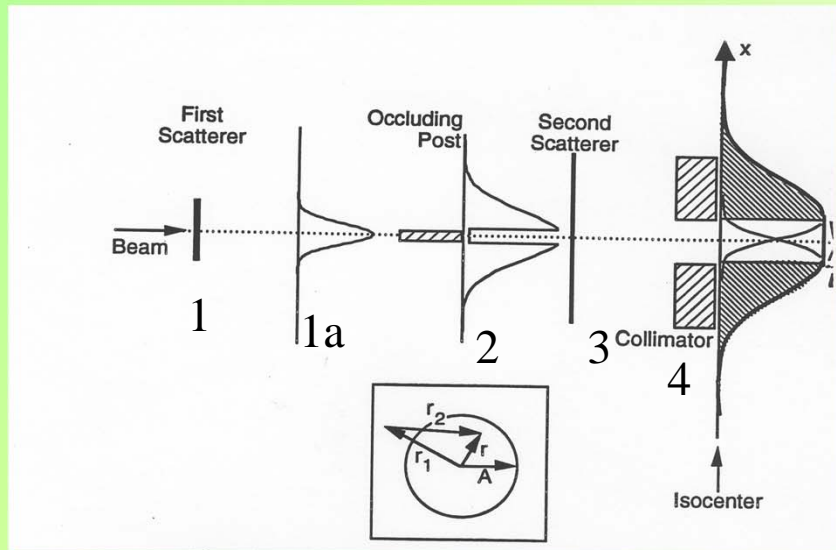
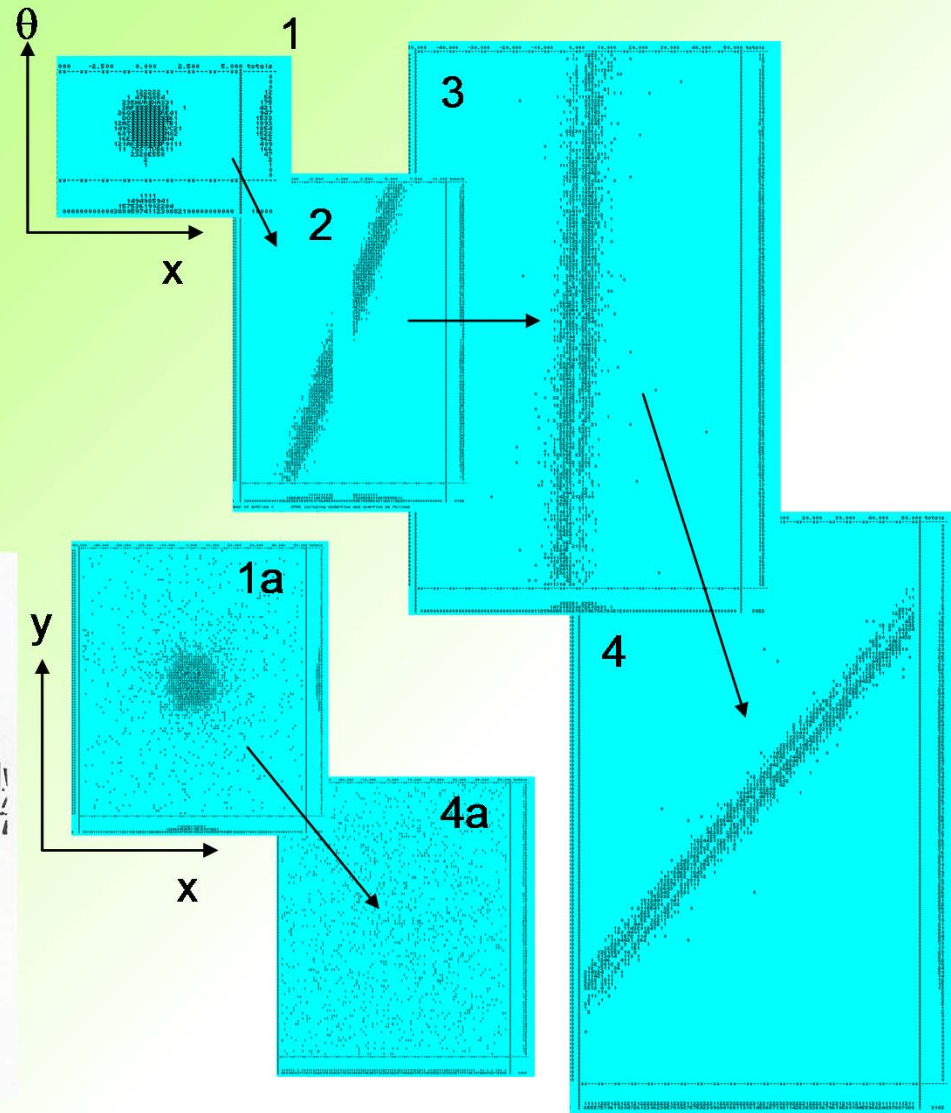
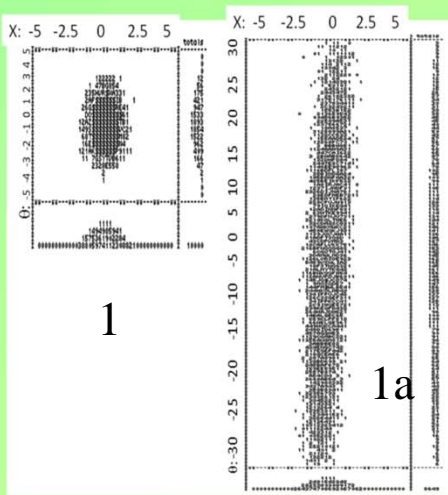


*Single Scattering*



*Simple form of Double Scattering*

# Double Scattering – The real story





# Combined First Scatterer and Range Modulator

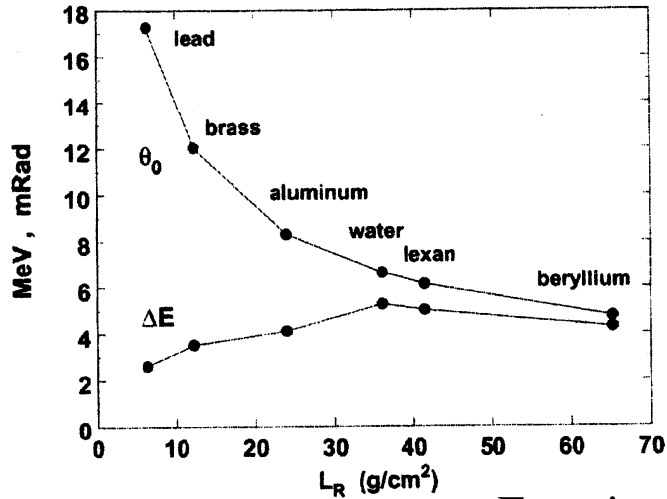
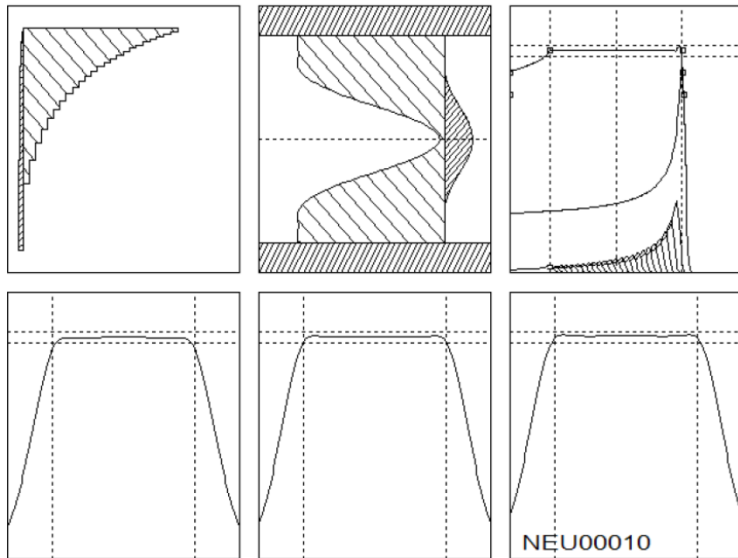
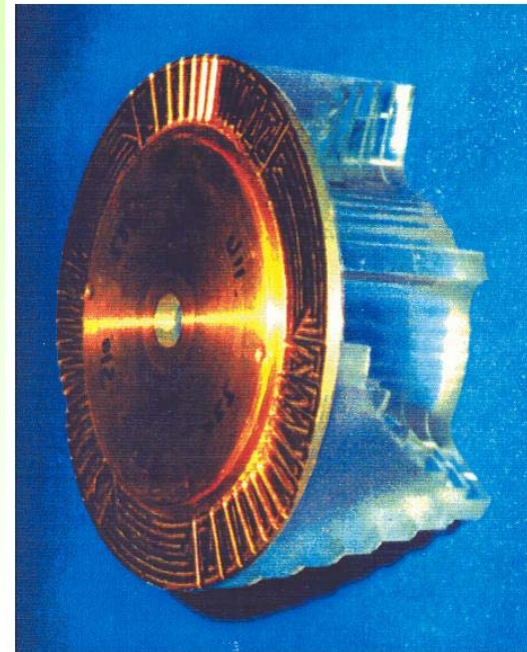


Figure 9.1: Scattering and stopping in various materials.

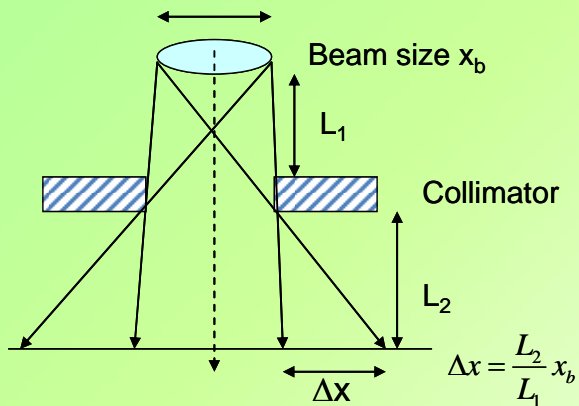
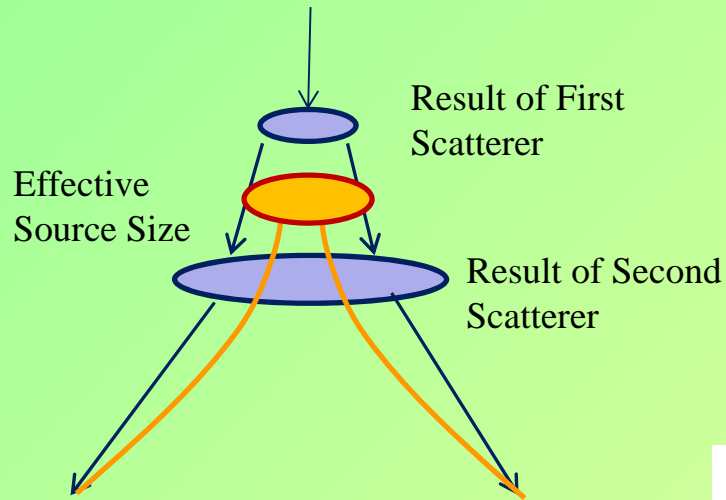
Function of A and Z



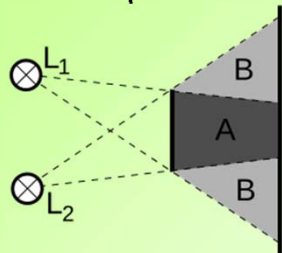
- Combining what we've learned about the Energy Loss and Multiple Scattering ...



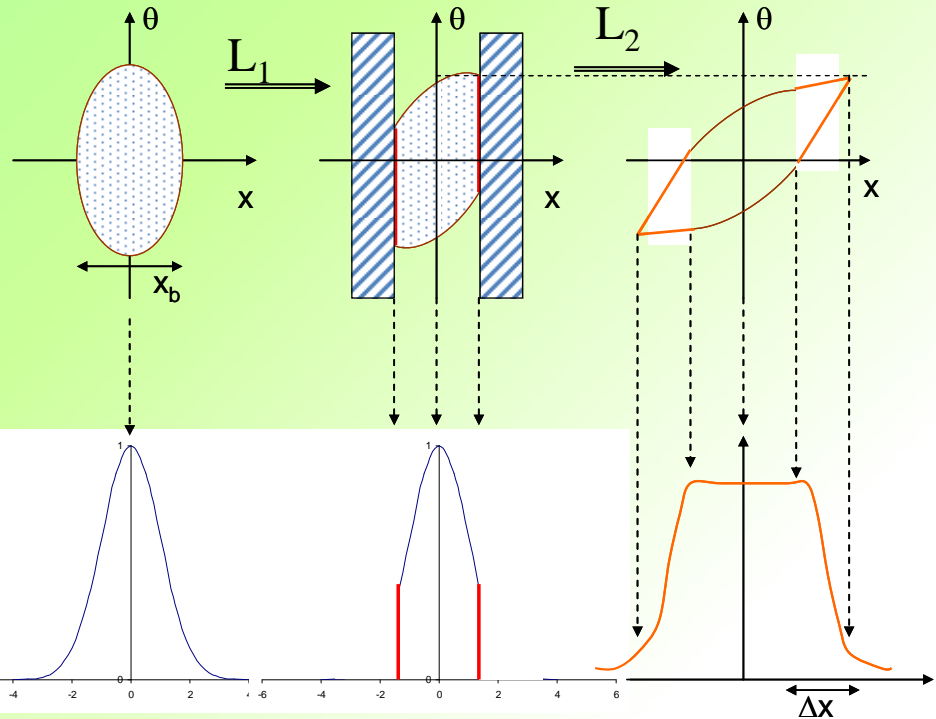
# Penumbra



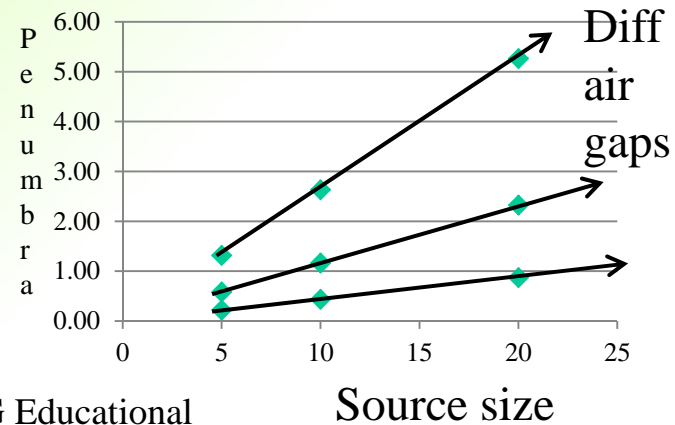
Geometric Representation of Collimation



The **umbra**, **penumbra** and **antumbra** are the names given to three distinct parts of a **shadow**, created by any light source after impinging on an **opaque** object. For a point source only the umbra is cast. Umbra (A) and penumbra (B)

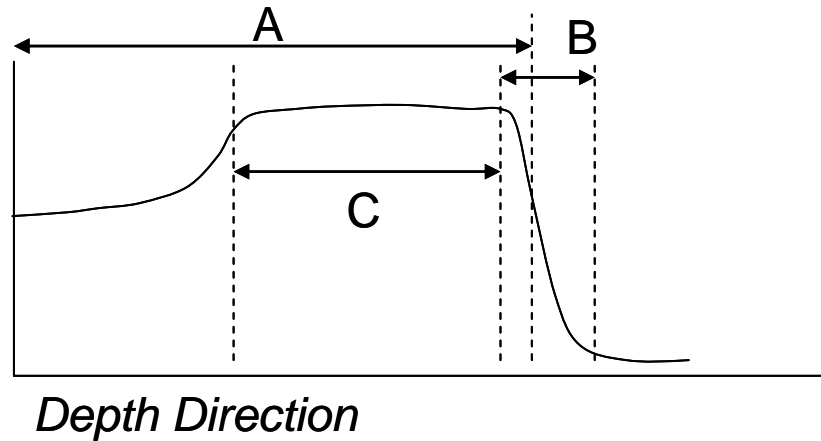


Optical Representation of Collimation

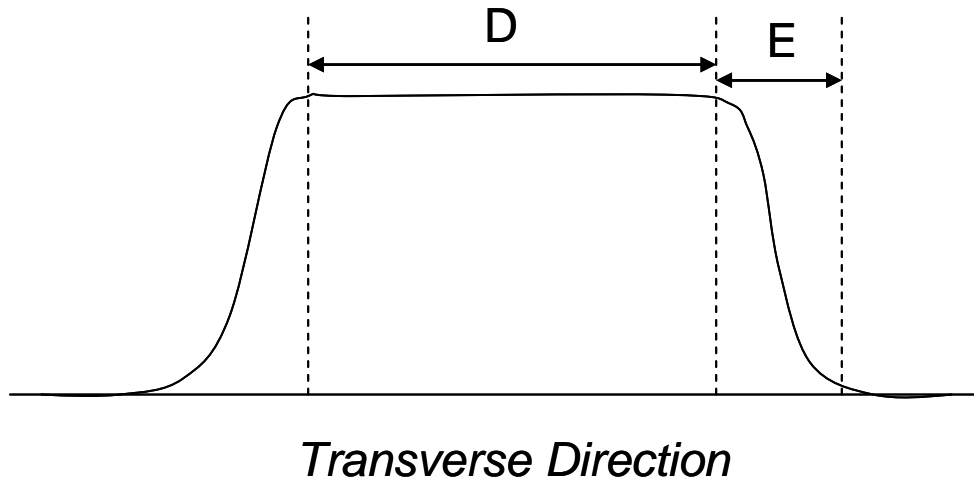




# *Dosimetric Regions of Interest for Scattering*



- A. Range (95%?)
- B. Distal Fall off (80%-20%)
- C. SOBP Width (95-98?)
- D. Lateral Width (50%)  
Uniformity(95%?)
- E. Penumbra (80-20%)



Not everyone uses the same  
Definitions?

# Particle Beam Scanning: Developing Frontier

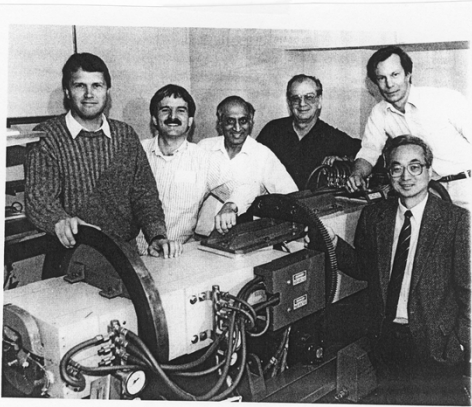


Fig. 4. Raster scanning system shown with its development team of Drs Chu, Renner and Ludewig engineers Nyman, Singh and Stradtner.



30 Years



Technology?  
Clarity?  
Vision?

- 1978-9: Spot Scanning at NIRS - 30 Patients
  - Range Modulator (Fast) + Lateral 2d Spot
- 1992 ish: B&W Scanning at BNL
- mid 1990's: Spot Scanning at PSI
- mid 1990's: Scanning at GSI

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- 2008: Scanning at MDA (with Hitachi)
- 2008: Scanning at MGH (with IBA)
- Renniker (RPTC) (with Varian)
- Upenn (with IBA)
- ...Others

**HITACHI**  
Inspire the Next

*Iba*

**VARIAN**  
medical systems

**MITSUBISHI ELECTRIC**  
Changes for the Better

**PROTOM**  
PROTON THERAPY TECHNOLOGIES

**Sumitomo**  
Heavy Industries, Ltd.

# What is Particle Beam Scanning (PBS)?

The idea is to SPREAD the beam with a dose distribution that conforms to the prescription.

Beam scanning can be defined as the act of moving a charged particle beam ('relative to the target') of particular properties and perhaps changing one or more of the properties of that beam for the purpose of spreading the dose deposited by a beam throughout the target volume.

Position (x,y)

Speed ( $v_x, v_y$ )

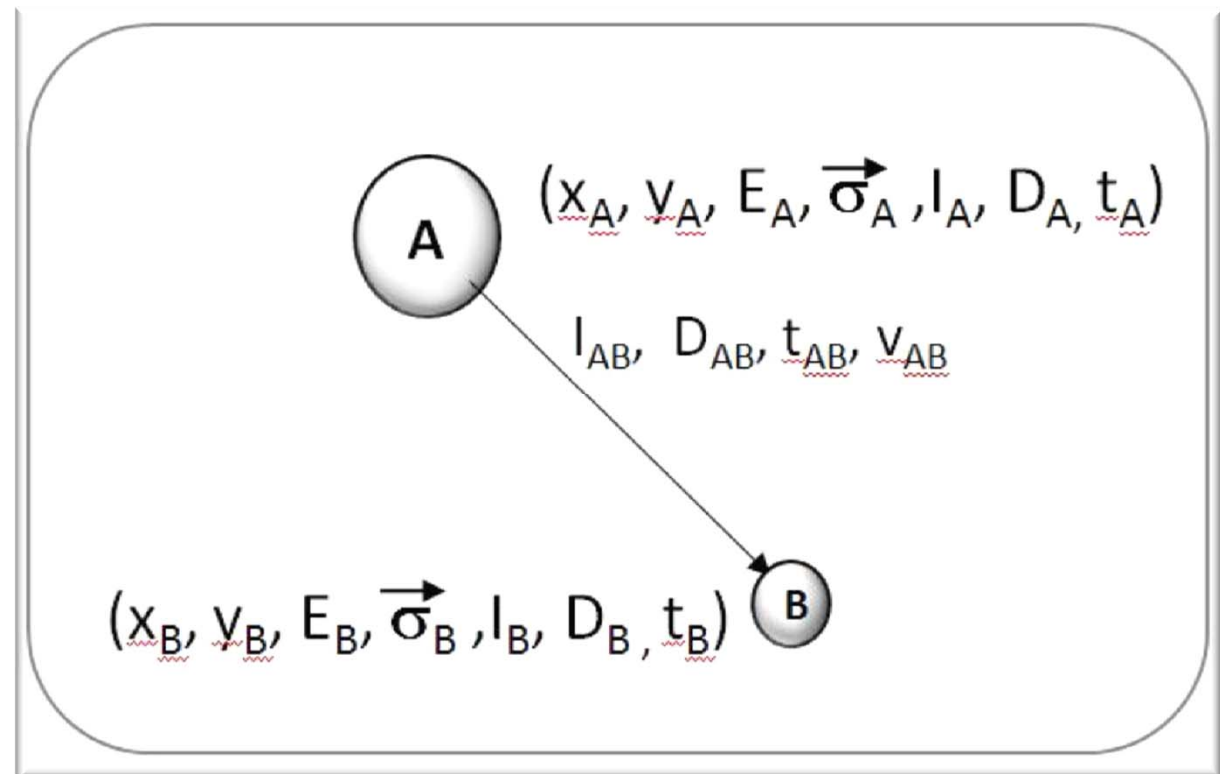
Energy (E)

Time (t)

Intensity (I)

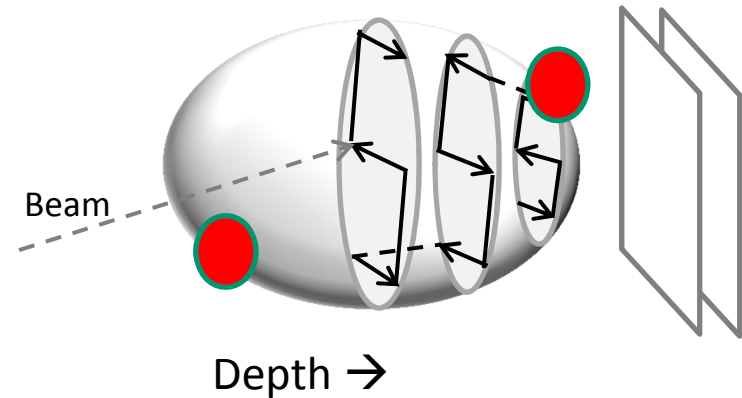
Size( $\sigma$ )

Dose (D)

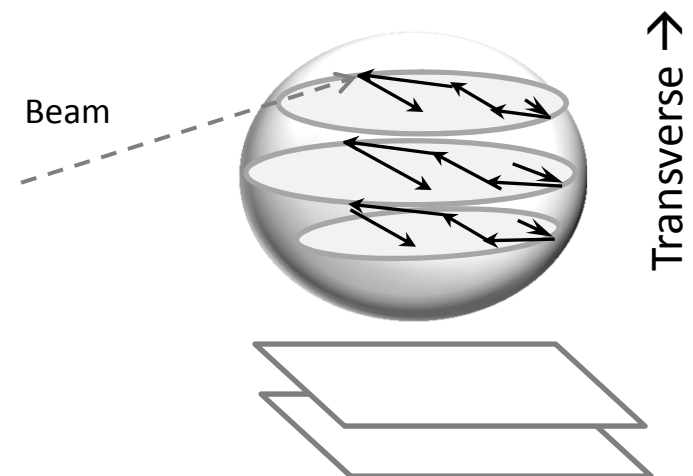


# How to spread out the beam (3d)?

- To deliver a conformal dose one must control the beam position transversely and in depth.
- Which combination of directions depends upon the many factors (e.g. speed...).
- Usually the Energy (Range) Change time is longest (e.g. 5 sec to 0.1sec (PSI)) vs. milliseconds transversely.



Two extreme examples



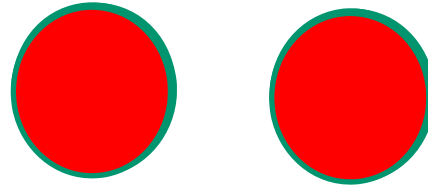
- Scattering techniques cover the 3D volume either instantly (Ridge filter) or at most over about a 0.1 second time interval.
- *Normally, Scanning starts at one position and irradiates 'sequentially' taking time to reach the last 3D position. (All things being equal (in time) one could do it diff)*
- *5 sec x 25 Layers = 125 sec (2 min)*
- *0.1sec x 25 Layers = 2.5 seconds ~ Respiration Cycle*

- **Organ motion can be an issue**

# What Names are used? (Technology)

- Dose Driven Scanning: *Dose at a spot determines what to do next.*
  - **Spot** Scanning: Irradiate one “spot” at a time. Stop the beam while moving to the next spot. Dose at a spot determines when to move. (LCD/LED TV)
  - **Raster** Scanning: Irradiate one “spot” at a time (mostly). Move the beam to the next spot while the beam is on.

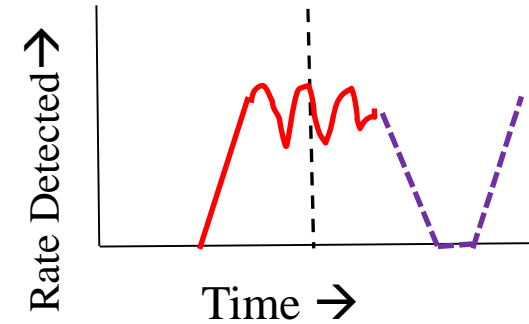
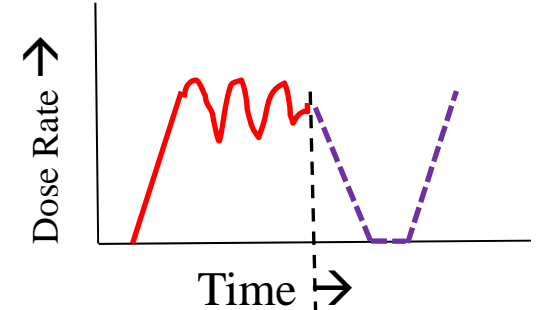
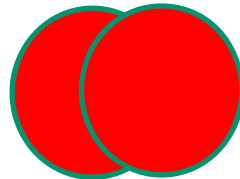
Spot



Raster



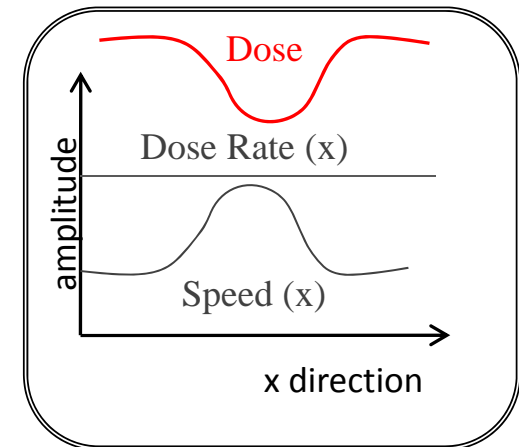
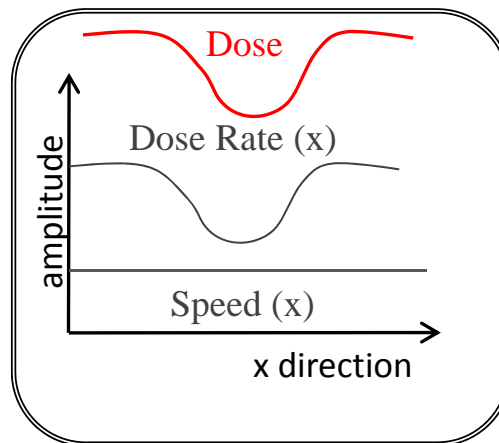
Many Spots = Anything ?



It takes TIME to measure and stop the beam if something is wrong. →  
Dose Rate LIMIT

# What Names are used? (Technology)

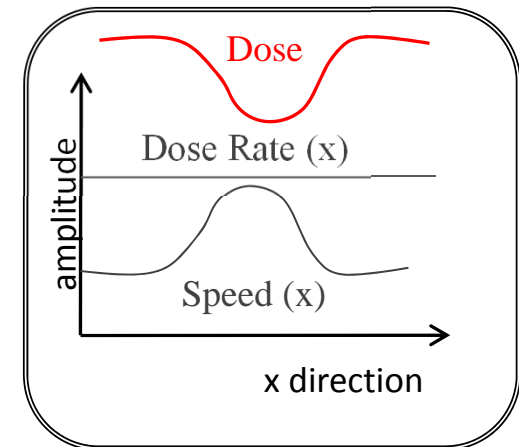
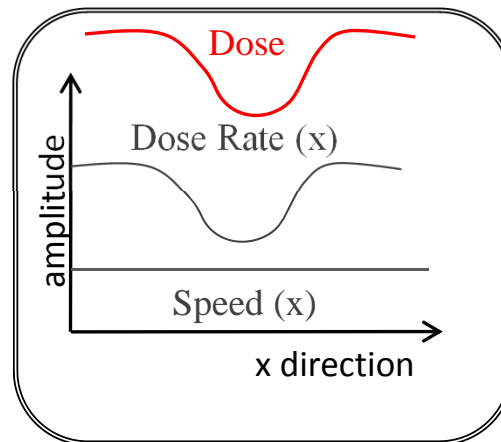
- Dose Driven Scanning: *Dose at a spot determines what to do next.*
  - **Spot** Scanning: Irradiate one “spot” at a time. Stop the beam while moving to the next spot. Dose at a spot determines when to move. (LCD/LED TV)
  - **Raster** Scanning: Irradiate one “spot” at a time (mostly). Move the beam to the next spot while the beam is on.
- Time Driven Scanning: *Time and intensity determines the dose at a location.*
  - Same as above (Spot & Raster)but wait a certain time rather than Dose (**If linked**).
  - Continuous/Line/Raster... Scanning: Irradiate while the beam is moving. Intensity or speed of beam can vary to determine the dose at a given location.
    - It takes TIME to measure and stop the beam if something is wrong. → Dose Rate LIMIT
    - → Repainting, even if you don't want to





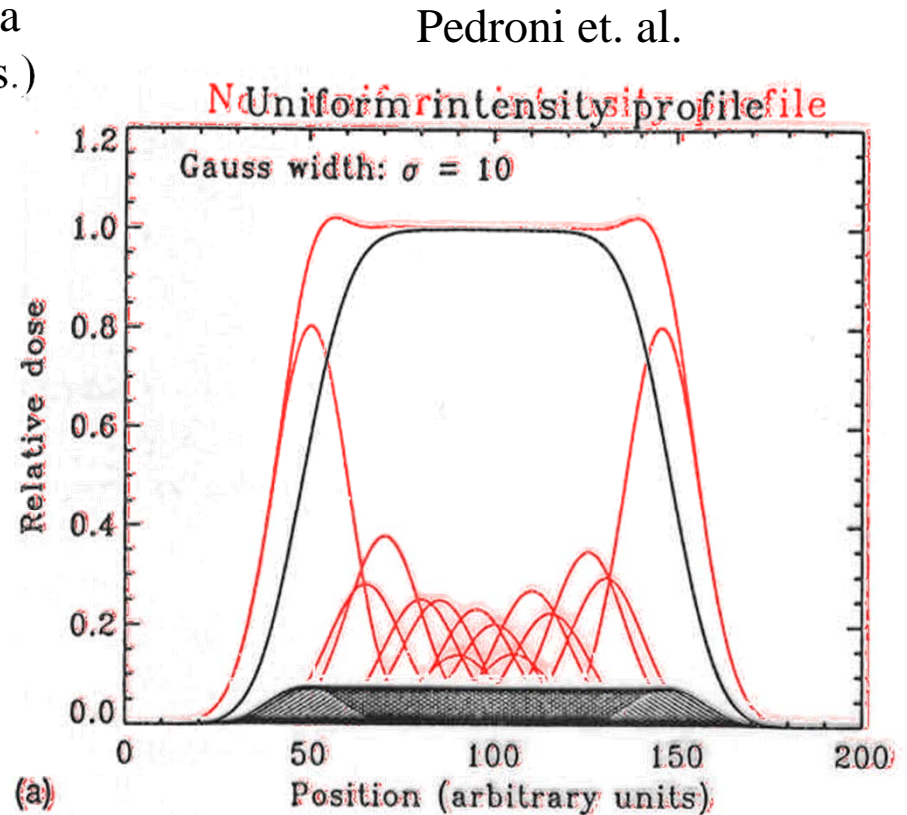
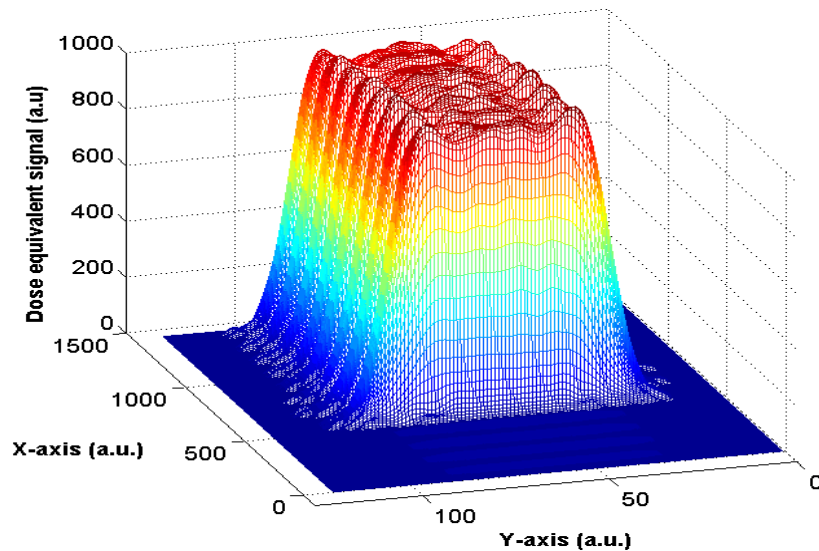
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  - Continuous/Line/Raster... Scanning: Irradiate while the beam is moving. Intensity or speed of beam can vary to determine the dose at a given location.
- Uniform Scanning: “Constant” speed and Current; Simulate Scattering
- Pencil Beam Scanning:  
Implies a very small transverse beam size (pencil point)
- Crayon Beam Scanning: Not so small as a pencil
- Others:  
Mechanical Motion, Ribbon Scanning (with Variable Collimators),...



# Idiosyncrasies of Scanning: *e.g. Penumbra Optimization*

- Penumbra Optimization (ala PSI/Berkeley)
  - This results in a balance between penumbra and overall uniformity. (There will be ears.)
  - TPS provides the map which must be compared with the measurement

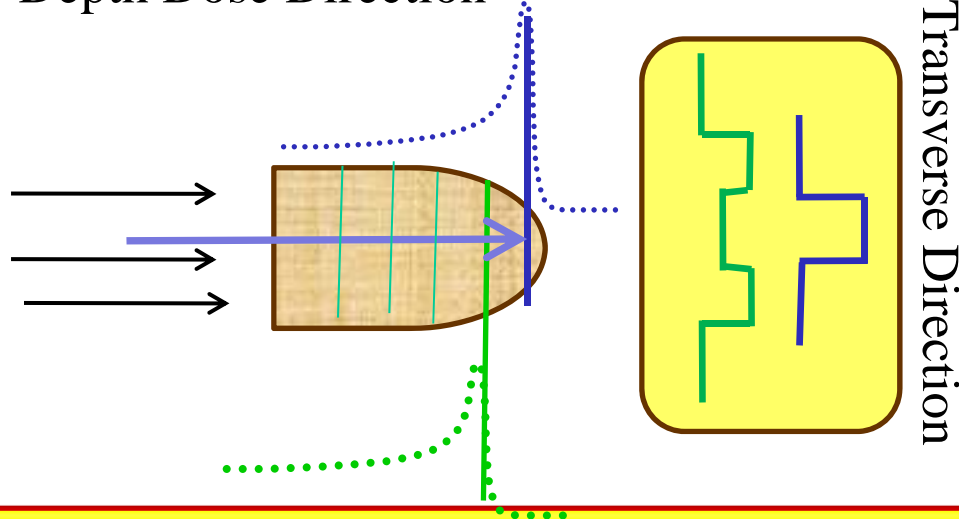


Therefore “Fluence Modulation” is required even for optimized Single Field Uniform Dose !

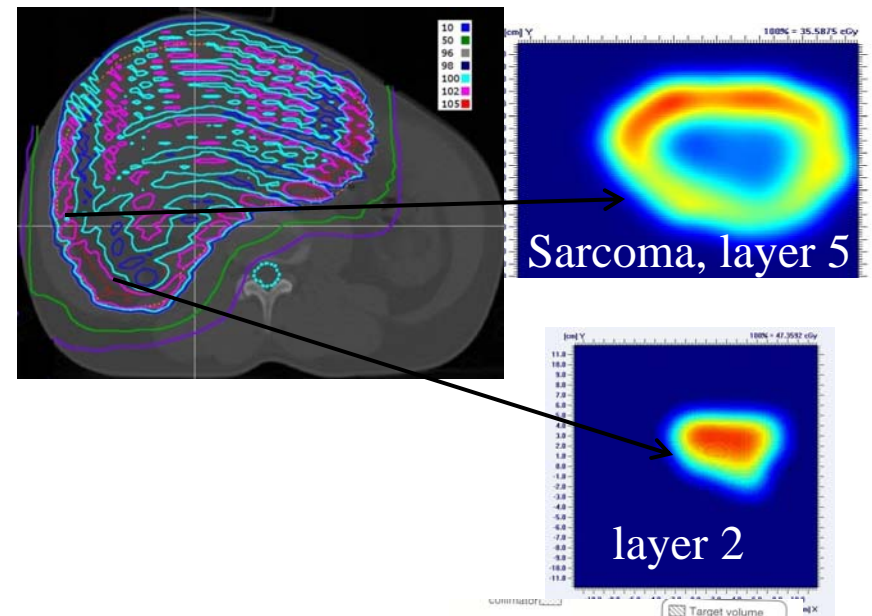
# Names for Scanning (Delivery)

- SFUD: Single Field Uniform Dose
  - Deliver a dose distribution with a scanning beam. At the **end of one field** the dose to the target should be uniform. (*Note that this says NOTHING about the distribution of any given subset of that dose.*)

Depth Dose Direction



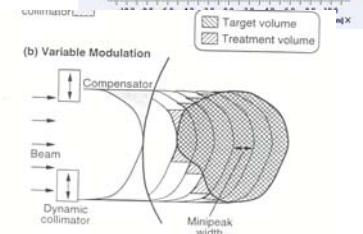
MGH 1st Patient Treatment – 4 liter Sarcoma



**SFUD REQUIRES Dose Modulation**

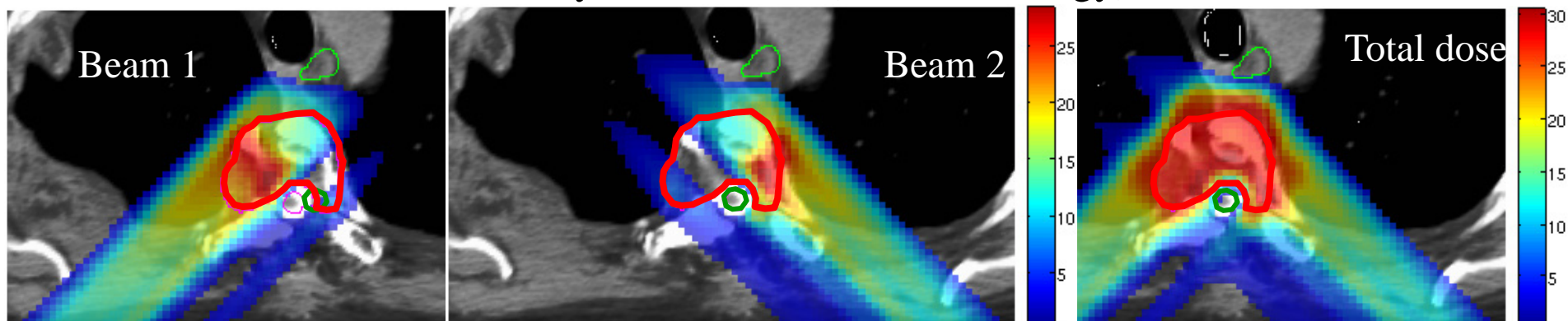
Why not a **BOOST** in a single field?

Without a Compensator  
Can Consider *WITH* a  
Compensator



# *Names for Scanning (Delivery)*

- SFUD: Single Field Uniform Dose
- IMPT: ~~Intensity~~ Modulated Particle Therapy
  - Deliver a dose distribution with a scanning beam. At the end of one field the dose to the target may NOT be uniform. Multiple fields will create a uniform or prescribed distribution. (In this case it takes Multiple Fields for Uniform Dose not a Single Field)
  - The number of protons deposited at a location MAY HAVE NOTHING to do with the Intensity of the beam (see Technology).

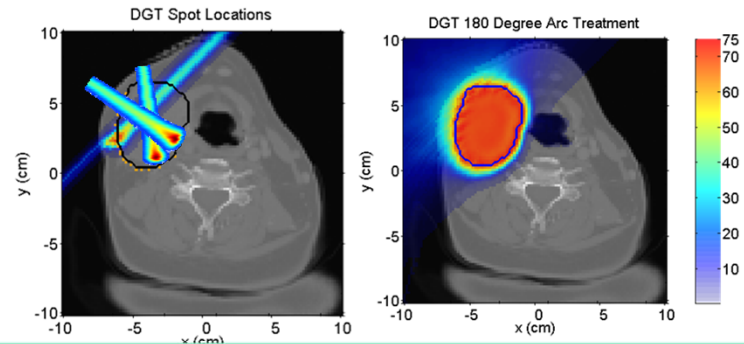


These names IMPLY the RESULT of a SINGLE field! There is NO difference between SFUD and IMPT/MFUD in the delivery technology (**unlike** 3DConformal vs. IMXT) but there could be a big difference in the character of IMXT and so-called IMPT.



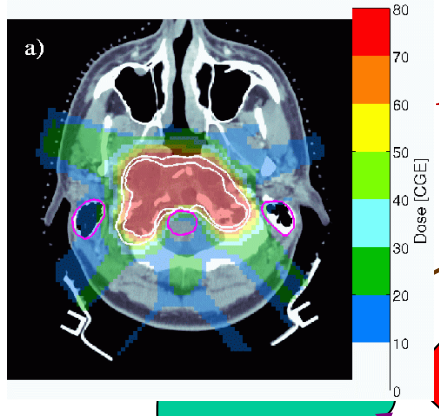
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  - The number of protons deposited at a location MAY HAVE NOTHING to do with the Intensity of the beam (see Terminology).
- DET: Distal Edge Tracking
  - Deliver beam around the target through to the distal edge of the target (!!! Angles, End of Range?)



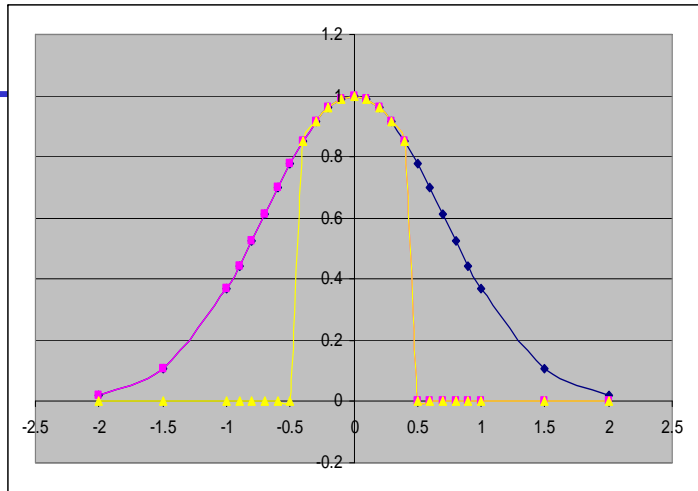
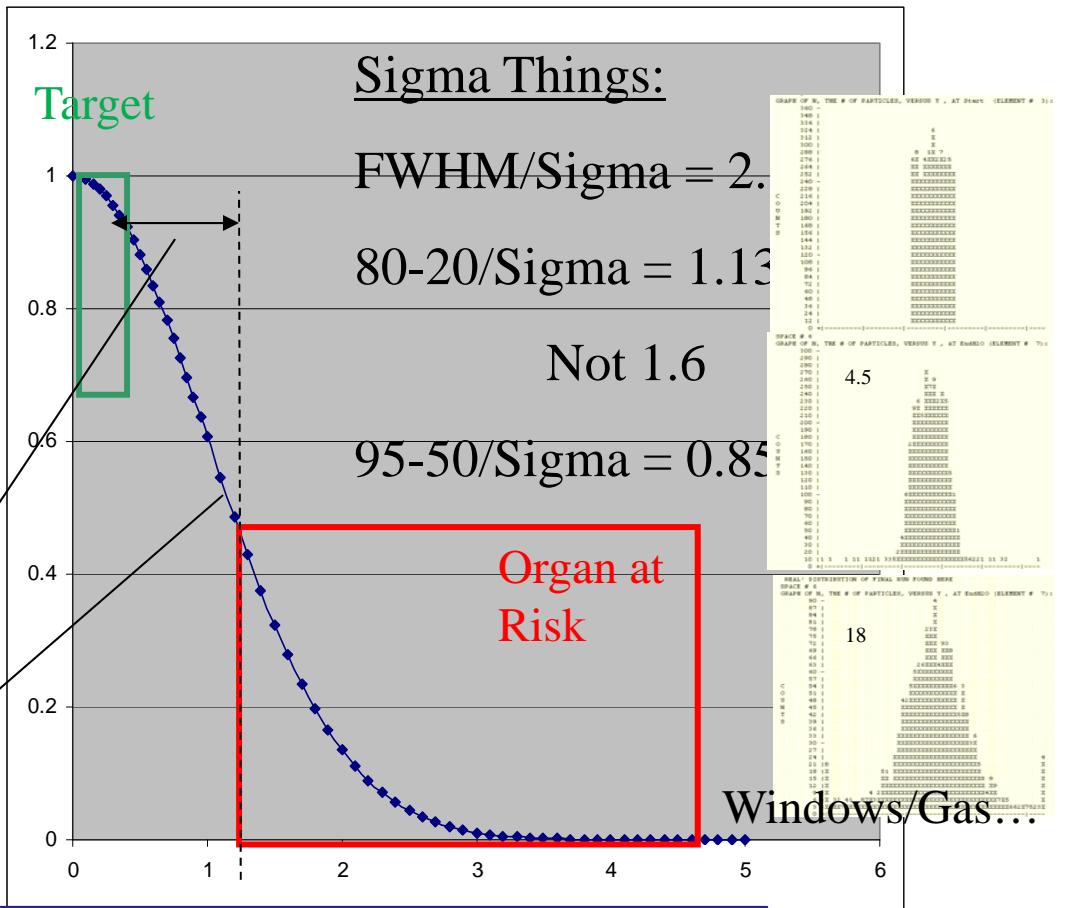
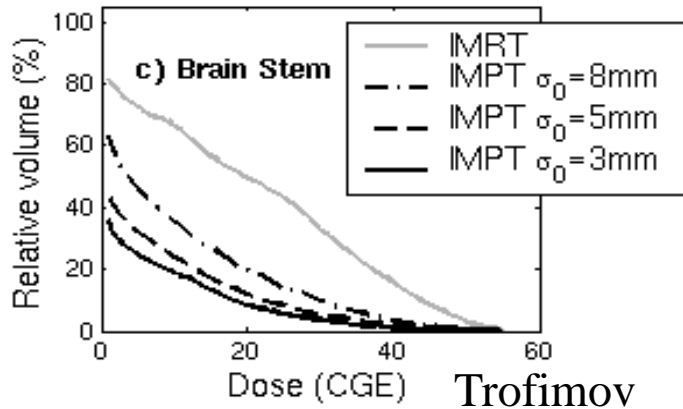
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# Beam Sigma or Penumbra or Edge ?



$$y = e^{-\frac{1}{2} \left( \frac{x}{\sigma} \right)^2}$$

Assume: Dose to Target within +/- 2.5% and Organ at Risk < 50%

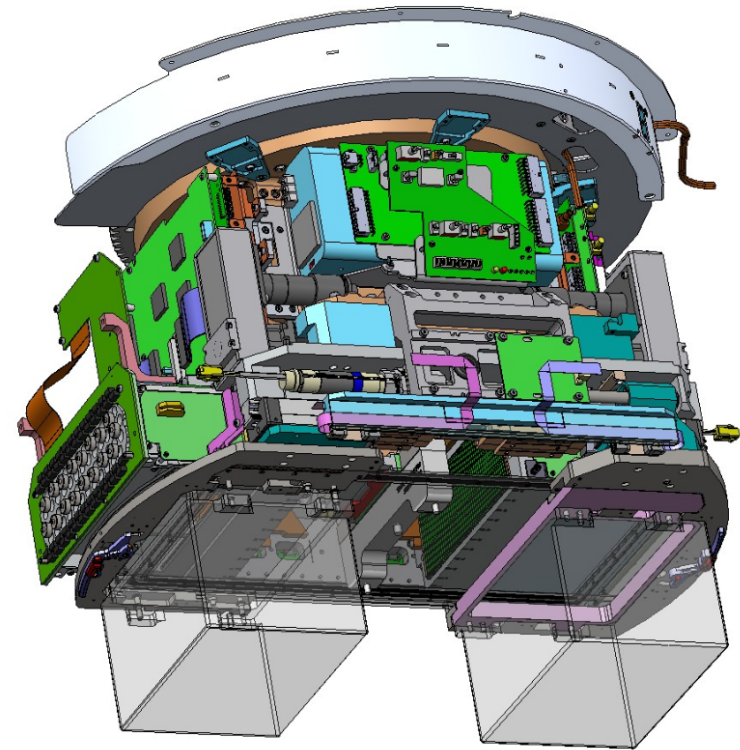
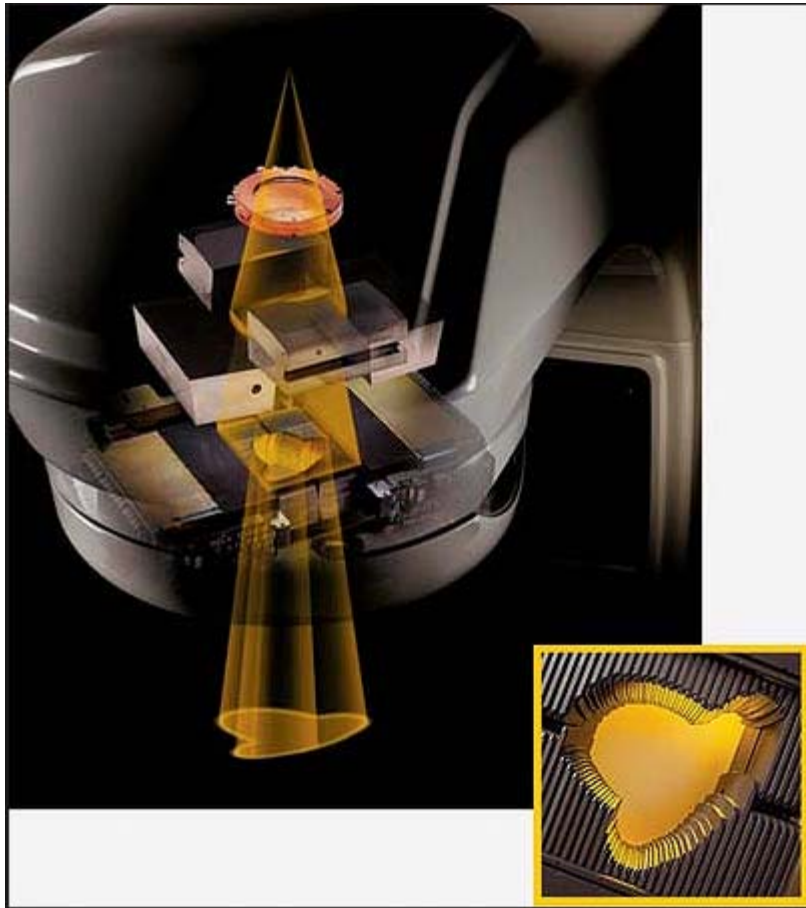


Not efficient to always use small beam !



# *Multi-Leaf Collimator for Protons*

(UPenn/Varian + Sumitomo)



# Magnetic Scanning Implementation

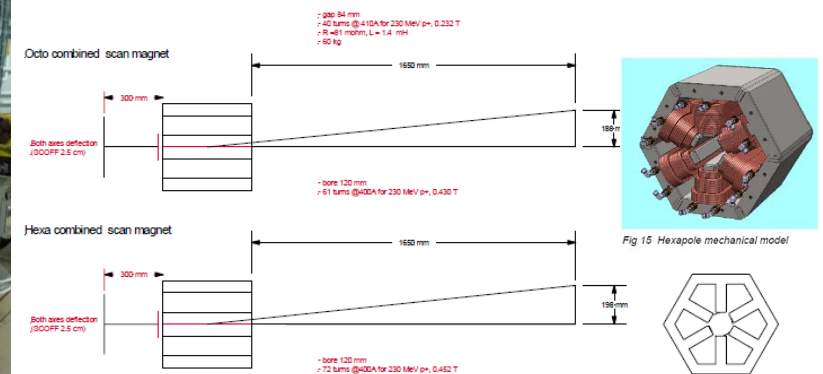
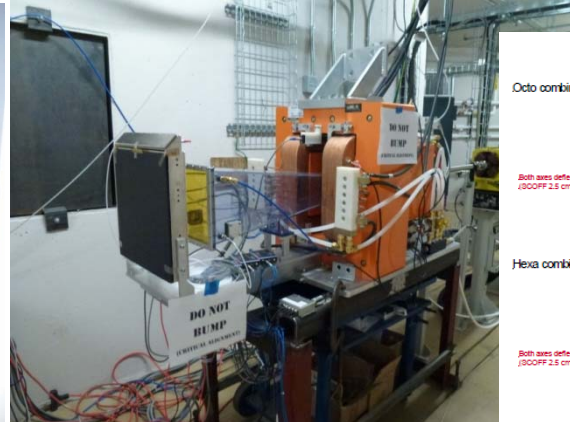
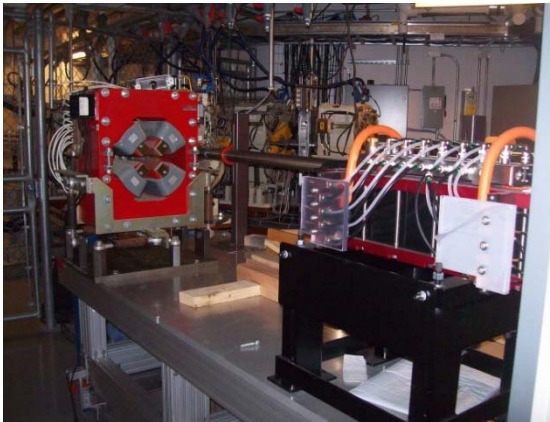
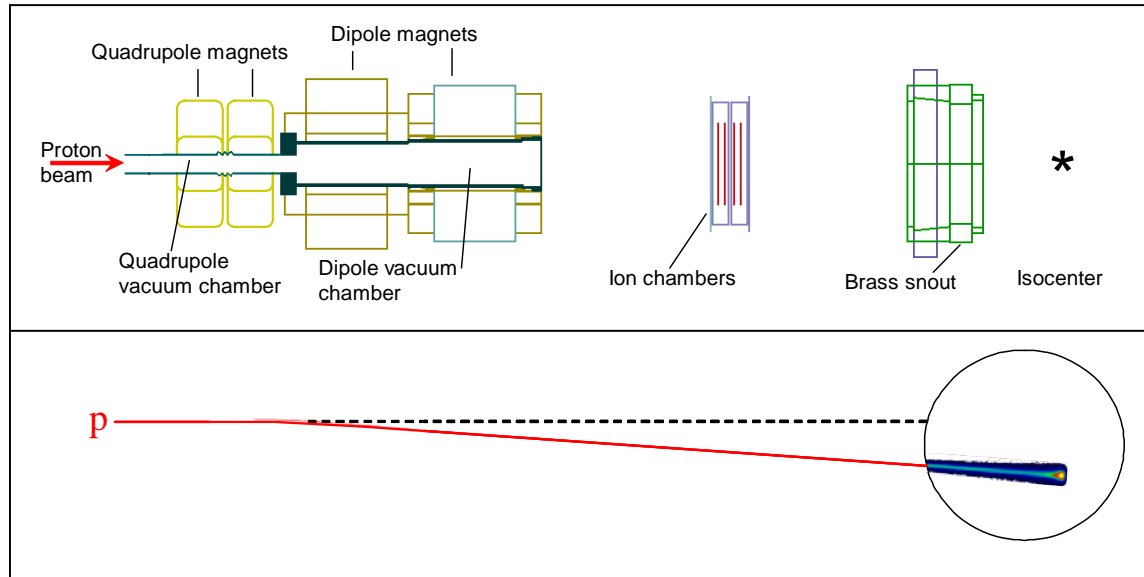


Fig 14 Deflection in multipole magnets combined-function magnet

See Poster Session !

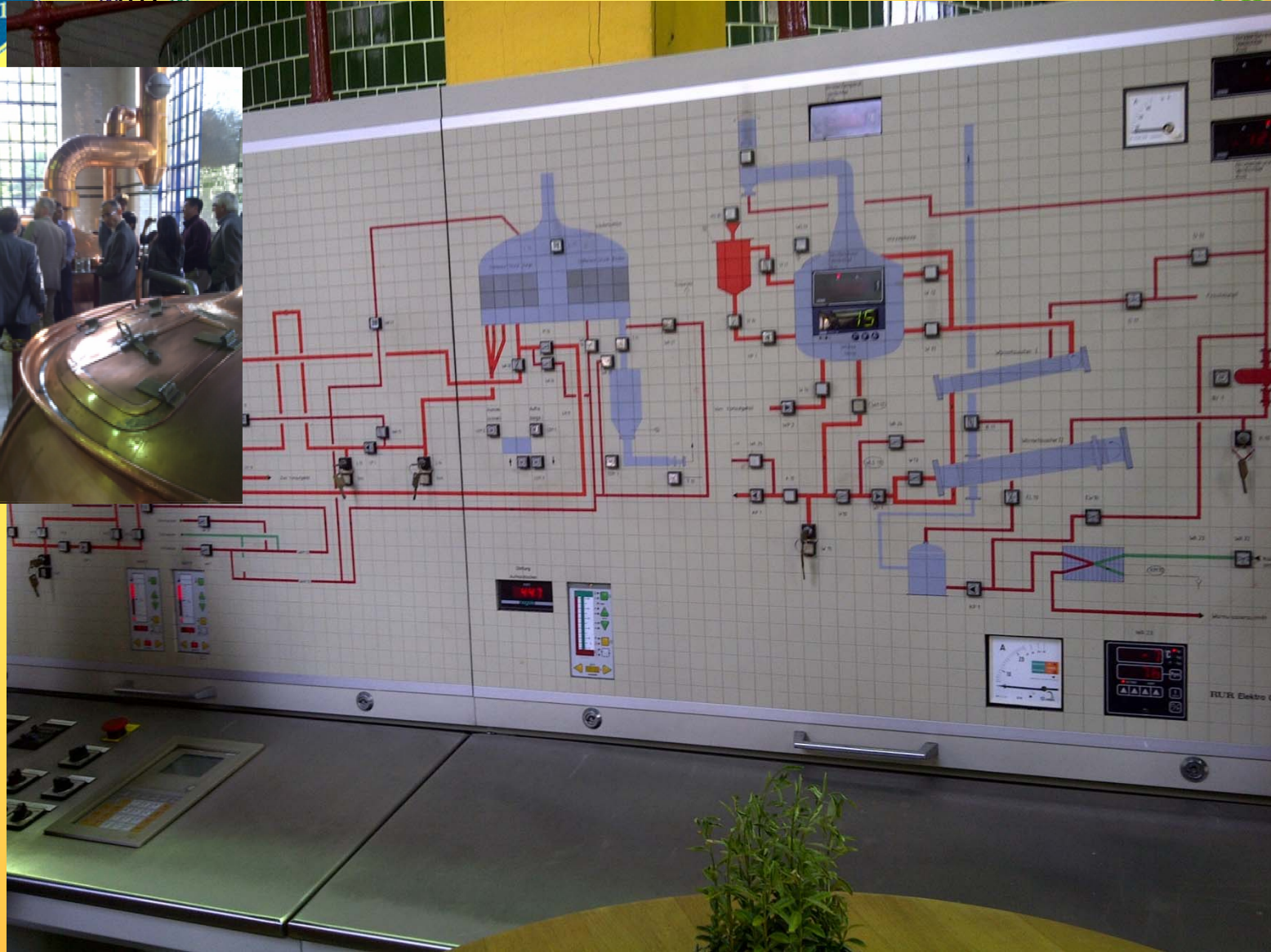






# Scanning Controls

iba



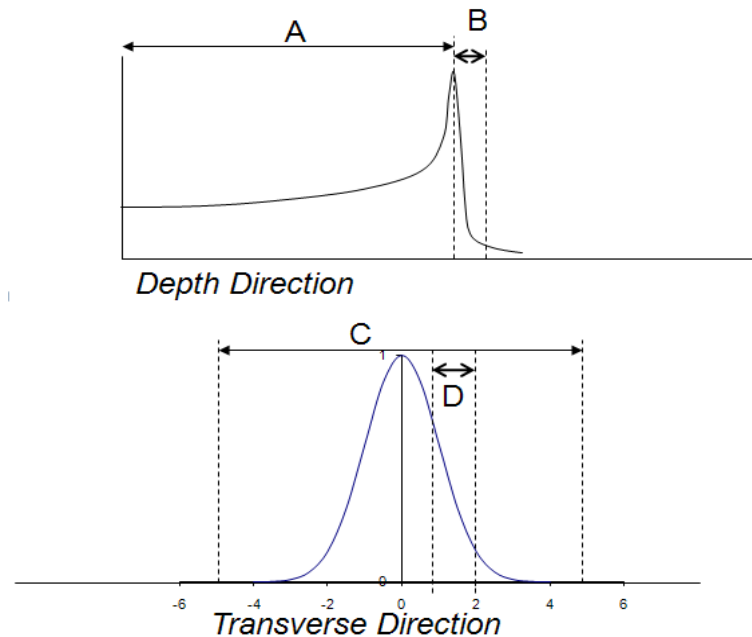
Unit



assumed

# *Dosimetric Quantities for Scanning*

Dosimetric Regions of Interest (Scanning)



- A. Range
- B. Distal Fall off
- C. Field Size
- D. Penumbra

- Reduce # fields for a uniform Dose Delivery (Clinical effects?).
- Reduce unwanted Dose (e.g. Proximal Primary Dose)
- Reduce the need for Patient Specific Equipment
  - Apertures
  - Compensators
- Reduce radiation from primary beam intercepting machine components (n)
- Allow a non-uniform Dose Delivery

# *Comparison - Time*

## **Scattering**

- Time to spread out in depth
  - Ridge Filter - 0
  - Mod Wheel – 0.1sec
  - Layer Stacking (Mechanical)
    - <1sec/layer
  - Energy Change
    - 5 sec to 0.1 sec
- Time to spread out x&y - 0

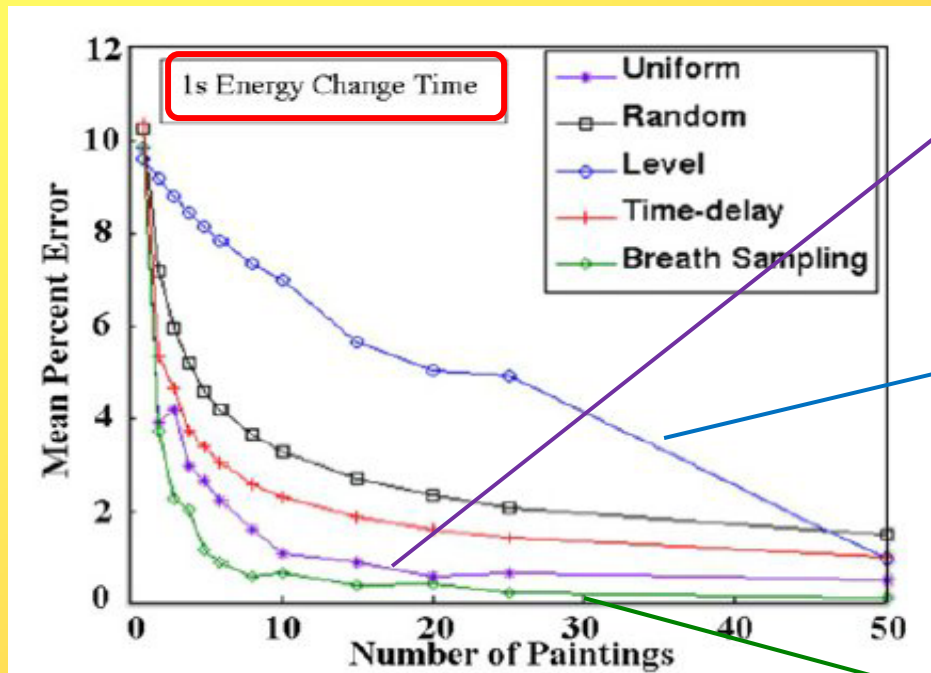
## **Scanning**

- Time to spread out in depth
  - Energy Change
    - 5 sec to 0.1 sec
- Time to spread out x&y
  - Spot scanning vs. Raster
  - Big Spots vs. Little Spots
  - >0.2sec slew time

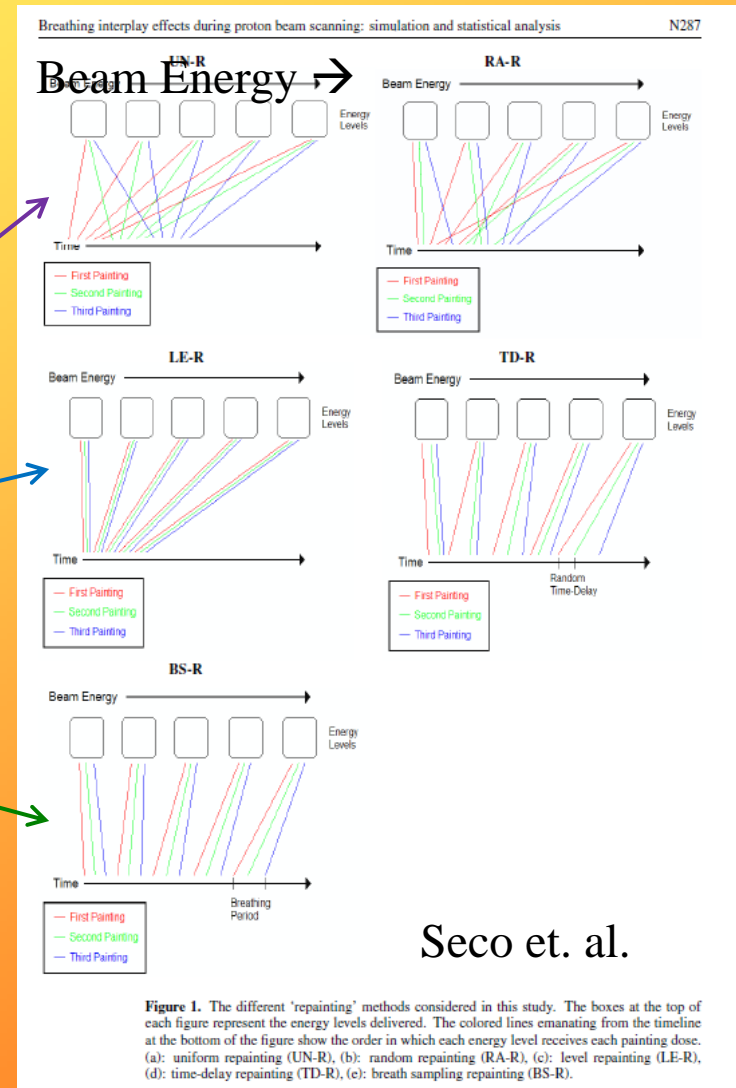


# Time Dependence of Repainting

Repainting helps to average out errors due to timing effects - Later



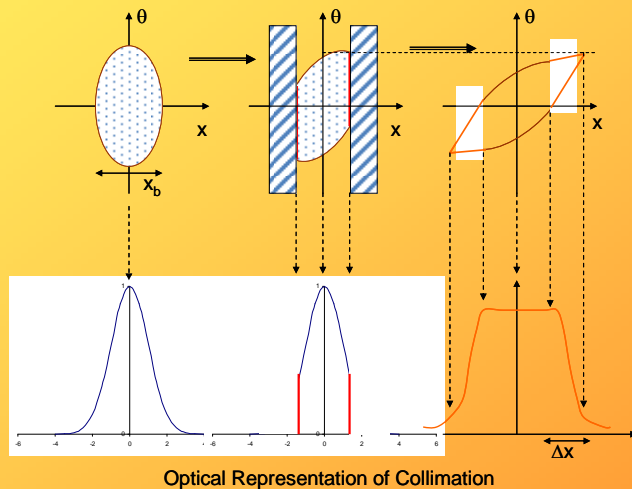
Therefore: Fast repaintings of a layer (e.g. continuous scanning) may not be better than slower. Must redo this for diff dE times!



# Comparison - Penumbra

## Scattering

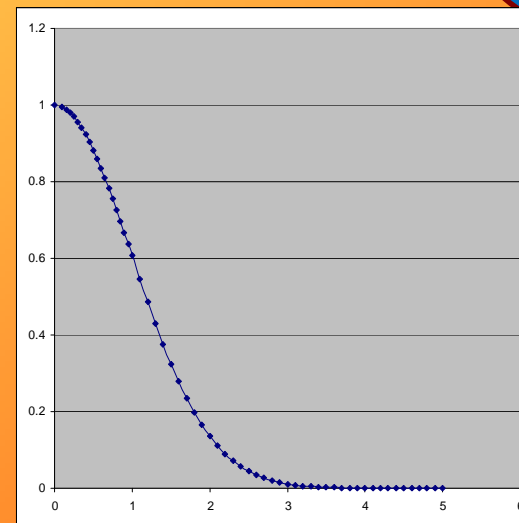
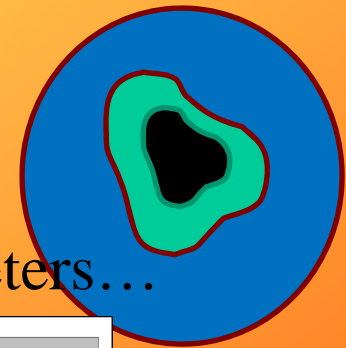
- Source Size
  - Single Scattering
  - Double Scattering
- Aperture
  - Must be used
- Distances



Depends upon  
Equipment/Hardware !

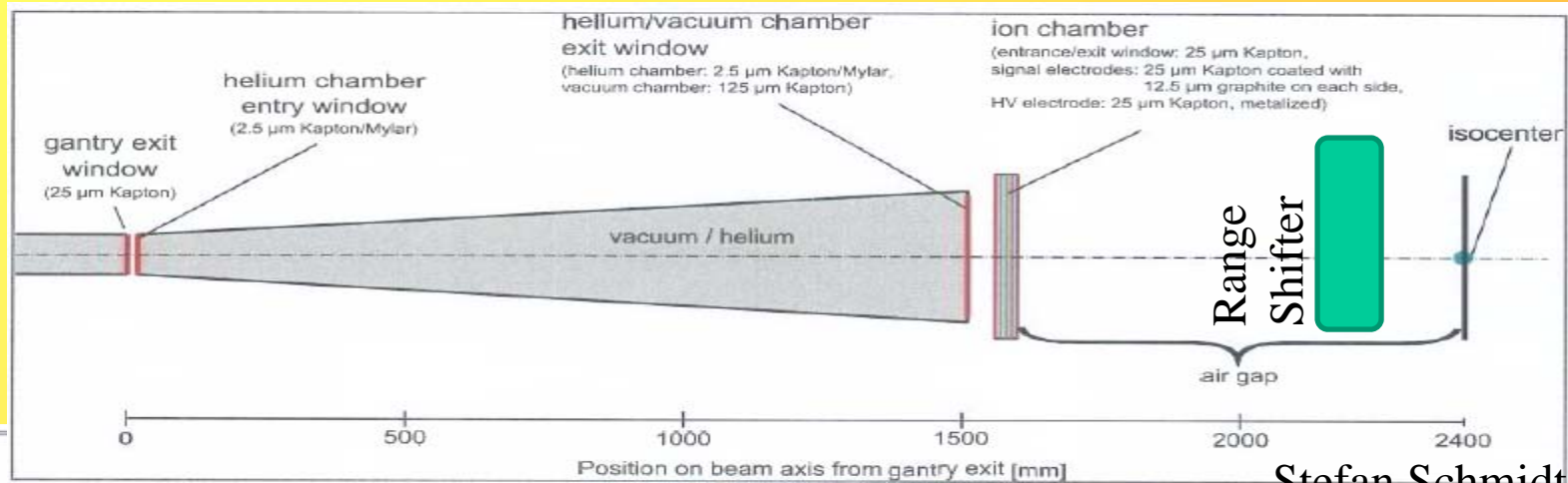
## Scanning

- Beam size = Source Size
  - Energy Change – Size dependence
- Aperture
  - CAN be used
- OTHER parameters...



Depends upon Beam !

# Effects of Air gap and Range Shifter



Stefan Schmidt

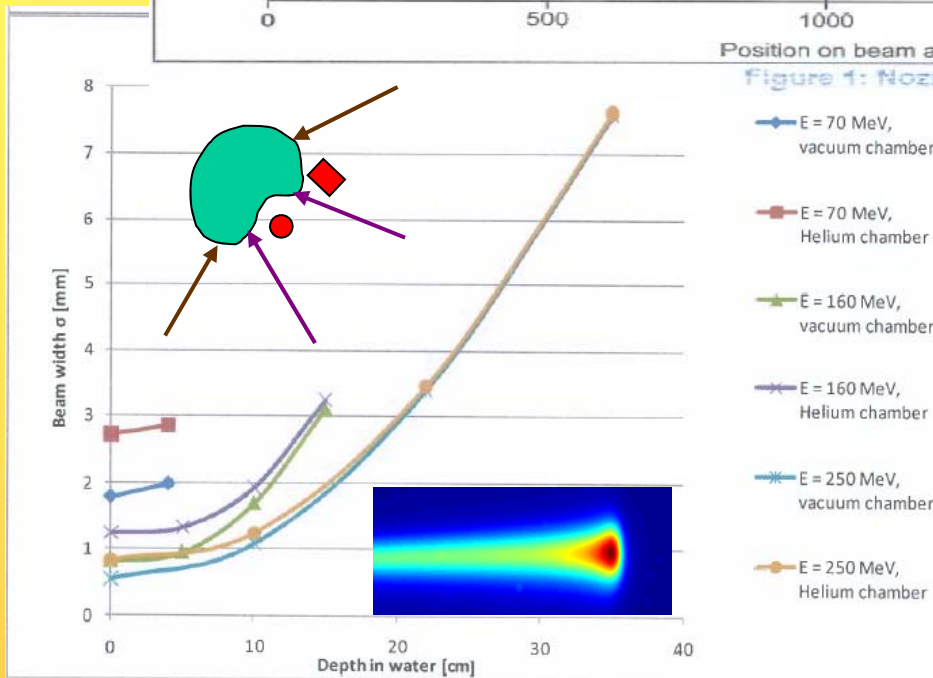
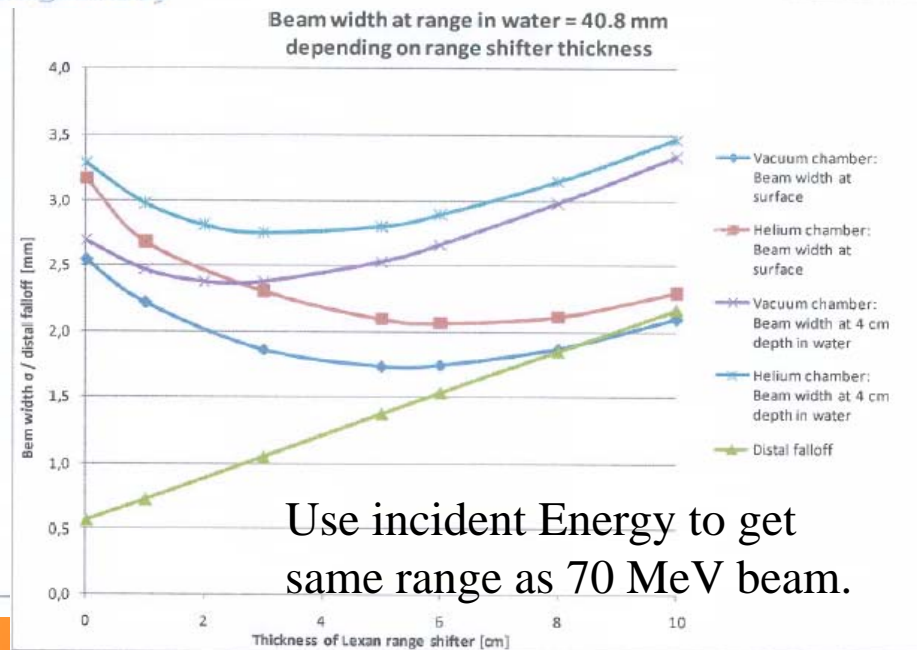


Figure 7: Beam width in water for 80 and 60-cm air gap

Figure 1: Nozzle geometry

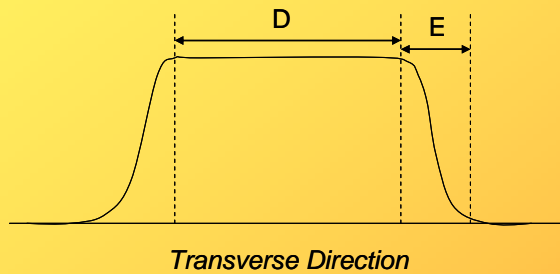
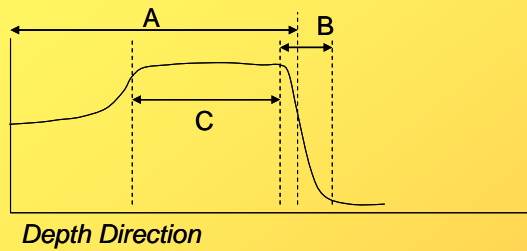


Use incident Energy to get same range as 70 MeV beam.

# Comparison - QA

## Scattering

Dosimetric Regions of Interest

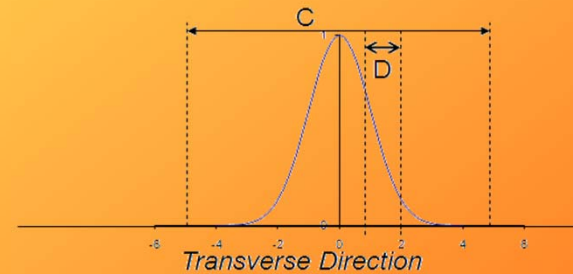
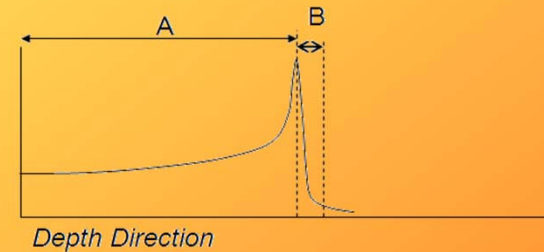


- A. Range
- B. Distal Fall off
- C. SOBP Width
- D. Lateral Width/Uniformity
- E. Penumbra

Depends upon  
Equipment/Hardware !

## Scanning

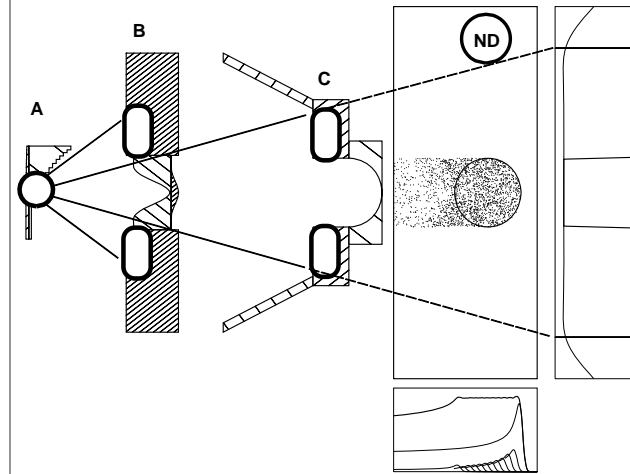
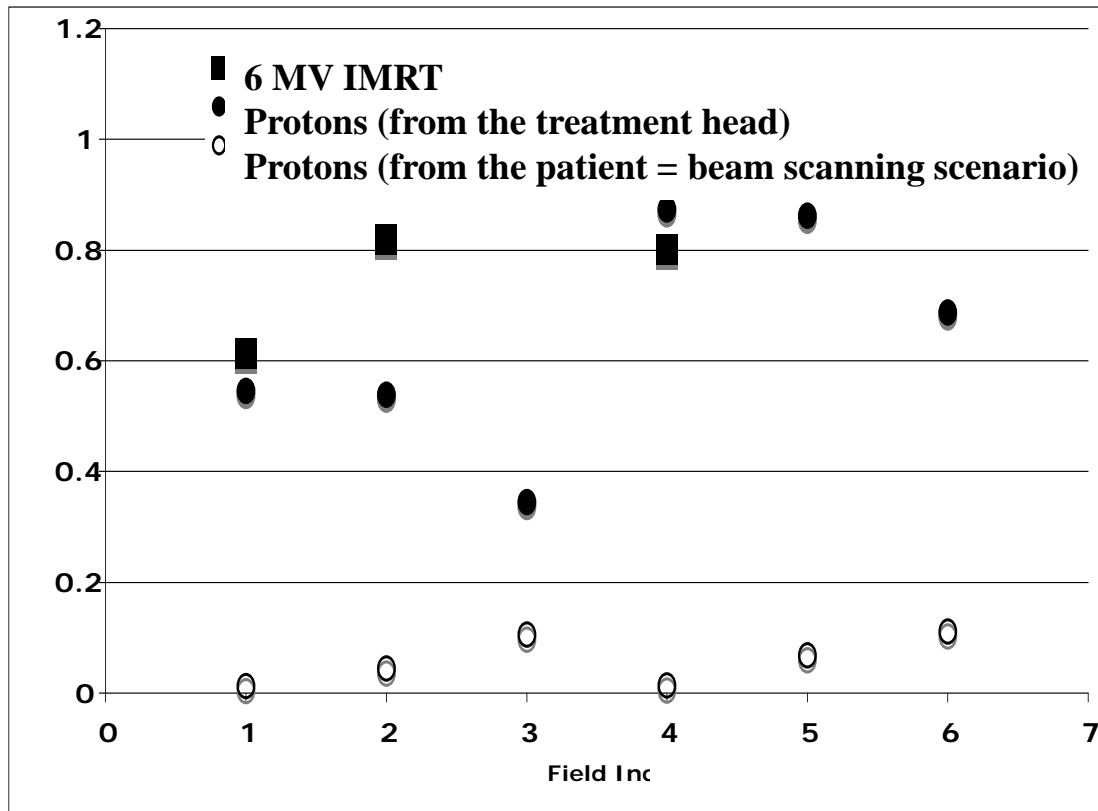
Dosimetric Regions of Interest (Scanning)



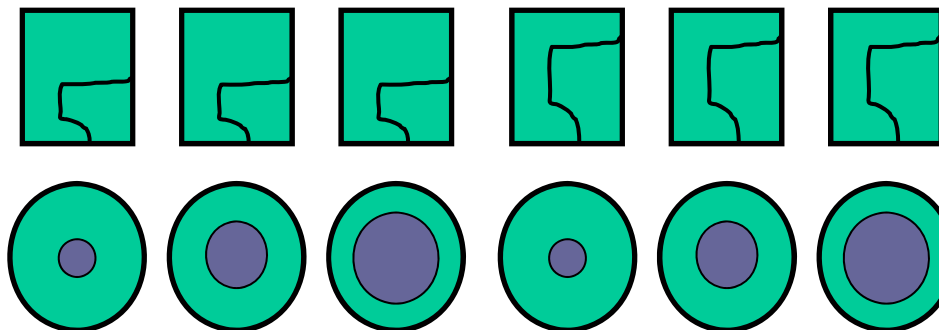
- A. Range
- B. Distal Fall off
- C. Field Size
- D. Penumbra

Depends upon Beam !

# IMRT and proton therapy / spine fields



Gottschalk



Photon and neutron equivalent doses as a function of field index

Paganetti



# *Innovations in Particle Therapy*

## *Enabled by OR Required by Scanning !*

- ***Image Guided Therapy (IGRT)***
  - *Need for more accurate alignment*
  - *Possibility to use proton Imaging*
- ***Hypofractionation***
  - *Need better conformality*
- ***Adaptive Therapy***
  - *Image; Re-Plan (Deformable registration); Treat*
    - *No patient specific Equipment*
- ***Organ Motion***
  - *Beam timing; Beam Tracking; Flex-Plan*
- ***End of Range Accuracy***
  - *Use of DET,*
  - *Simpler Plans*
- ***Increased Throughput***
  - *Less patient hardware (Field to field time)*
- ***Lower Cost (vs. Better Parameters)***

# Summary

- The basic principles to modify raw beam to deliver a uniform dose to a target, have been described. Basic physical principles of the interaction of ions with matter is the basis of the optimization of these methods.
- **Scattering**
  - *Sometimes the term “passive” scattering has been misused. Most modern scattering systems require synchronization of the beam with a moving device, either a wheel or paddles. In some cases, the beam current is further modulated.*
  - *Single scattering provides the smallest penumbra, but is very inefficient in terms of beam usage and can result in secondary radiation produced*
  - *Double scattering is more efficient, in some cases up to 40%.*
- **Scanning**
  - *Scanning has the promise for the most conformal treatment, but is also most sensitive to organ motion.*
  - *Beam scanning is essentially 100% efficient and minimizes the secondary radiation delivered to the patient.*
  - *A scanned beam delivery may provide the most efficient treatment scenario. Deliver multiple fields without entering the room.*
  - *Scanning may not provide the best penumbra . Creating a very small beam is very difficult and expensive and can lead to longer treatment times (under some conditions), and it may be worth considering some cases for which lightweight apertures can produce an advantage.*
  - *There may be some situations in which the use of a range compensator is useful to minimize the beam-on delivery time.*
- Many thousands of patients have been successfully treated using most of these techniques.



# The Francis H. Burr Proton Therapy Center



**Thank You !**